

High Frequency Brain Signal : Methodology and Application

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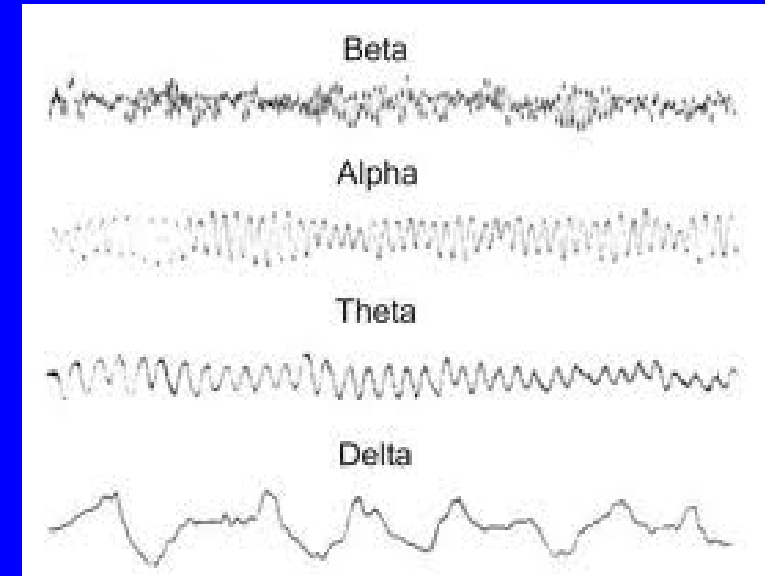
*Director of MEG Research, MEG Center
Cincinnati Children's Hospital Medical Center*

Content

- High Frequency Brain Signals (HFBS)
- Hardware development for detecting HFBS
- Software development for analyzing HFBS
- Clinical Applications of HFBS
 - Epilepsy
 - Migraine
 - Functional mapping and others
- Discussion

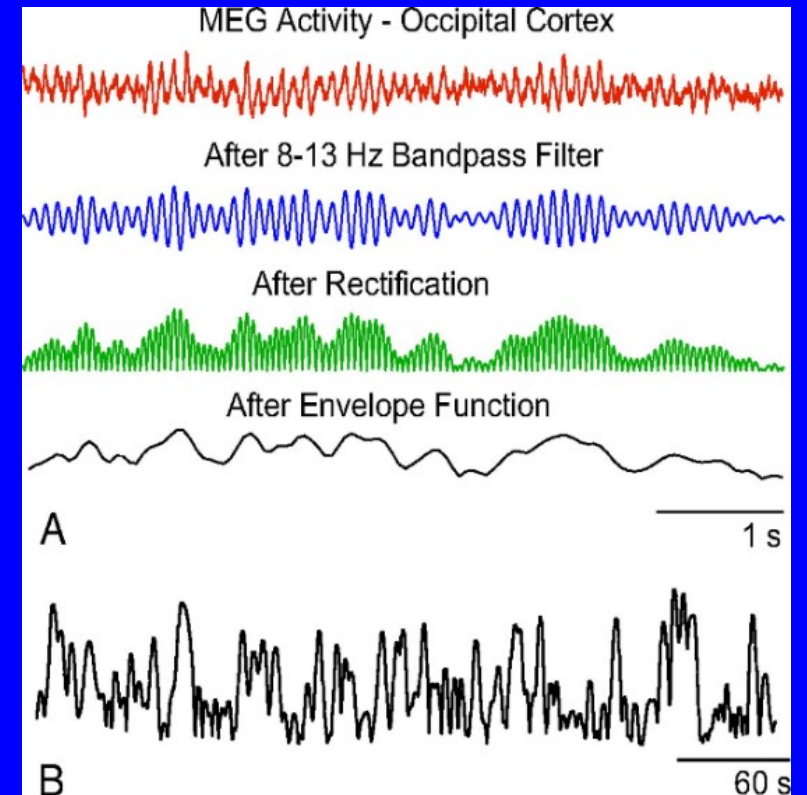
Background (1)

- The brain generate electric/magnetic signals in a set of frequency bands.
 - Delta wave – (0.1–4 Hz)
 - Theta wave – (4–7 Hz)
 - Alpha wave – (8–12 Hz, Mu: 8-13 Hz)
 - Beta wave – (13–30 Hz)
 - Gamma wave – (30–100 Hz, 30-120 Hz, 40 Hz)
 - High-frequency oscillations (HFOs): brain activity (signals) in a high-frequency range. (e.g. > 30 Hz, 70 Hz or 80 Hz)



Brain Signals in Frequency Domain

- Nomenclature for bandwidths and upper and lower bounds of each bandwidth of interest still evolving
 - Spike: 14-70 Hz
 - Gamma
 - Low 30-70 Hz
 - High 70-150 Hz
 - Ripples 80/100 – 200/250 Hz
 - Fast ripples > 200/250 Hz (250-600 Hz)
 - HFOs: 30-600 Hz
 - Very HFOs (VHFOs): 1000 – 2500 Hz (> 600 Hz)
- No standardized names or terms
- HFBS includes HFOs in the presentation

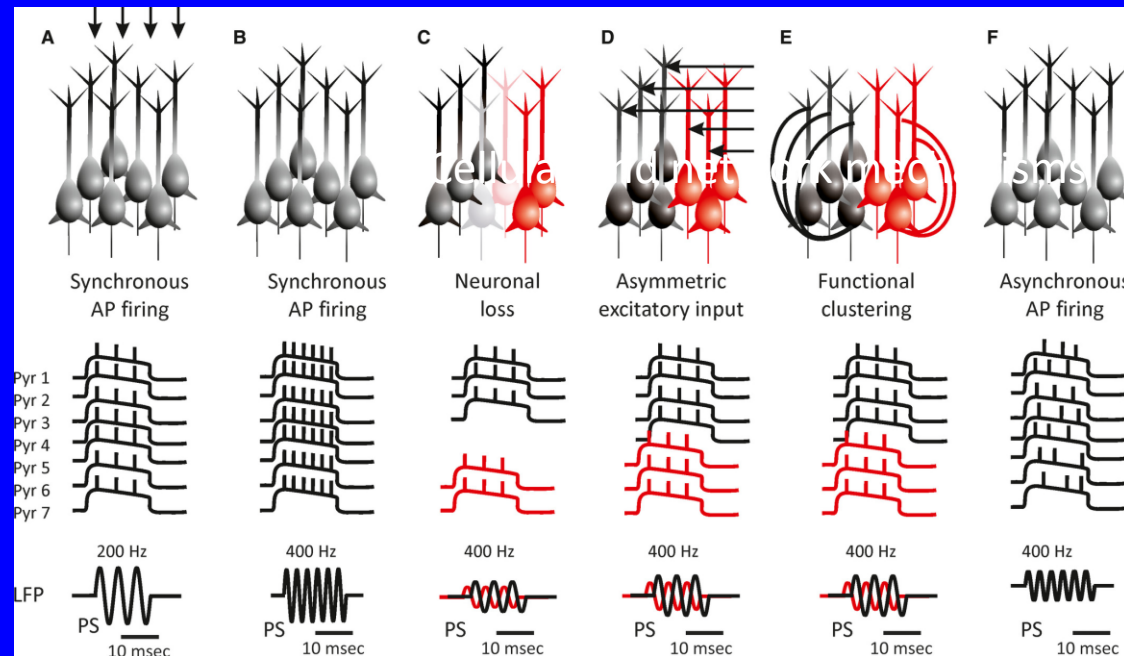


Classification of HFBS

- Physiological High Frequency Brain Signals
 - Elicited/Evoked Functional Activation (Gamma)
 - Low 30-70 Hz
 - High 70-150 Hz
 - Spontaneous/Intrinsic/Endogenous Brain Activity (HFOs)
 - Ripples
 - High 70-150 Hz
- Pathological High Frequency Brain Signals
 - Oscillatory HFOs
 - Ripples (80-250 Hz)
 - Fast ripples (250-600 Hz)
 - High frequency spikes (HFSs)
 - Spikelets (80-250 Hz)
 - Fast spikelets (250-600 Hz)

Cerebral Mechanisms (1)

- The exact mechanisms underlying the generation of HFOs remain unclear.
 - “Out of phase” activity : discharges of groups of neuronal populations.
 - “Axon-axon gap” junctions: generate coherent population oscillations higher than 100 Hz.



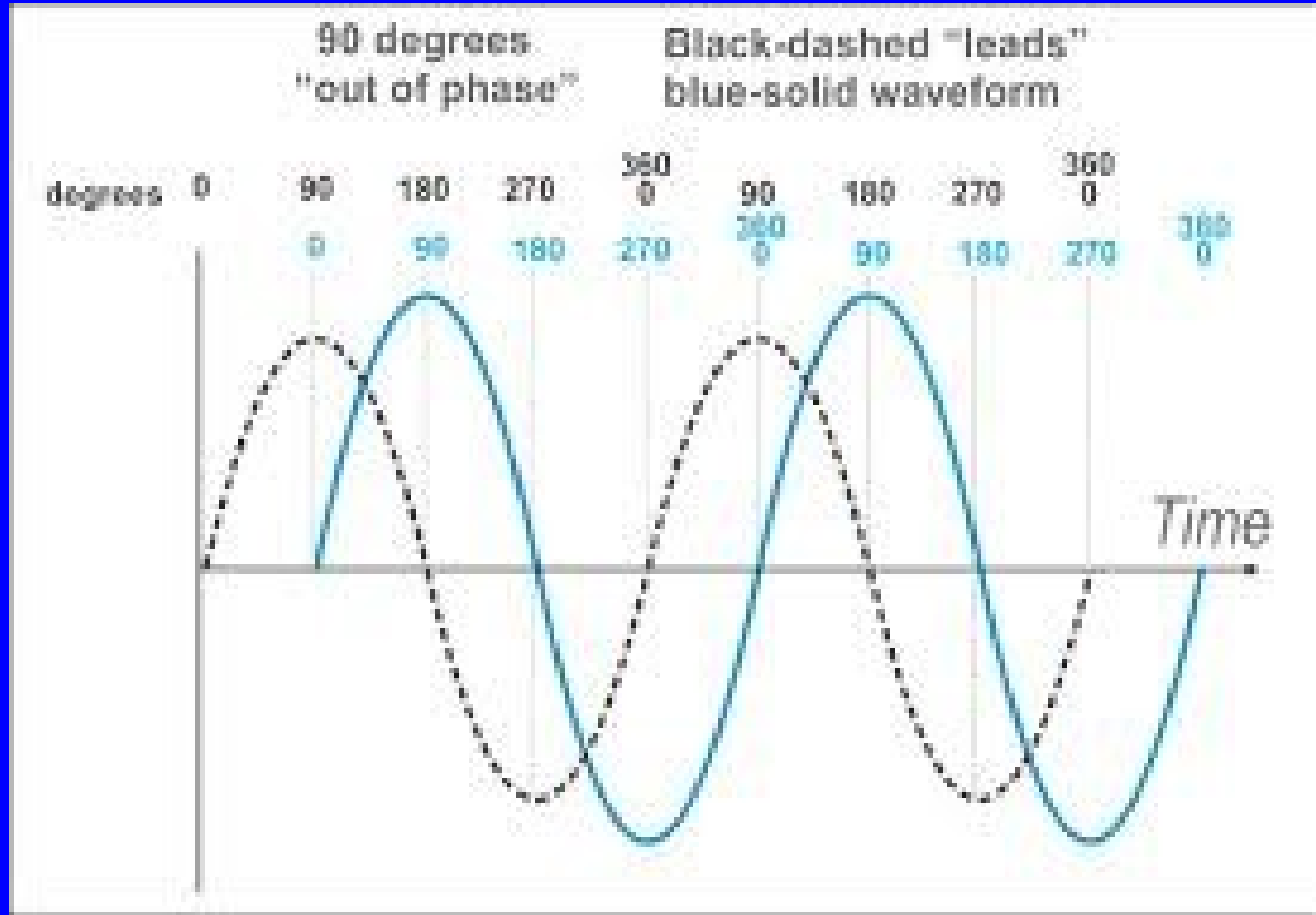
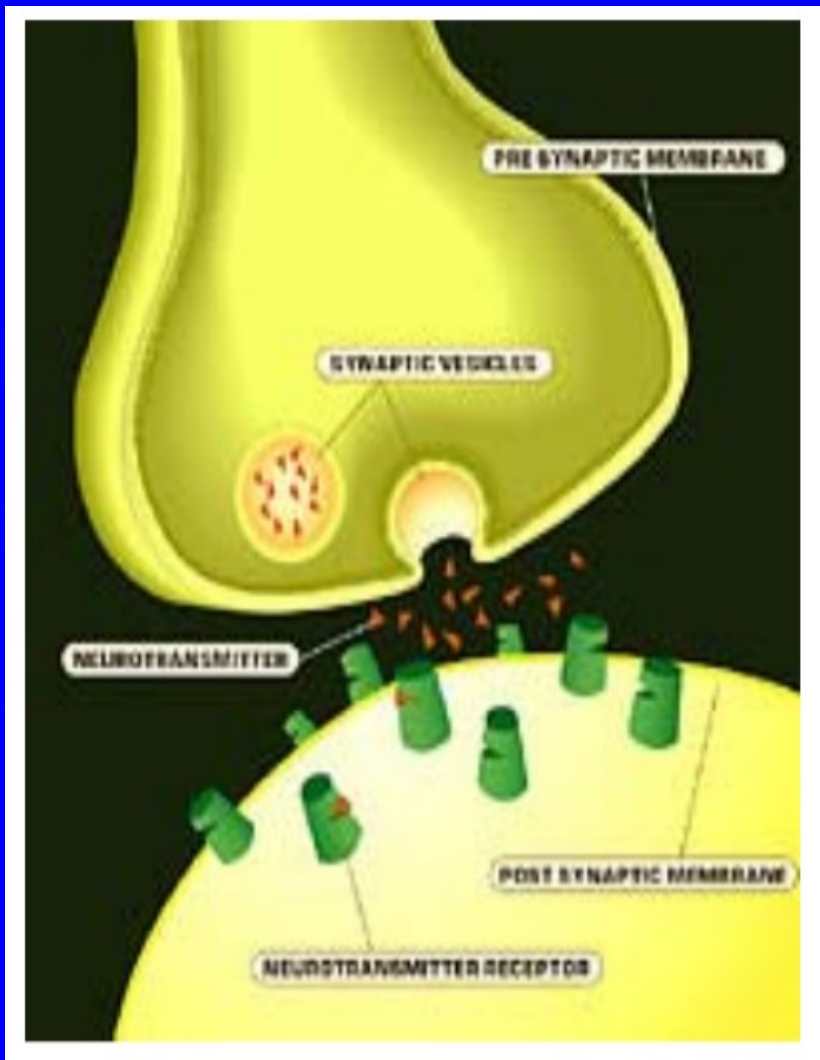
Cellular and network mechanisms of HFOs

Jiruska et al. Epilepsia 2017; 58:8; 1330

The burst discharge by pyramidal cells may be detectable with MEG and EEG when **10,000–50,000** cells are synchronously active.

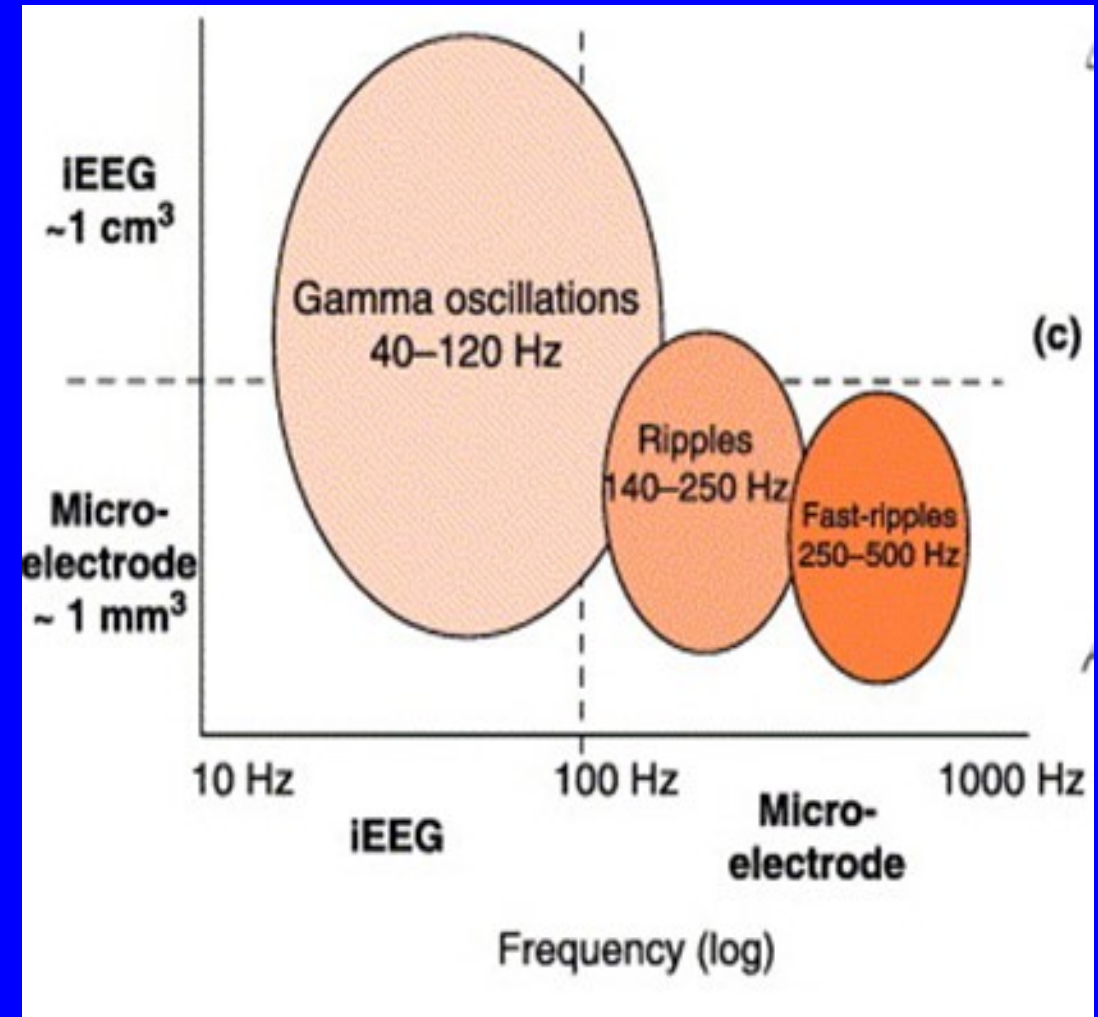
Murakami, et al. J Physiol 575.3 (2006) pp 925–936

Cerebral Mechanism (2)



Cerebral Mechanisms of HFOs

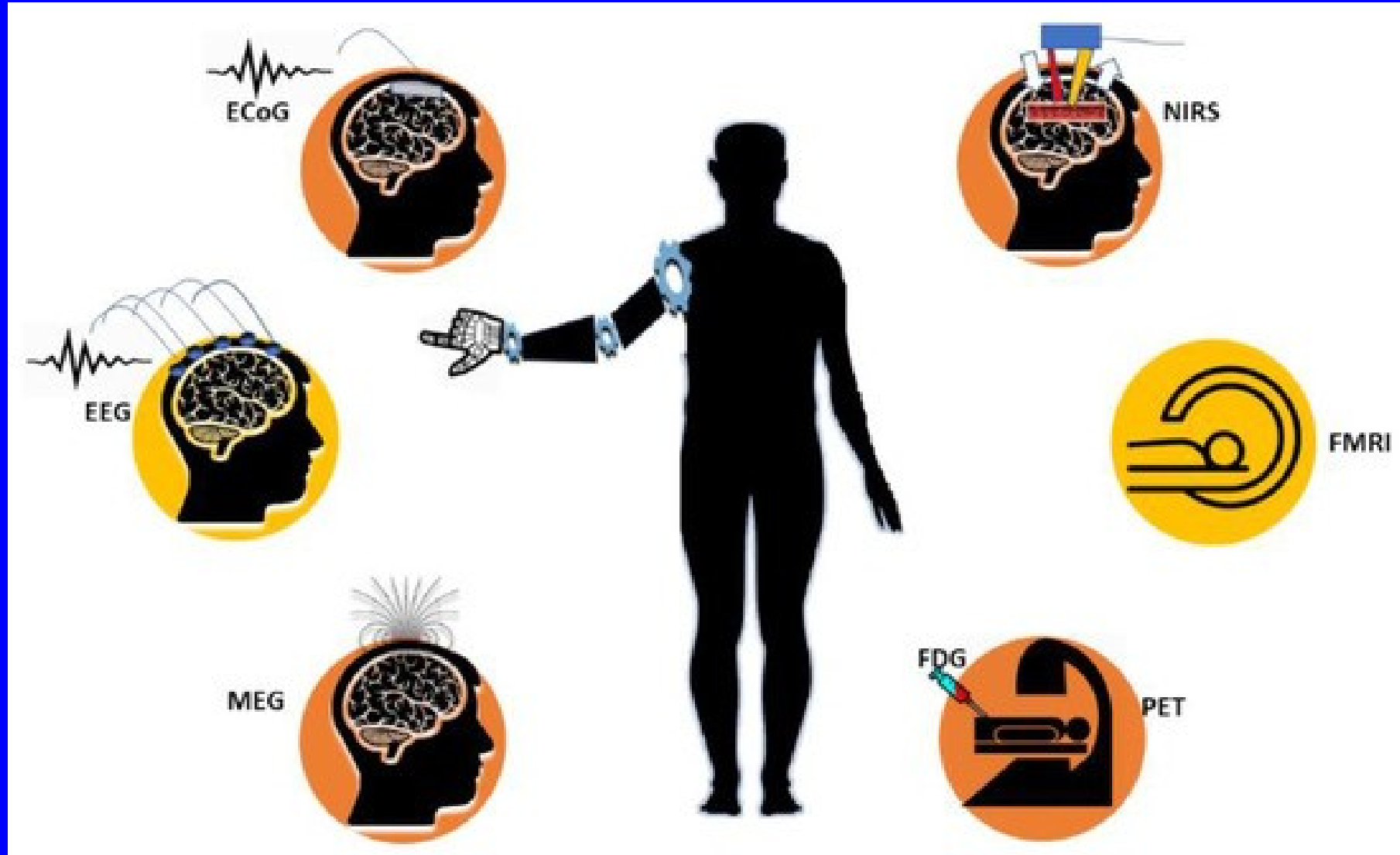
- Different generator:
 - Low frequency: post-synaptic potentials
 - High frequency: gap junction and/or “out of phase”
- Brain HFOs \neq Neural HFOs
- Frequency signatures of MEG/EEG signals
 - Spatiotemporal overlaps of $\sim 50,000$ neurons
- Frequency-spatial relation:
 - Low frequency : large area
 - High frequency: small area



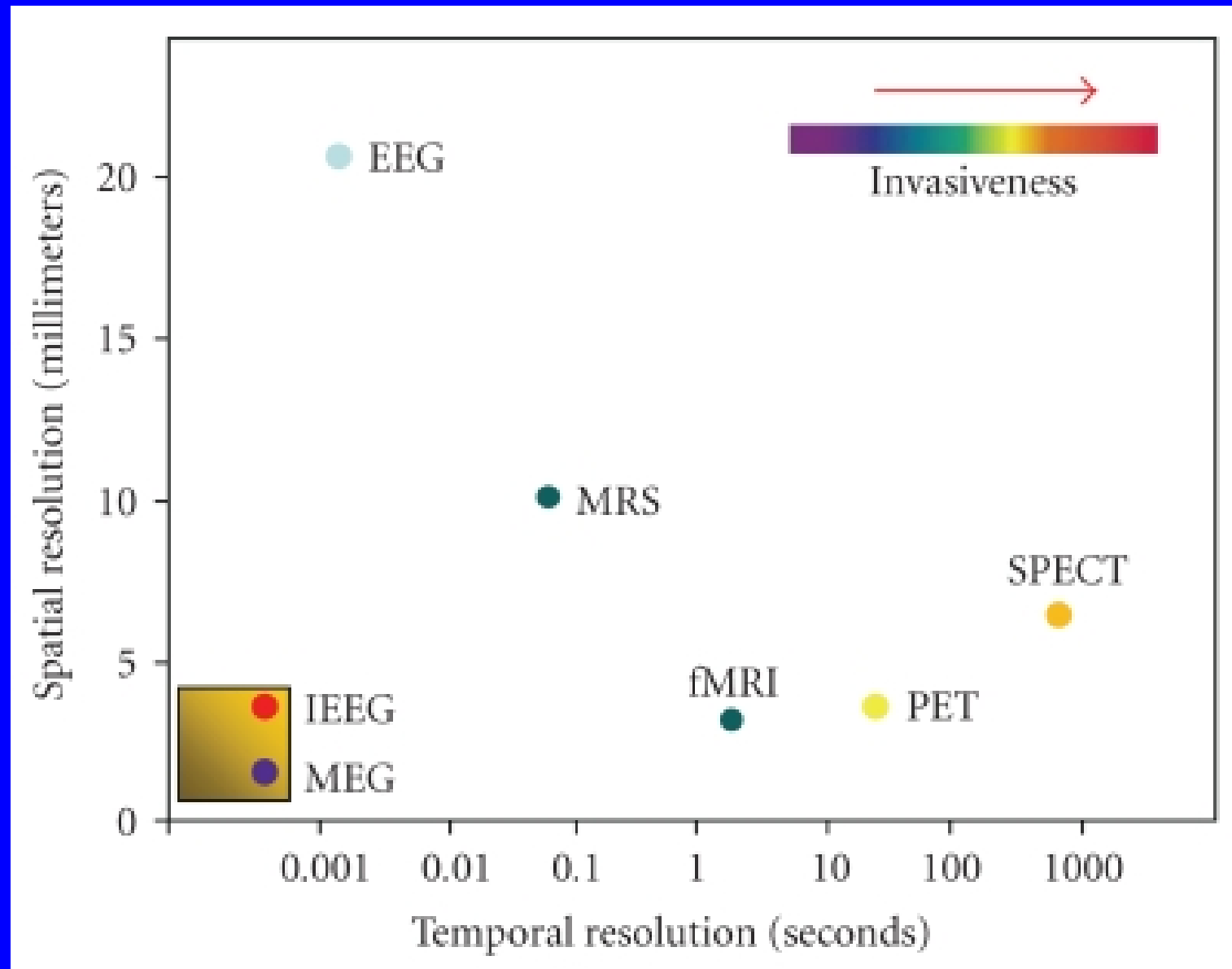
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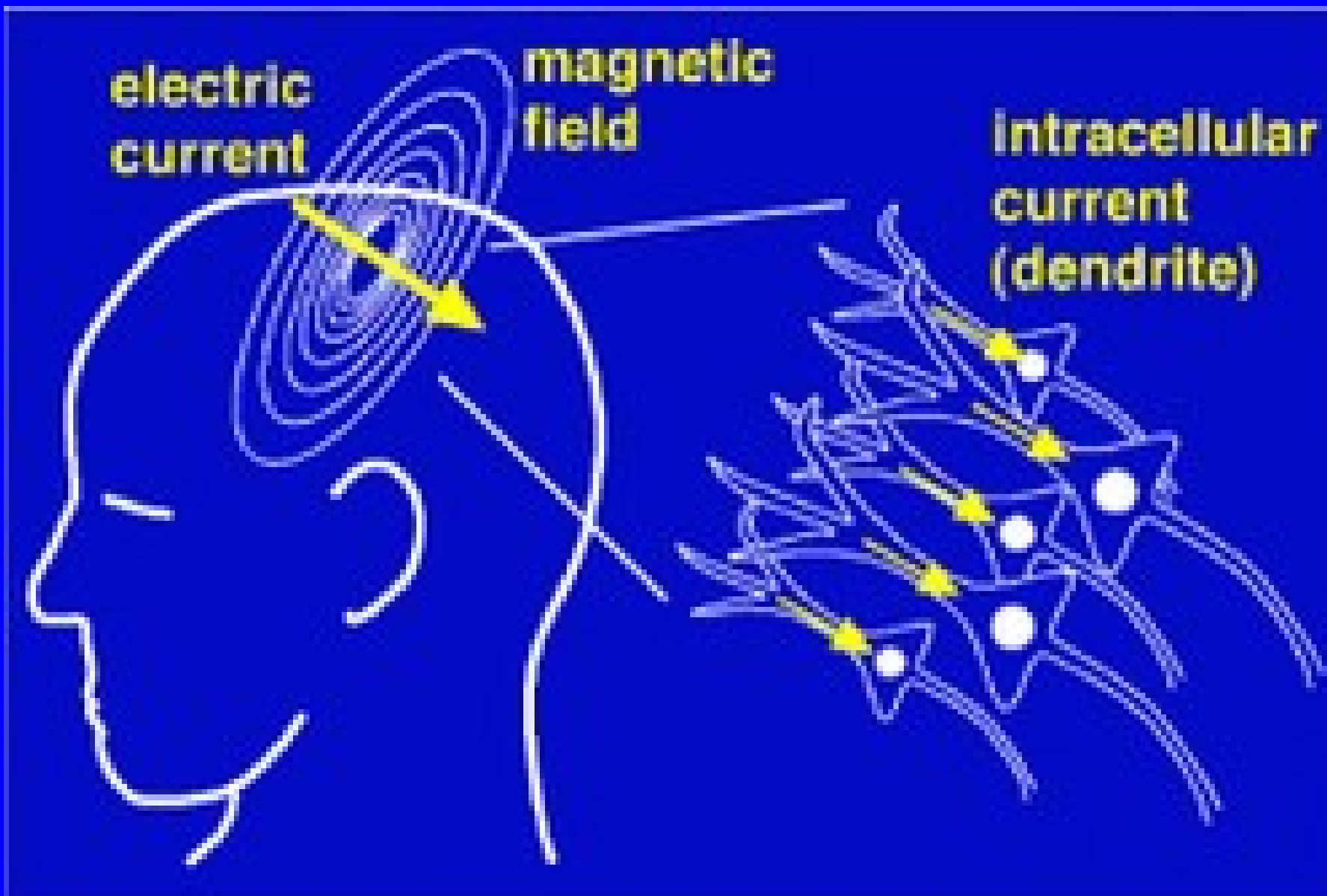
Neuroimaging Techniques for Detecting HFBS



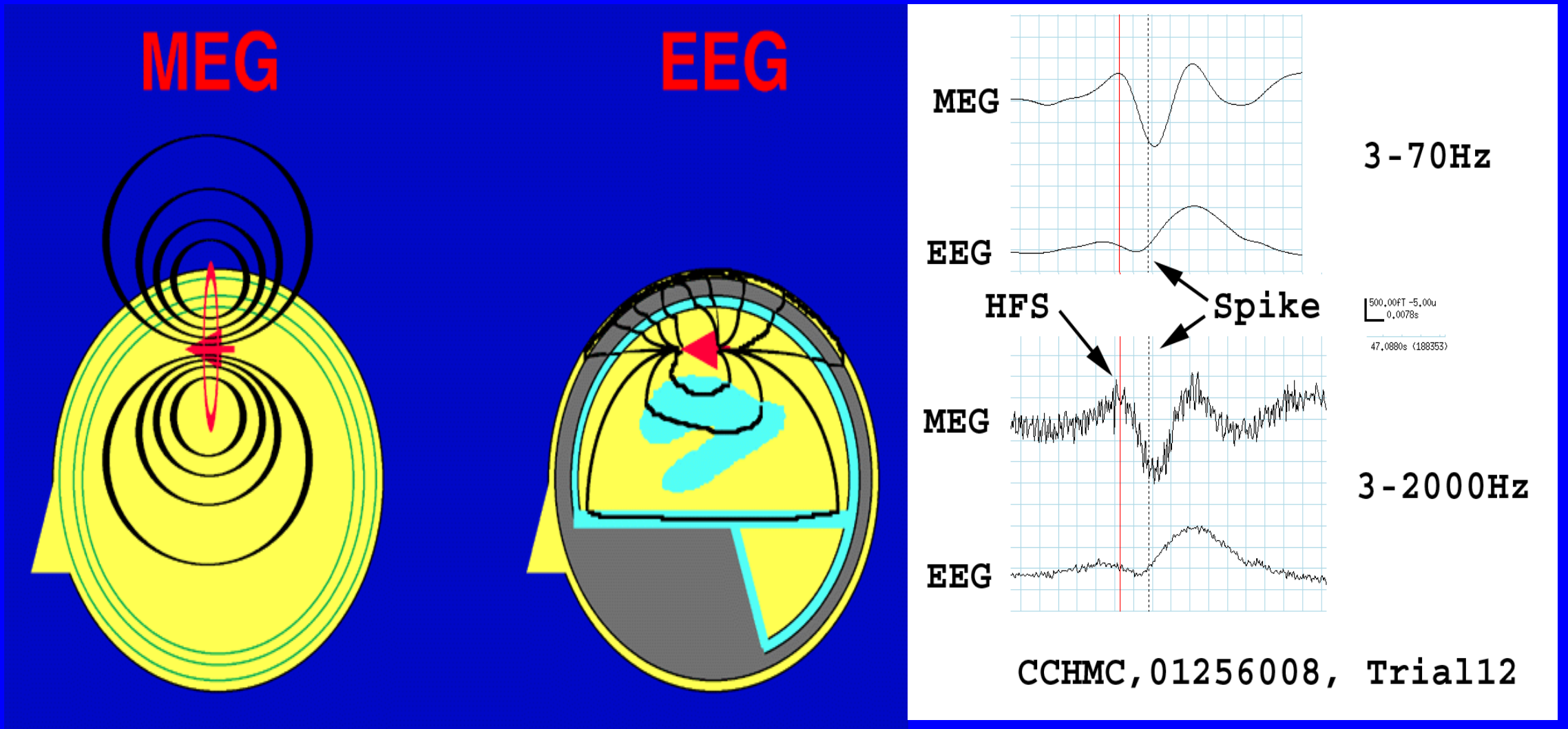
Neuroimaging Techniques for Recording HFBS



MEG \leftrightarrow EEG

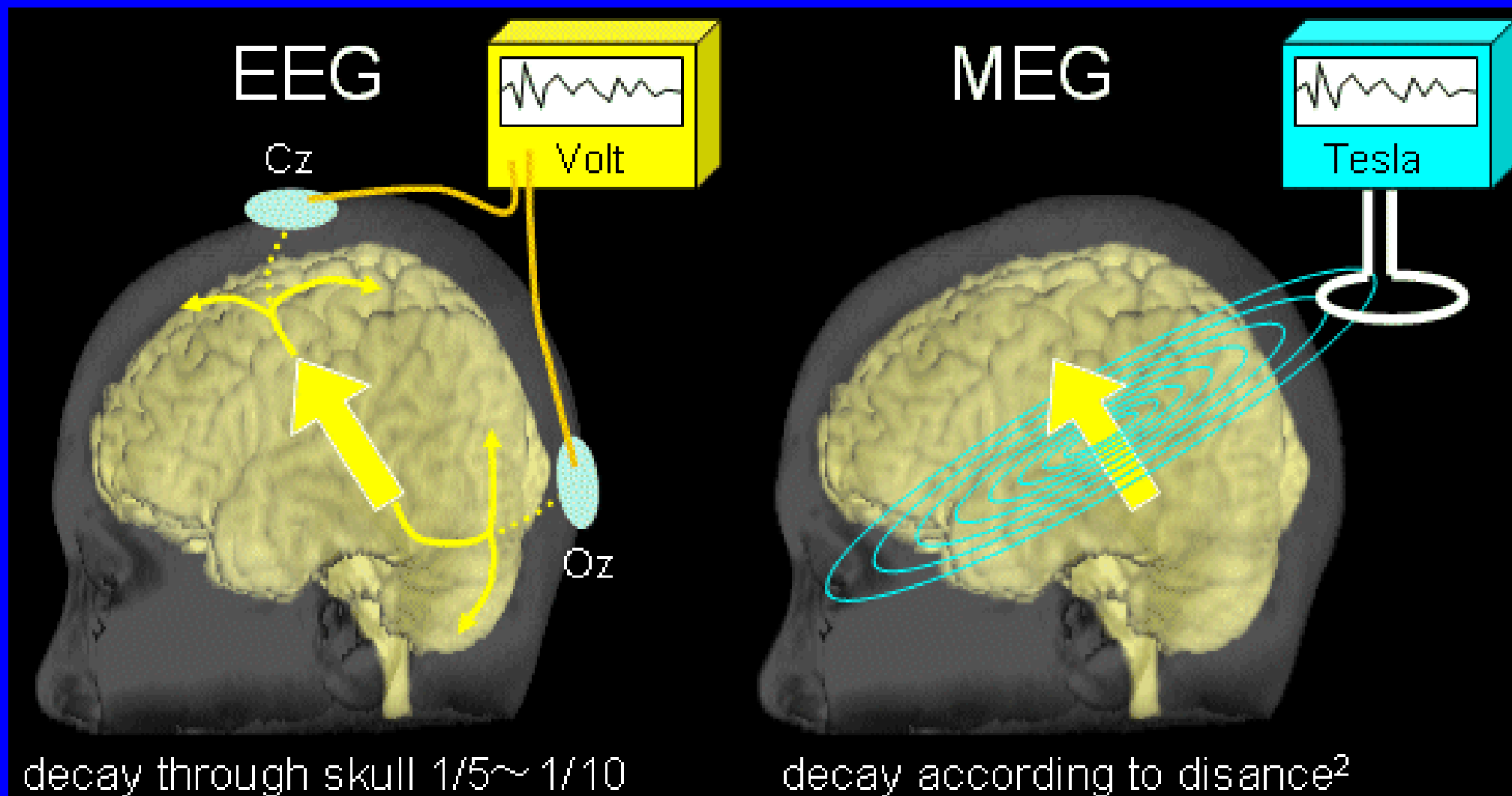


HFOs and MEG/EEG



- Skull and skin blocks much of the EEG high frequency signal. MEG passes through skull and skin unchanged.

MEG and EEG



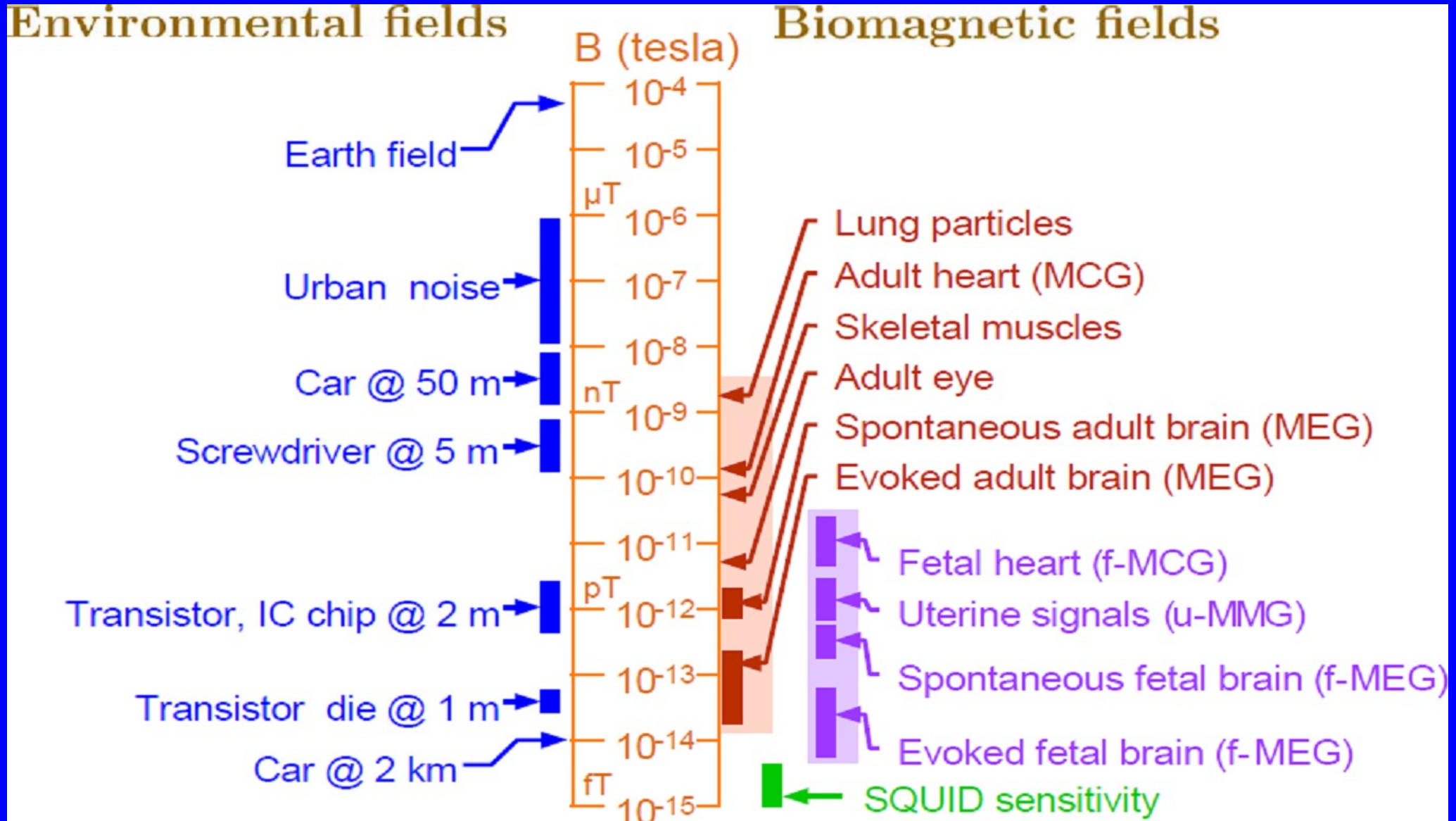
Parameters	MEG (Magnetic flux)	EEG (Electric current)
Original	intracellular	extracellular
direction	Perpendicular to current	Parallel to current
distortion	Not distorted as they pass through the brain tissue	Significantly distorted by brain tissue
resistance	Biological tissues offer practically No resistance to magnetic signals	Biological tissues offer resistance to magnetic signals
Generators	Tangential pyramidal neurons	Radial pyramidal neurons
formation	At least 50,000 neurons firing	At least 10,000 neurons firing
Spatial characteristics	Very close spatial neighboring Neurons firing	Spatial neighboring Neurons firing
Frequency effect	No low pass filter effect	Low pass filter effect
Spatial resolution	High spatial resolution	Low spatial resolution
Sensitivity to spikes	70% spikes similar to EEG, 20-30 different	70% spikes similar to EEG, 20-30 different
References	Practically no.	Yes, a set of montages
Record sensor direction	Magnetometers (coils, has direction)	Electrodes, no direction

Magnetometers are placed across the head surface	The shape of a brain activity source can be determined (in theory)	The shape of a brain activity source cannot be determined (in theory)
Source and distribution of magnetic flux	The depth of sources is well proportional to the distance between the extrema	The depth of sources may not be well proportional to the distance
Distance and source strength	Greatly affects the strength	affect the strength
Orientation and source strength	Greatly affects the strength	affect the strength
Orientation and sensitivity	Tangential sources	Radial (and tangential) sources
Brain structural and sensitivity	Sensitive parallel to surface of skull (e.g. along the sides of sulci)	Sensitive perpendicular to surface of skull (e.g. tops of gyri or at bottoms of sulci)
Spatial resolution	3-4 mm (or 1-2 mm in surface) at good condition	7-8 mm or worse
Price	Very expensive	Cheap

MEG and EEG

Frequency Effect	No low pass filter effect (Skull, skin and other tissues)	Low pass filter effect (Skull, skin and other tissues)
Spatial resolution	High spatial resolution Decay with distance significantly	Low spatial resolution Decay with distance slightly
Sensitivity to spikes	Tangential spikes/HFOs (MEG vs. EEG: 70% same)	Radial spikes/HFOs (MEG vs. EEG: 20-30 different)

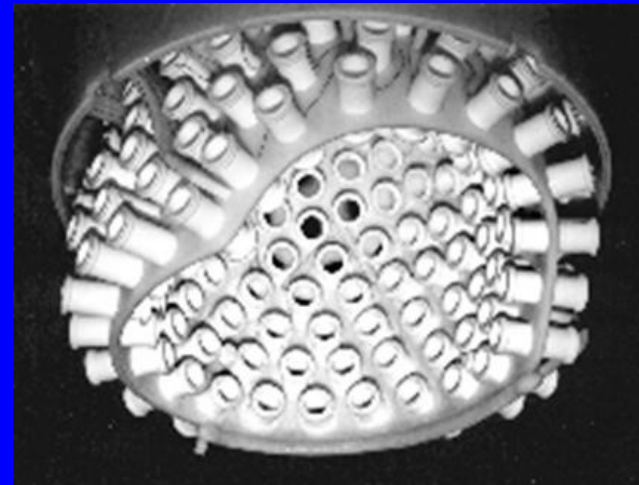
Biomagnetic Signals are Very Weak



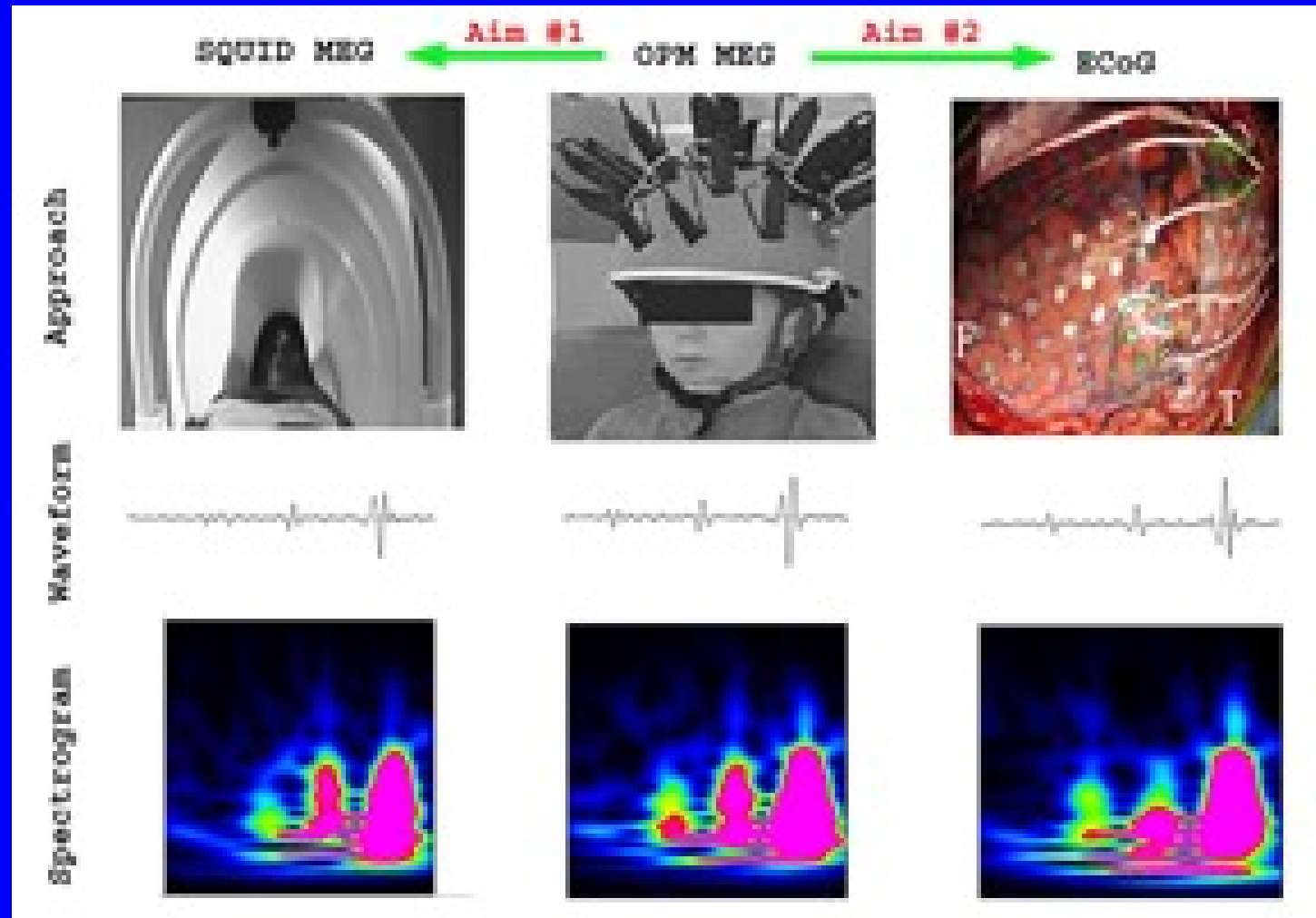
MEG System (Hardware)



- 275 MEG channels and 128 EEG electrodes
- Sampling rate is 12,000 Hz per channel.



New MEG Technology Detect HFOs



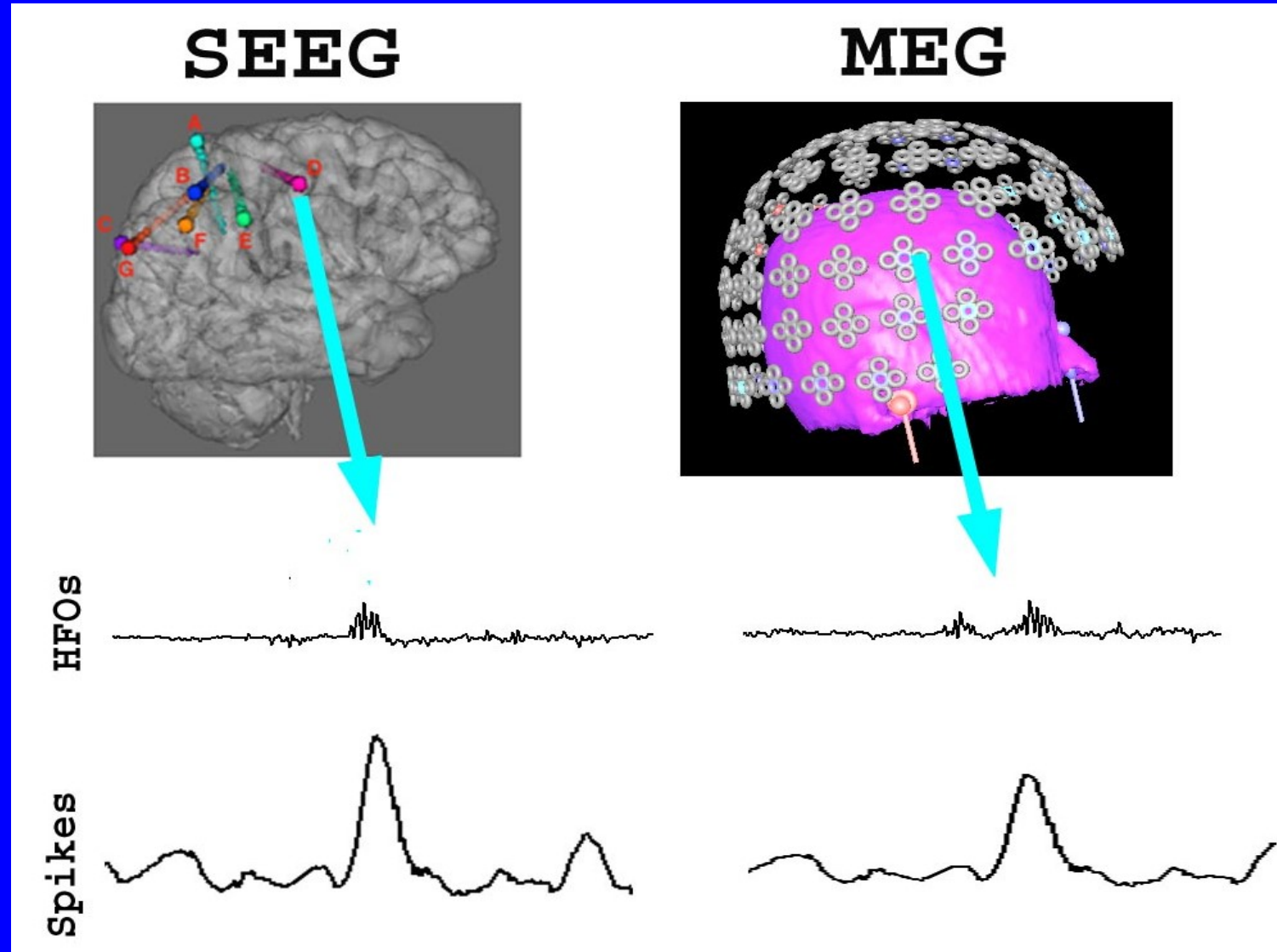
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Methods (1)

- A Set of manual or automatic methods have been developed for detecting HFOs
- Visual identification is the widely used method
 - one band-pass filter
 - Multiple band-pass filters
- Sensor levels:
 - Waveforms
 - Accumulated spectrogram (spontaneous)
 - Real-time Spectrogram (elicited)

HFOs at Sensor and Source Levels

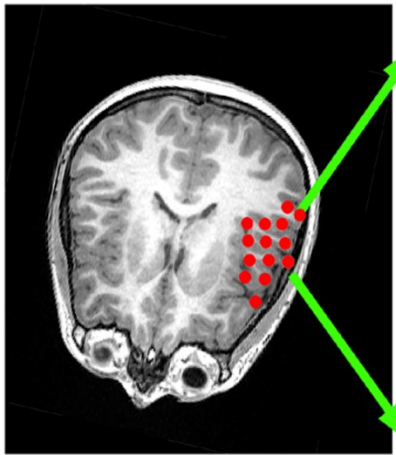


Methods (2)

- Detect HFOs at source levels
 - Precise spatial information
 - High signal-to-noise ratio
- Virtual Sensor
 - MEG virtual sensor waveform -> iEEG
 - MEG virtual sensor waveform->SEEG
- Source Imaging
 - MEG HFO source imaging ->iEEG sources
 - MEG HFO source imaging->SEEG sources

HFOs at Source Levels (Virtual Sensor) (waveforms)

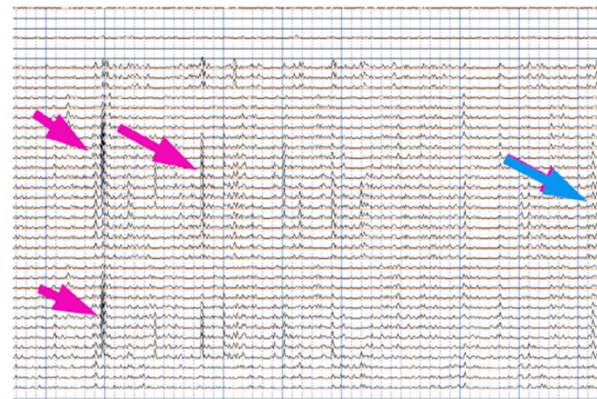
Epilepsy



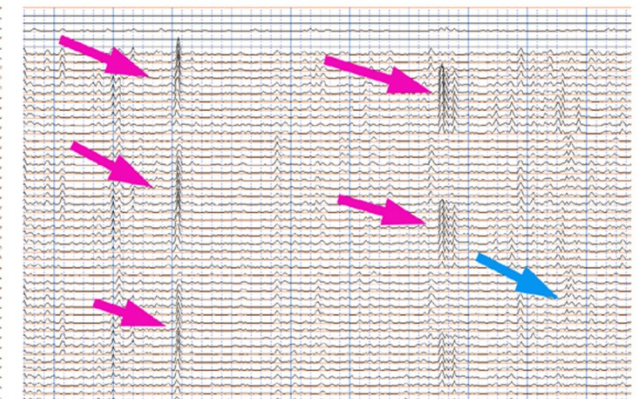
2-80 Hz (Spikes)



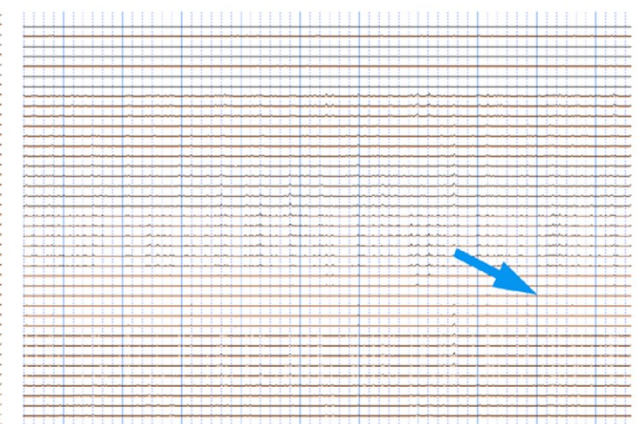
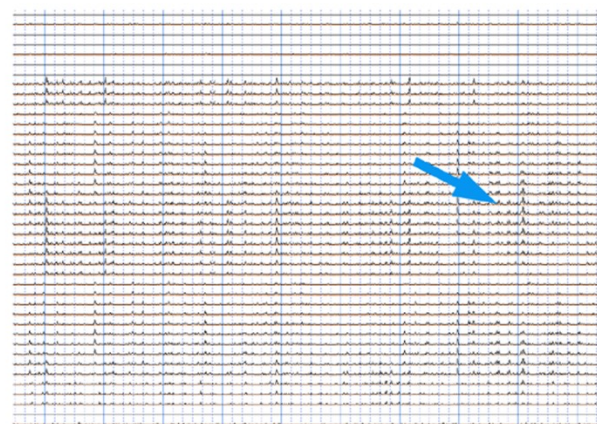
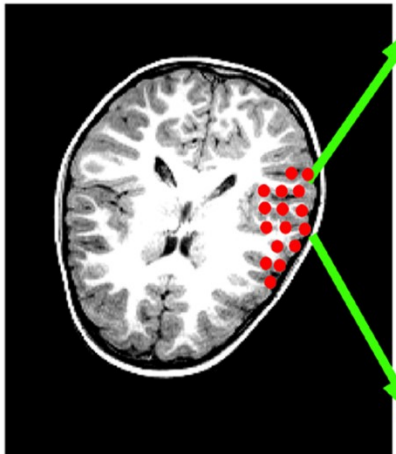
80-250 Hz (Ripples)



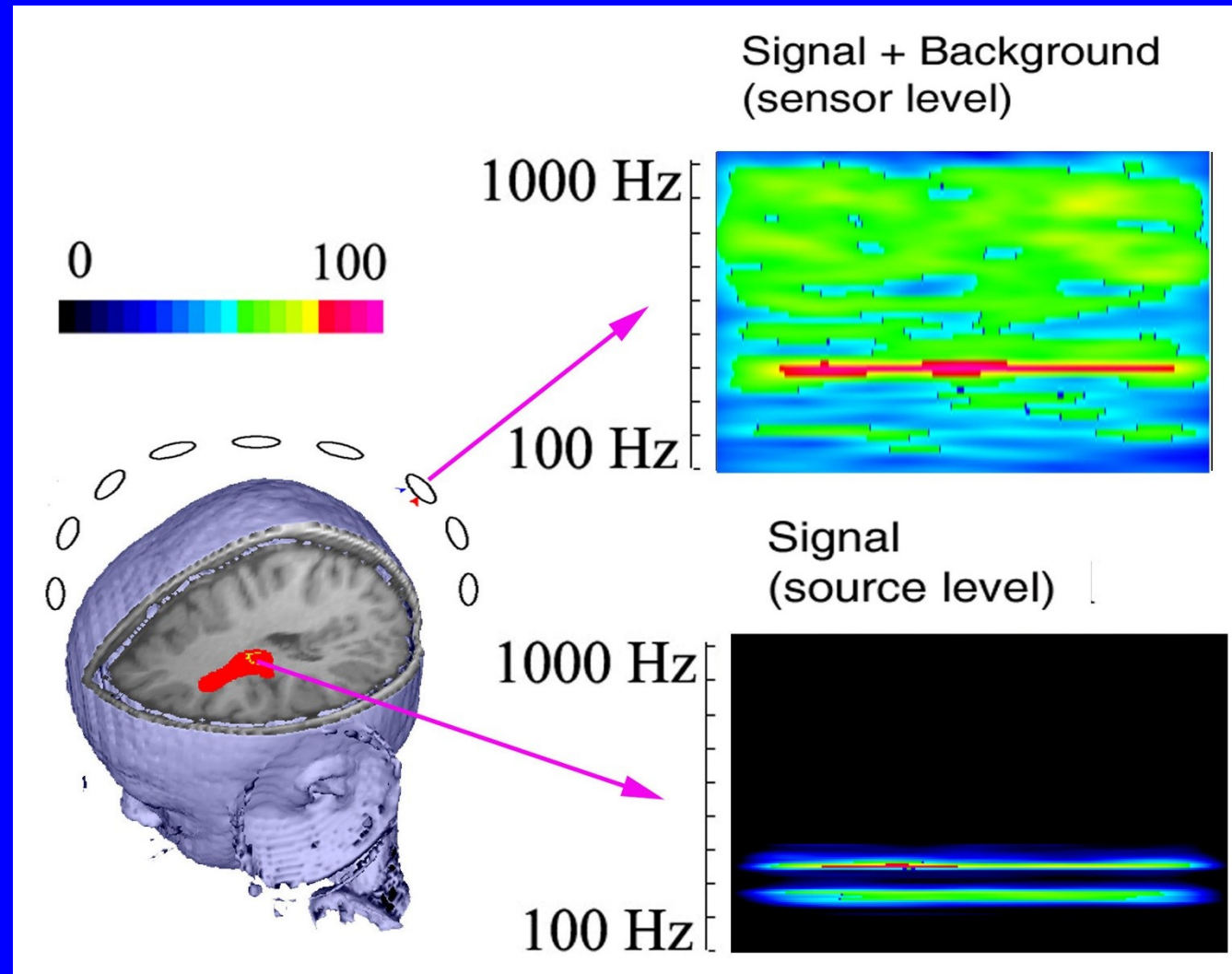
250-600 Hz (Fast Ripples)



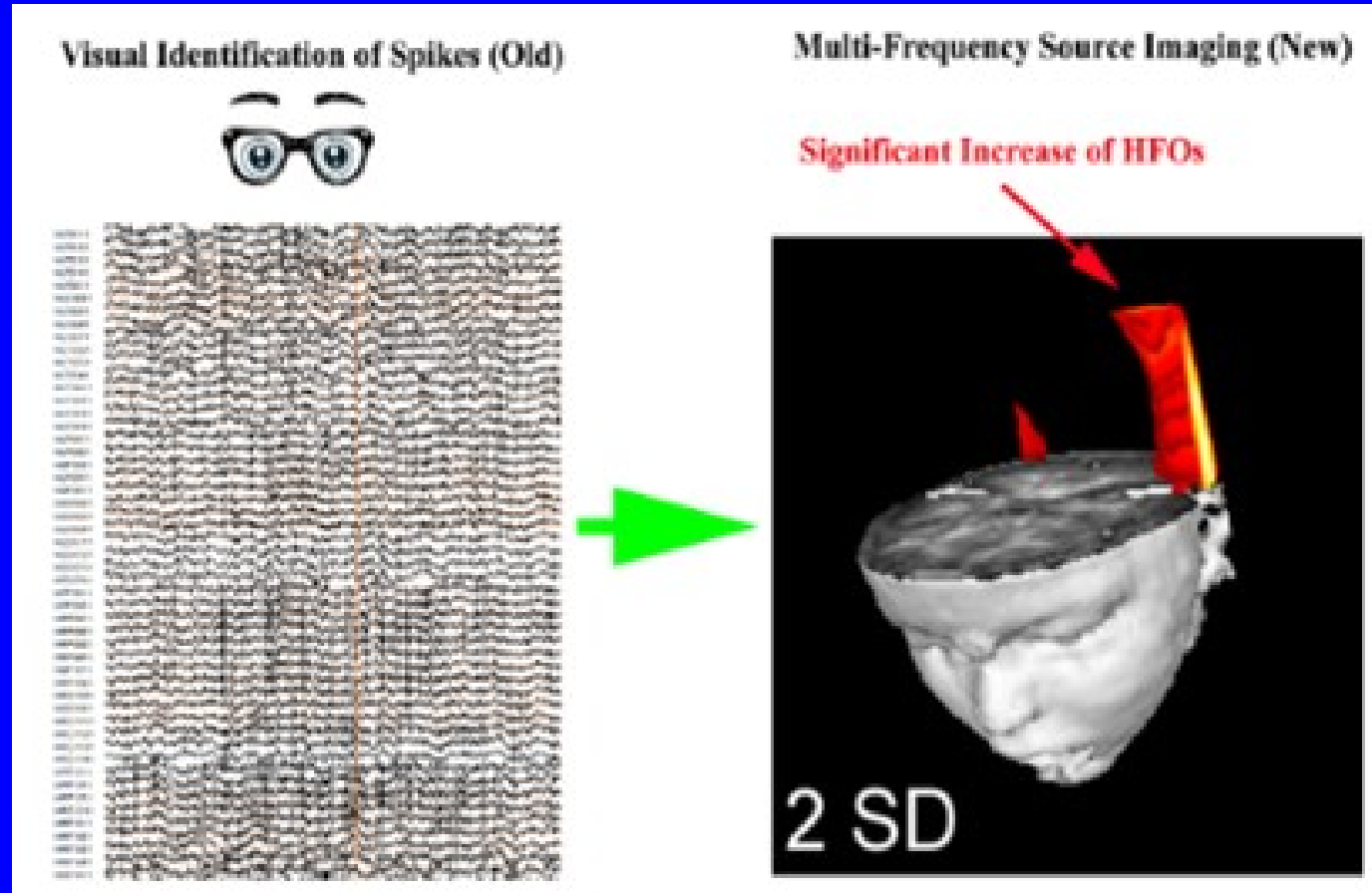
Normal



HFOs at Source Levels (Virtual Sensor) (spectrograms)



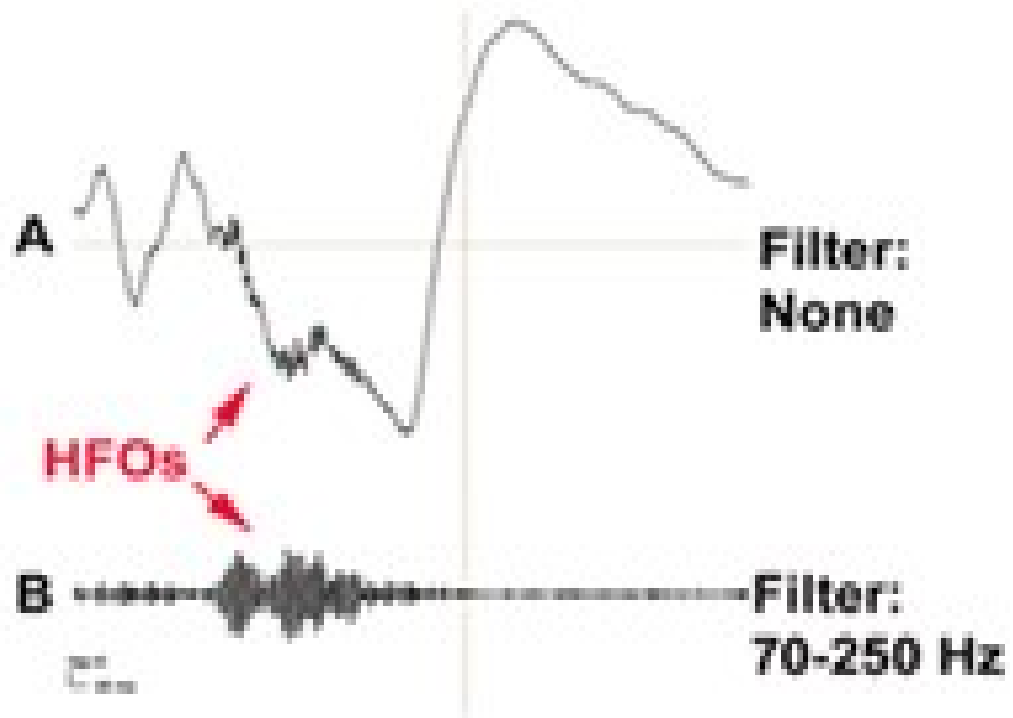
Detect and Localize HFOs with AI



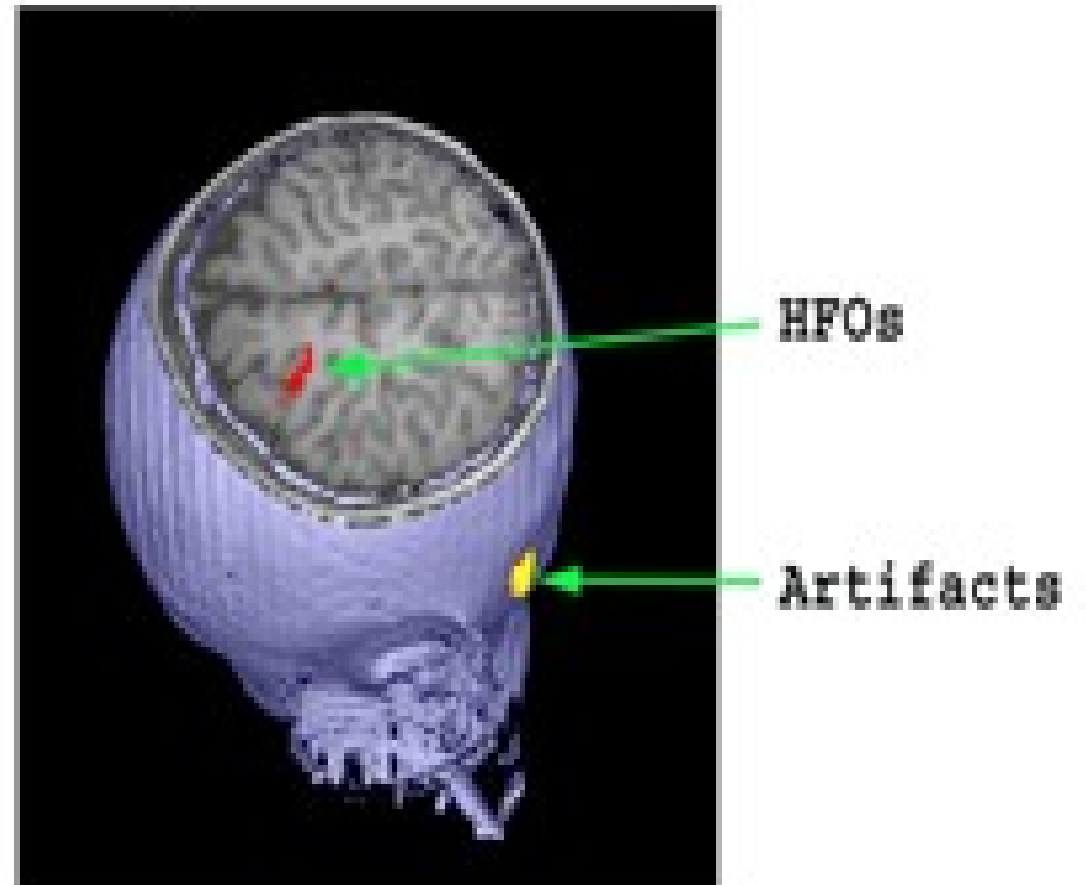
AI mark HFOs -> Volumetric Source Imaging

Separate HFOs from Muscle Artifacts

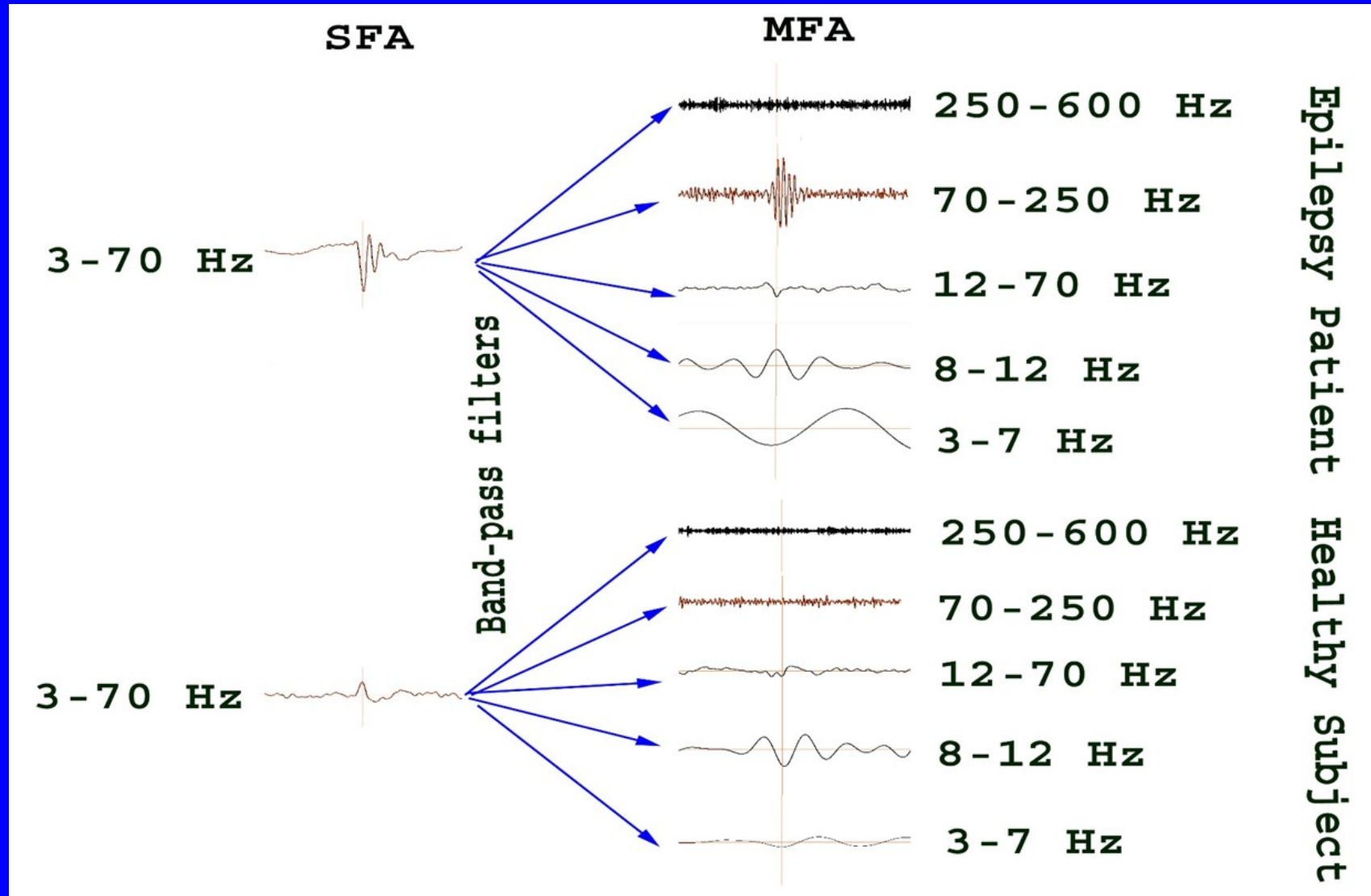
Digital Filter



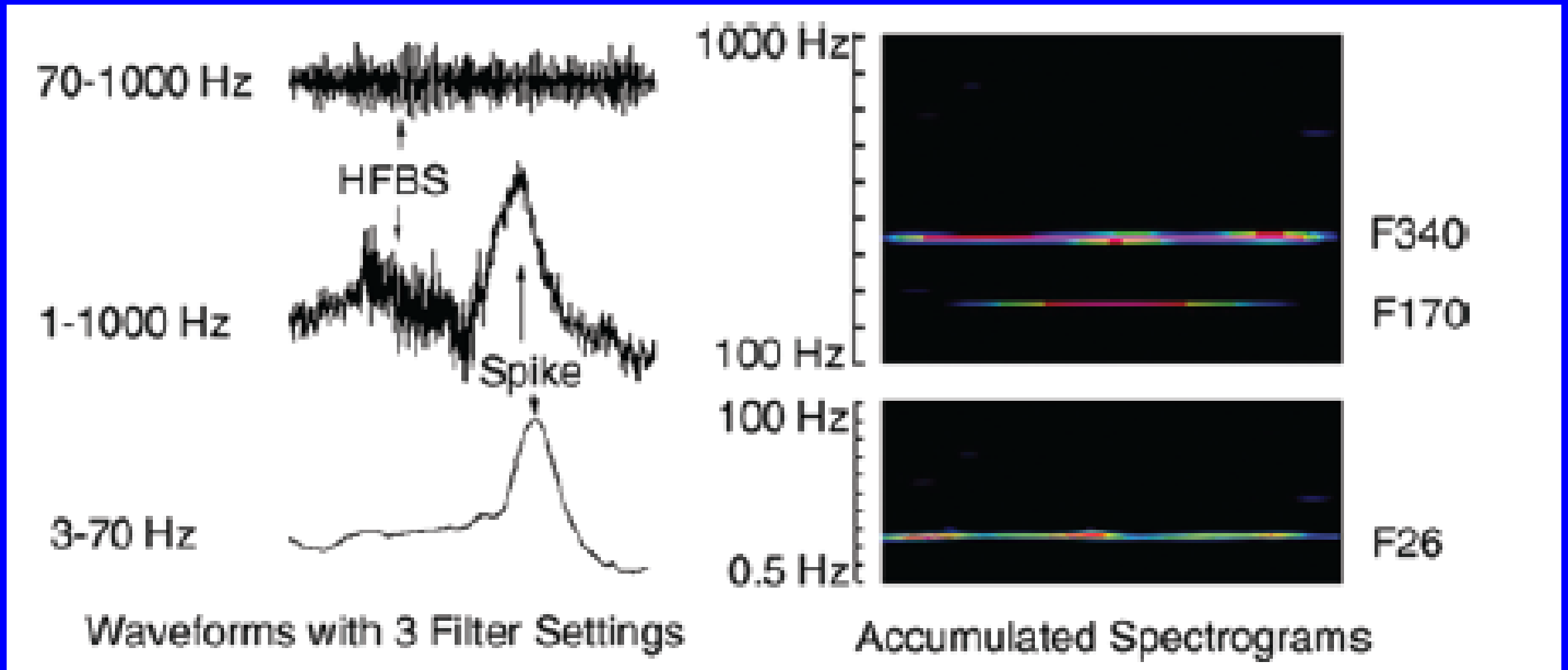
Spatial Filter



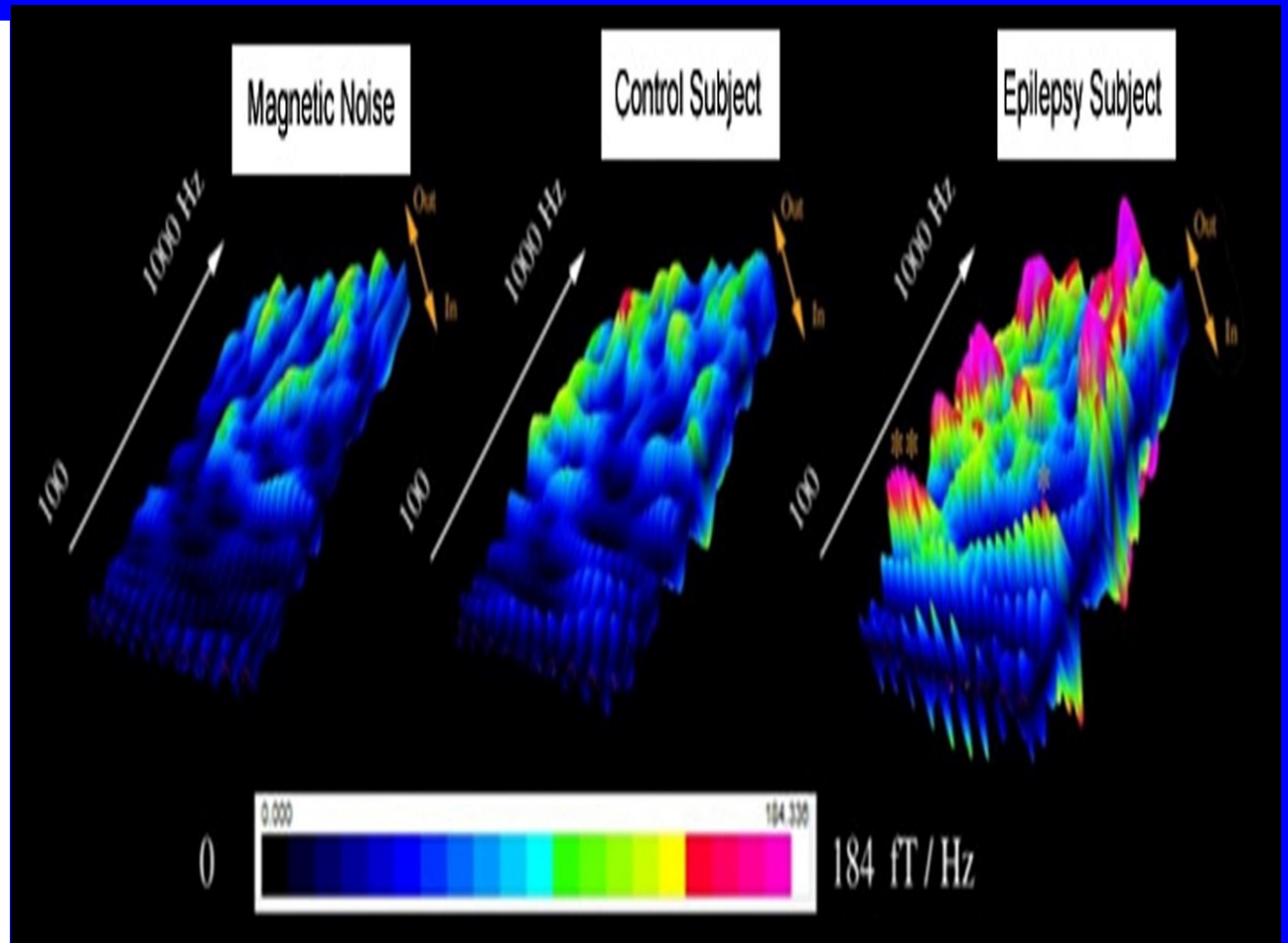
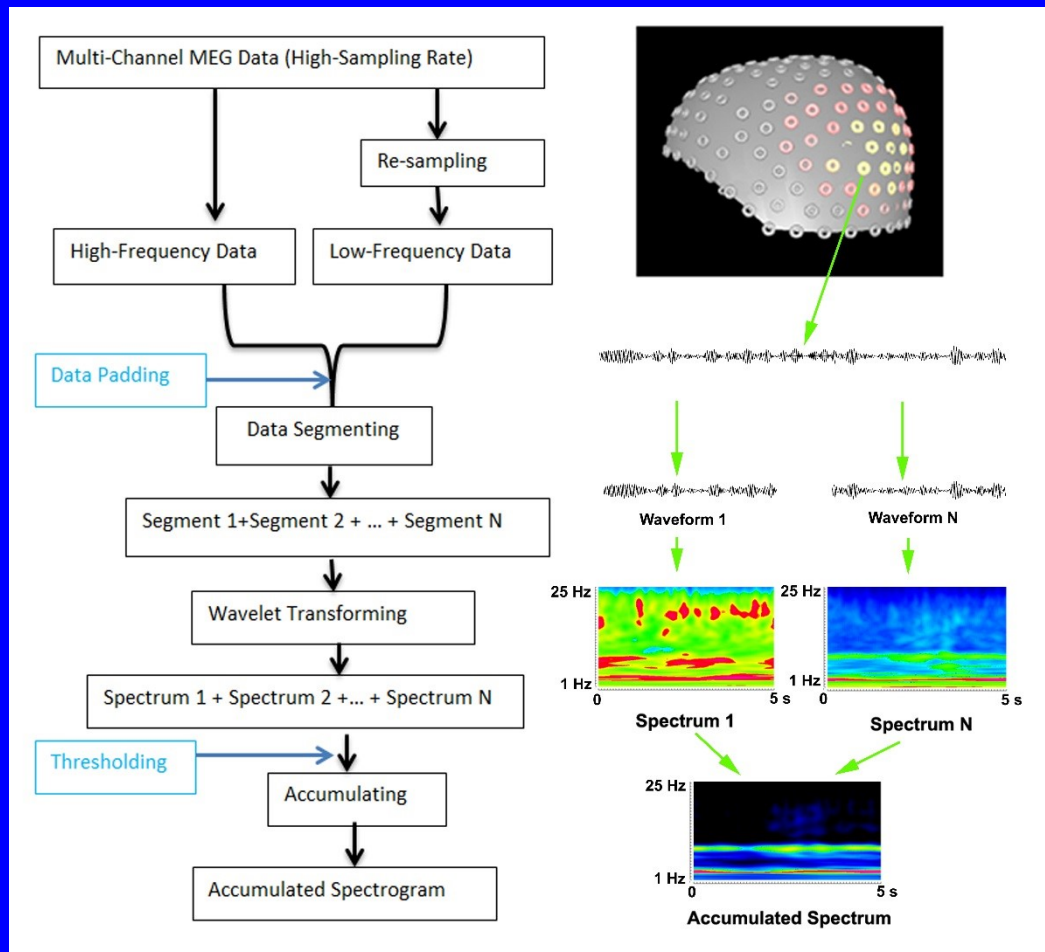
HFOs at Sensor Levels (Multi-Filters)



HFOs in Spectrograms (Precise Frequency)

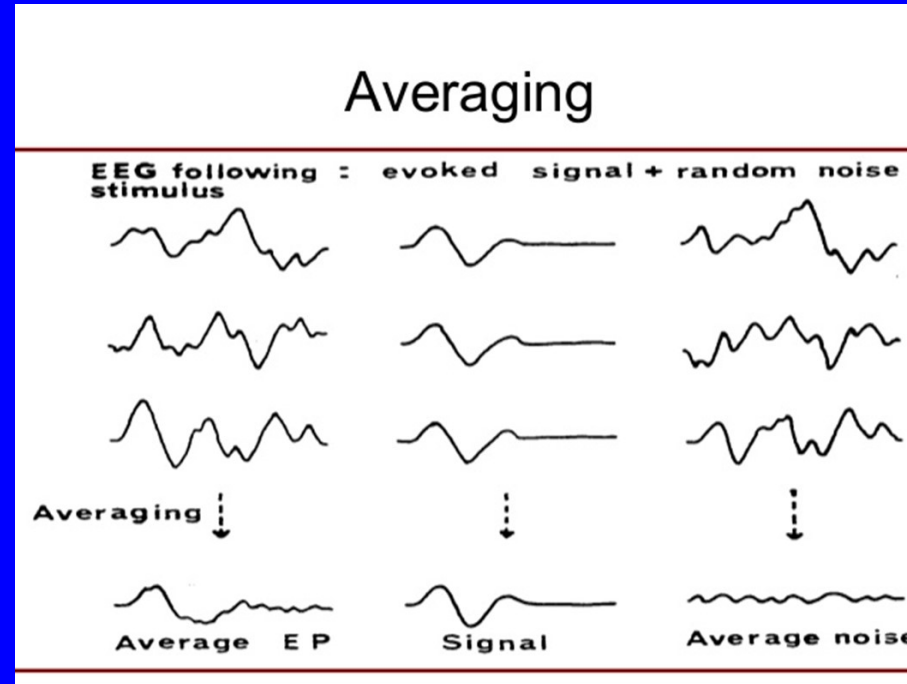
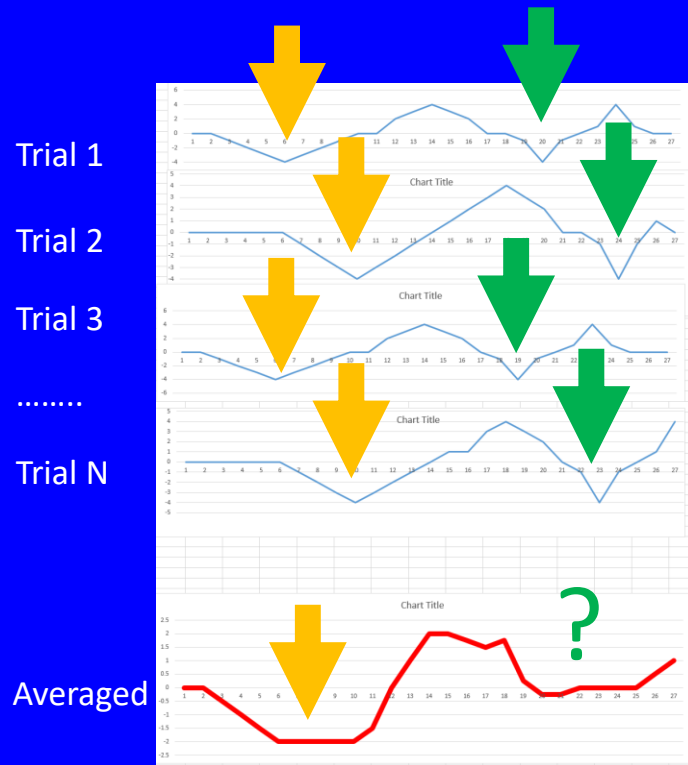


Accumulated Spectrogram (Effective)



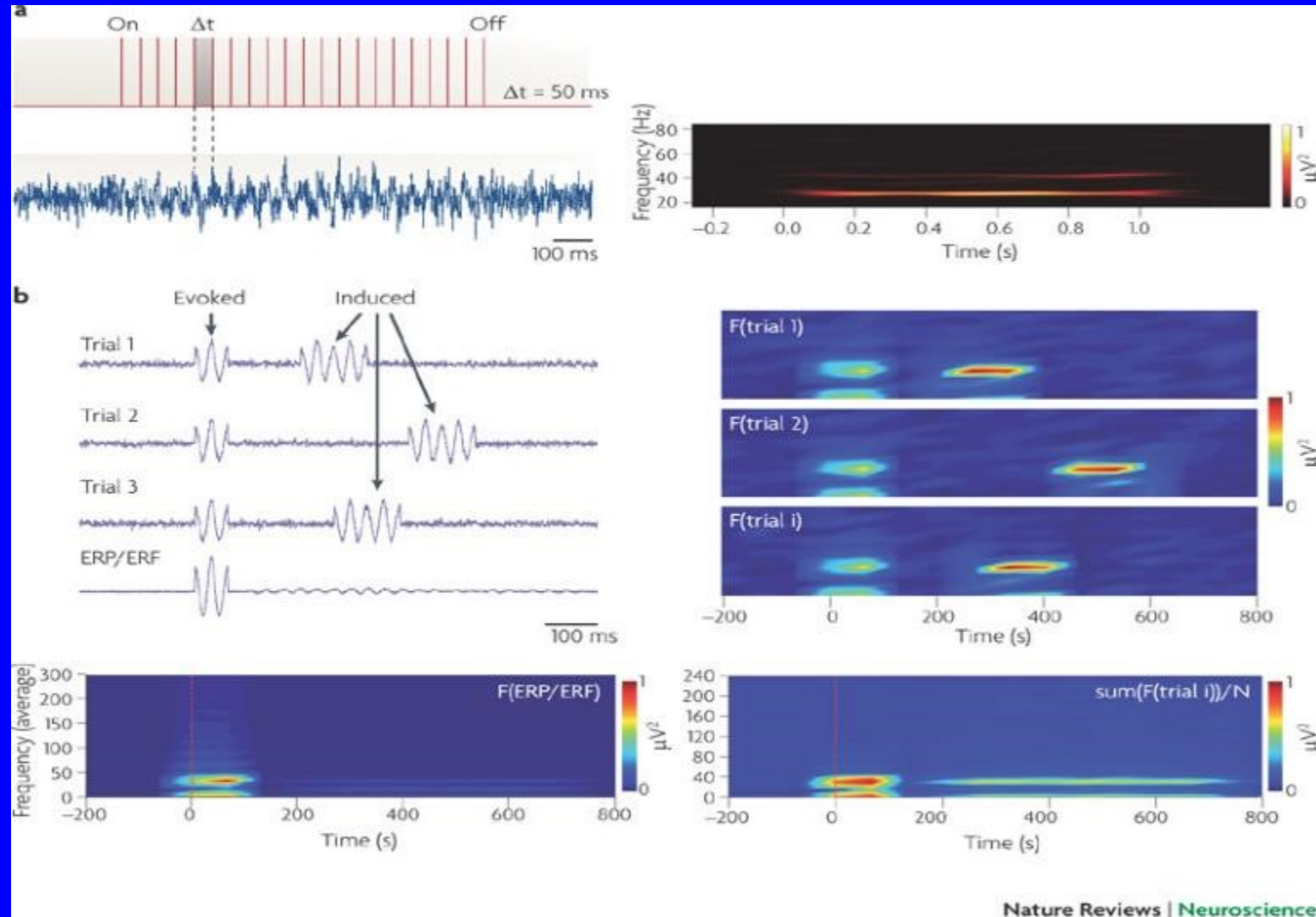
Visual Identification: subjective and time-consuming, Accumulated Spectrogram: objective and efficient (fast)

Functional/evoked HFOs (average vs. accumulation)

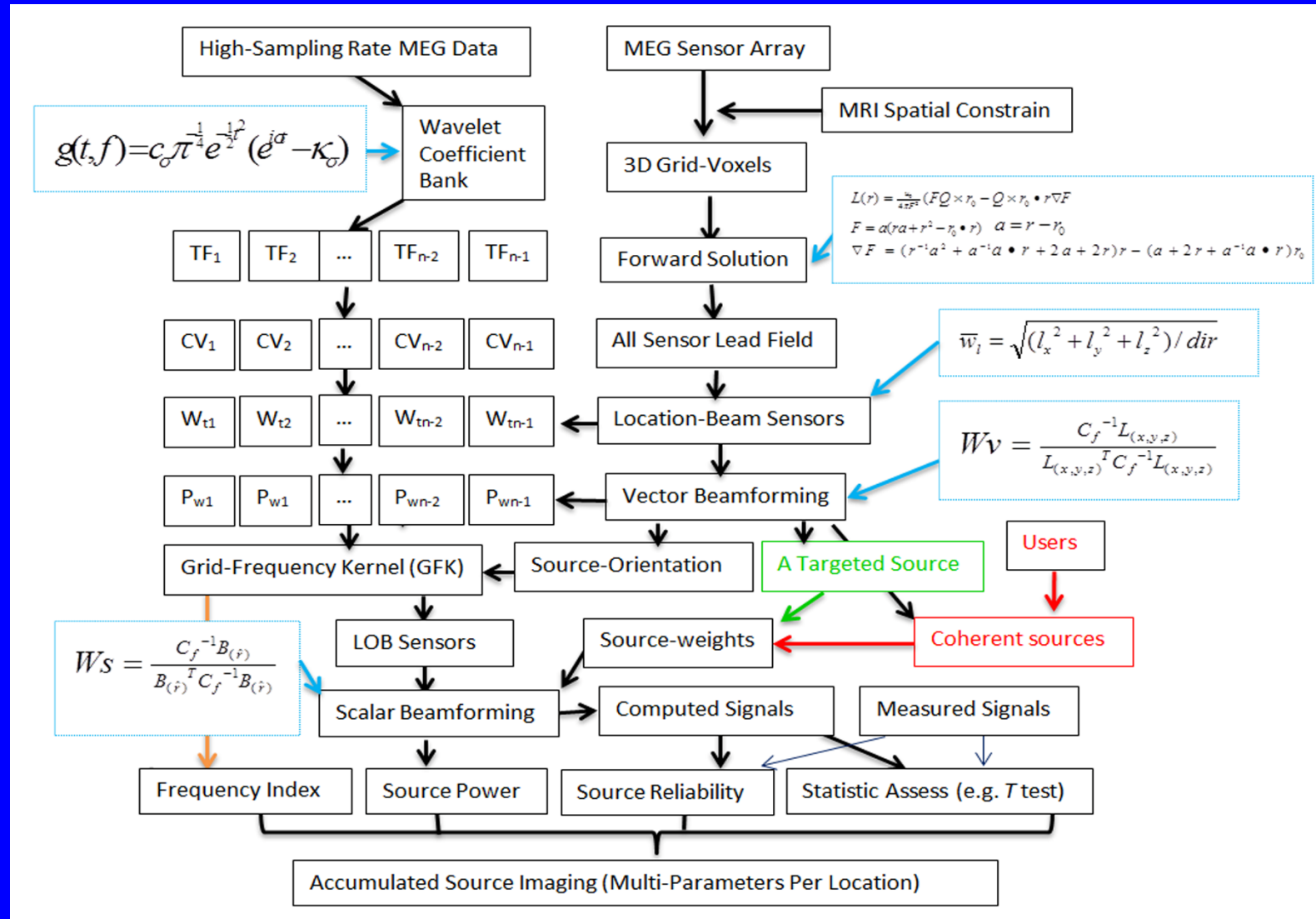


Latency variation of brain responses significantly affect s high frequency signals :
Low frequency components remain,
High frequency components disappeared

Functional/Elicited HFOs (accumulation)

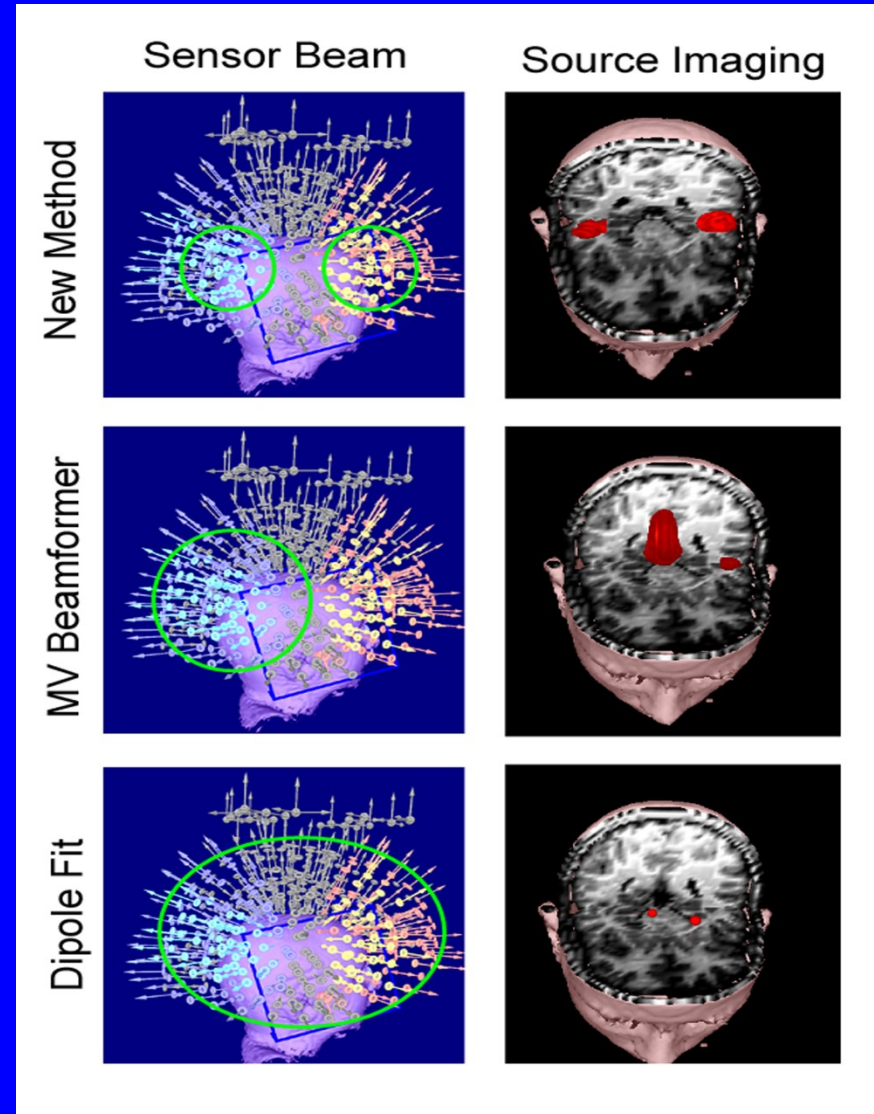


Accumulated Source Imaging (ASI)



Accumulated Source Imaging (2)

1. Increase the reliability by combining spatial filtering and accumulating.
2. Increase the accuracy by using two-step beamforming



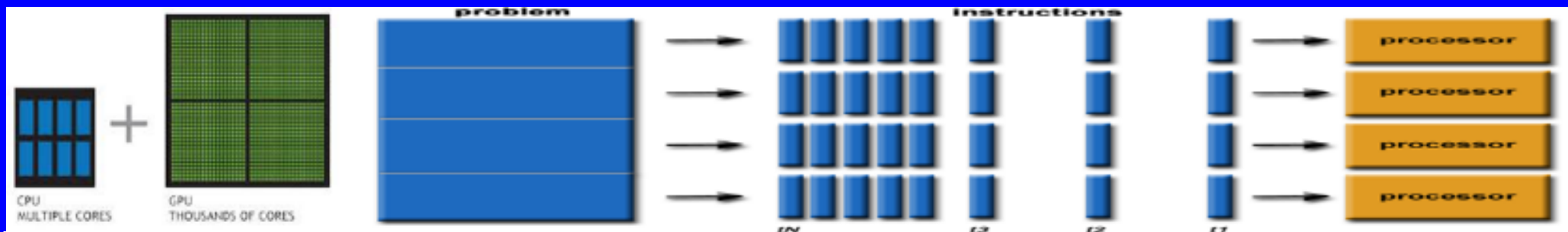
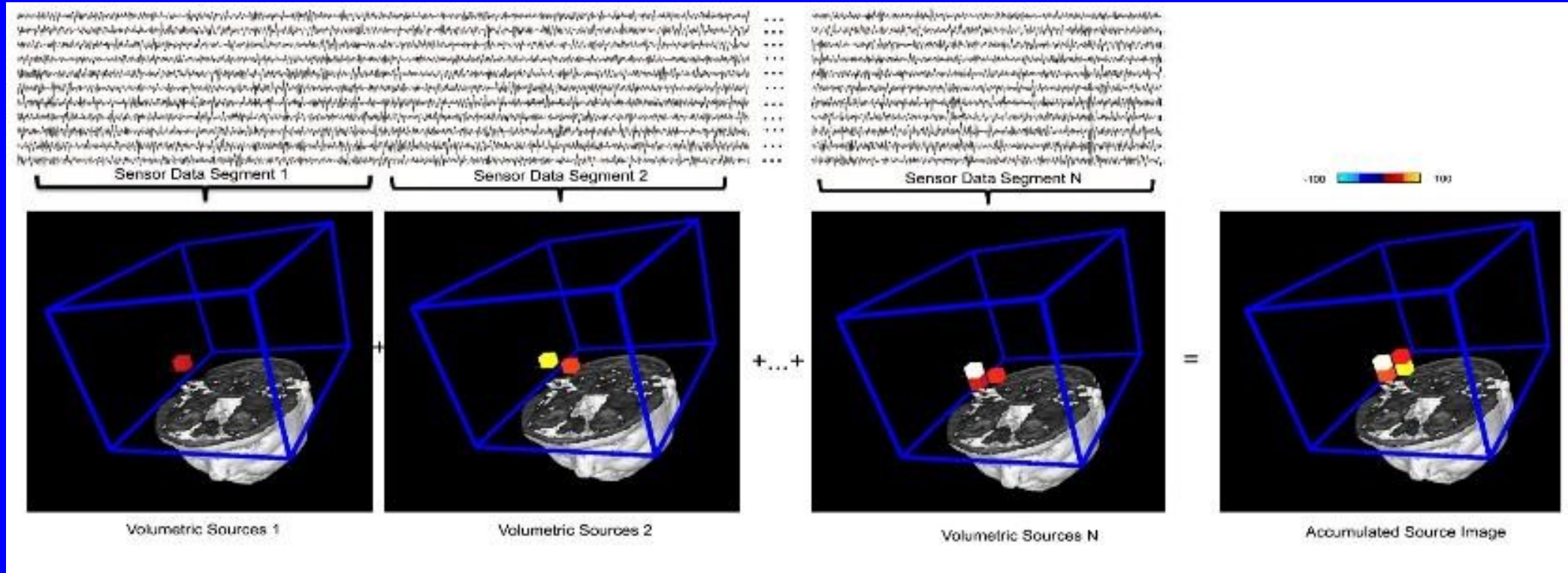
MEG Processor (One of the Best?)

Table . Differences between accumulated source imaging (ASI) and similar methods.

	ASI	DM	SAM	SAM(g2)	·BF	MN	MUSIC
Optimized for Localizing HFOs	Yes	No	No	No	No	No	No
Handle Large dataset	Yes	No	No	No	No	No	No
Handle multi-frequency signals	Yes	No	No	No	No	No	No
Multi-parameter per location	Yes	No	No	No	No	No	No
Volumetric source scan	Yes	No	Yes	Yes	Maybe	Yes	Yes
Detect dynamic sources	Yes	Yes	No	No	No	Yes	Yes
Detect stationary sources	Yes	No	Yes	Yes	Yes	No	No
Detect correlated sources	Yes	Yes	No	No	No	Yes	Yes
Noise suppression	Yes	No	Yes	Yes	Yes	No	Yes

ASI: accumulated source imaging; DM: dipole modeling (dipole fitting); SAM: synthetic aperture magnetometry; SAM(g2): SAM excess kurtosis (g2); BM: conventional beamforming; MN: minimum-norm; MUSIC: multiple signal classification

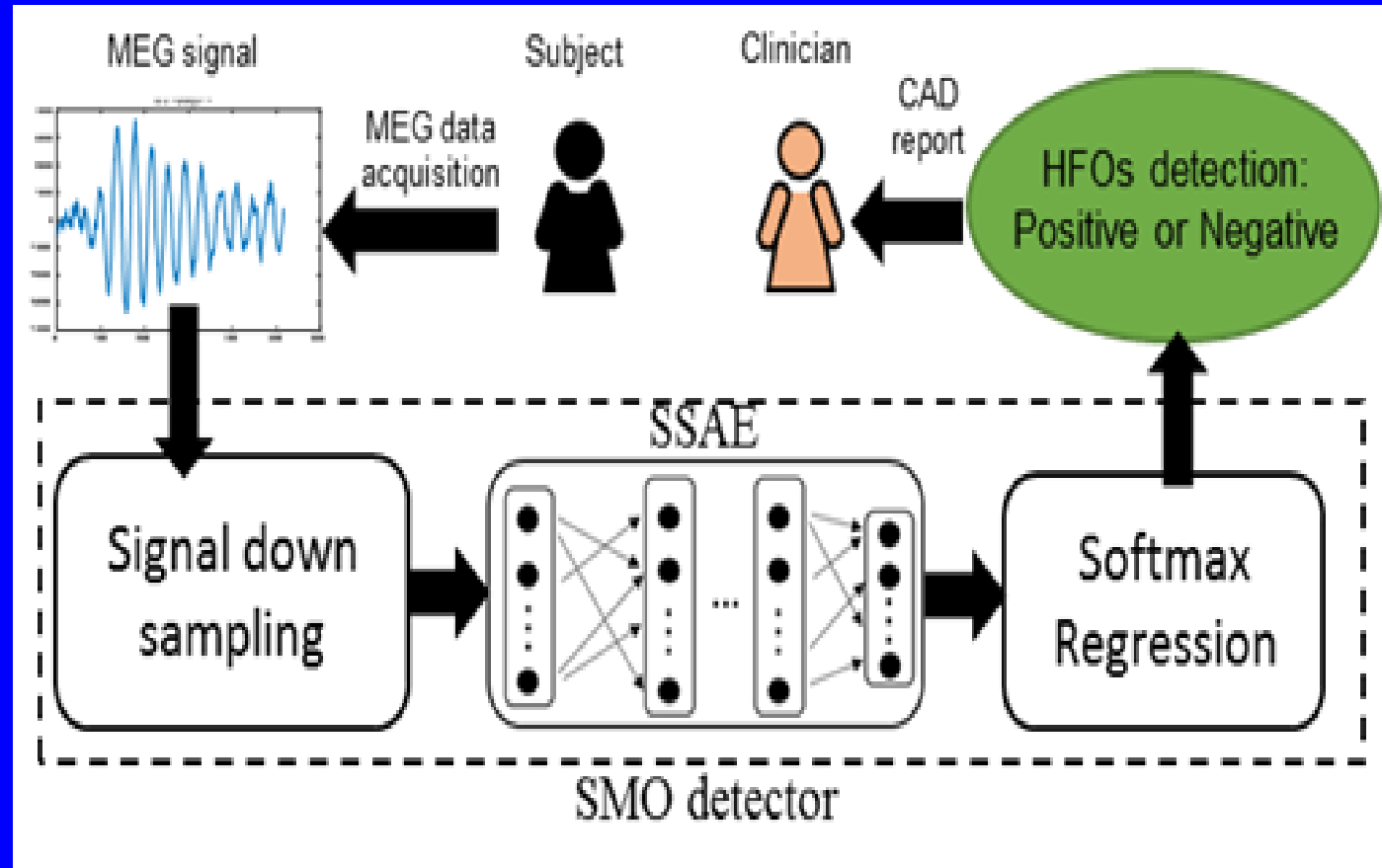
Accumulated Source Imaging



Methods (3)

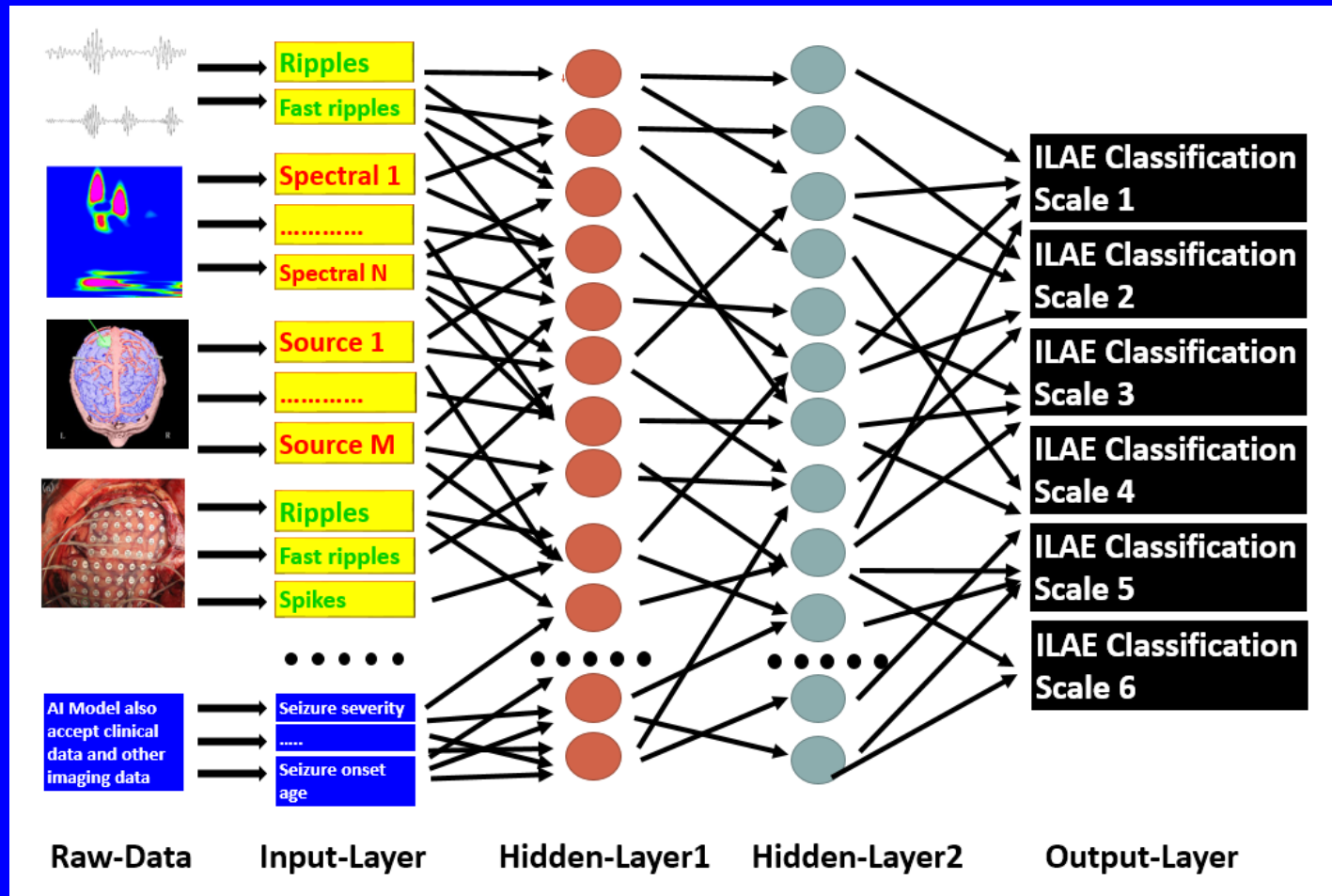
- Artificial Intelligence (AI):
 - Deep learning
 - Machine learning
 - stacked sparse autoencoder
- Other methods
 - Pattern recognition
 - Wavelets, Spectral power,
 - stationarity, and others

Automatically Detect HFOs with AI



stacked sparse autoencoder (SSAE)-> SSAE MEG Oscillation (SMO) Detector

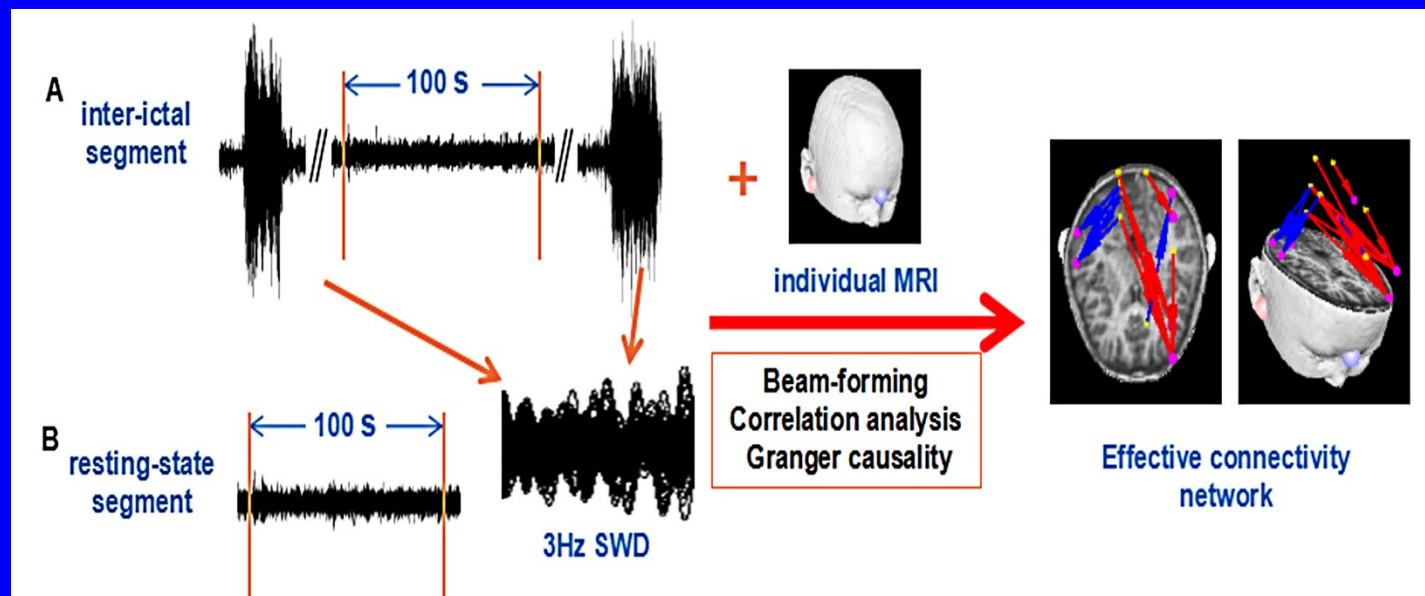
Automatically Detect HFOs with AI



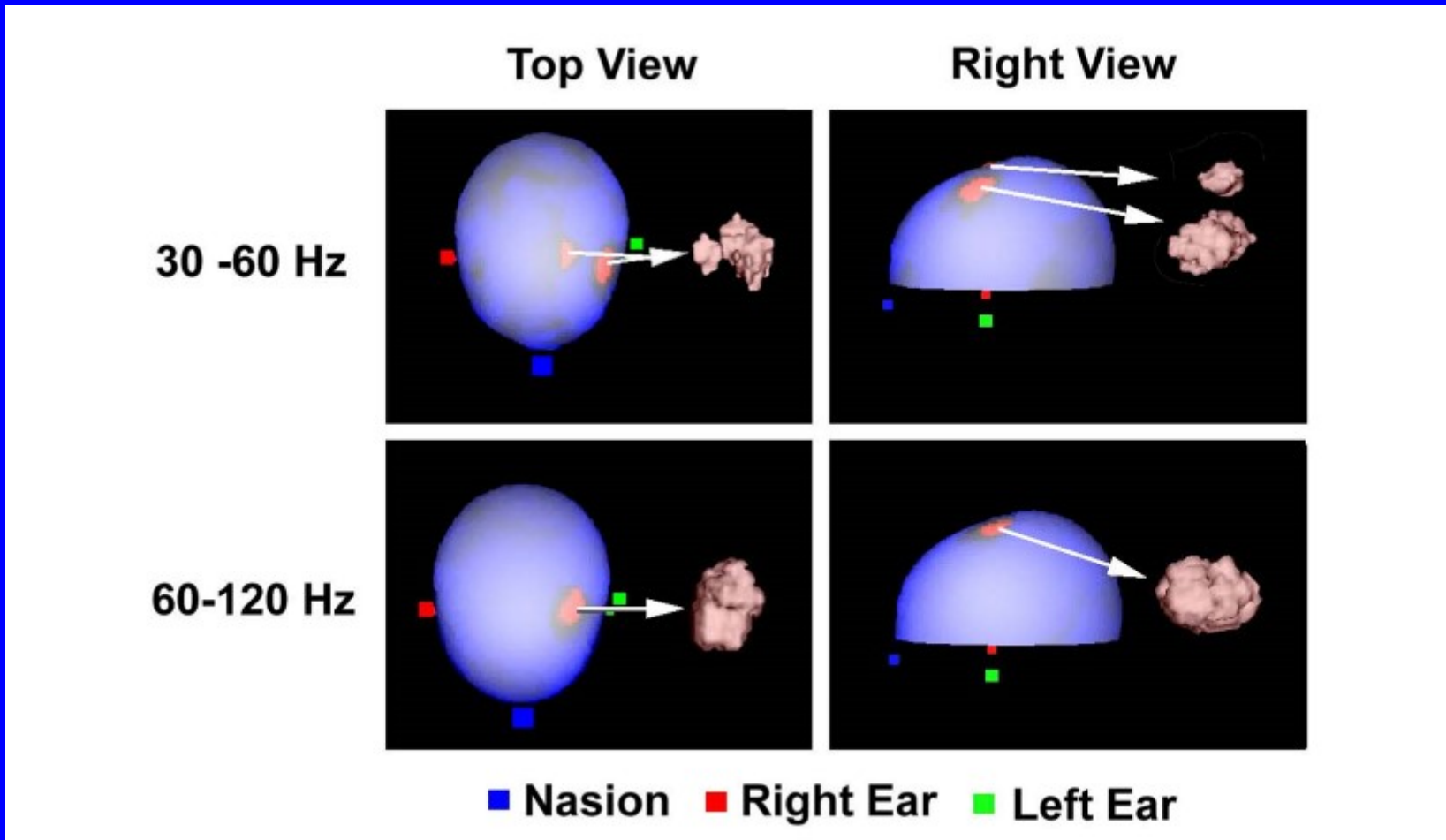
Methods (4)

- Advanced HFO technology
 - Frequency Encoded Source Imaging
 - Epileptogenicity Index
 - Frequency coupling
 - Frequency dependent networks
 - Others
-

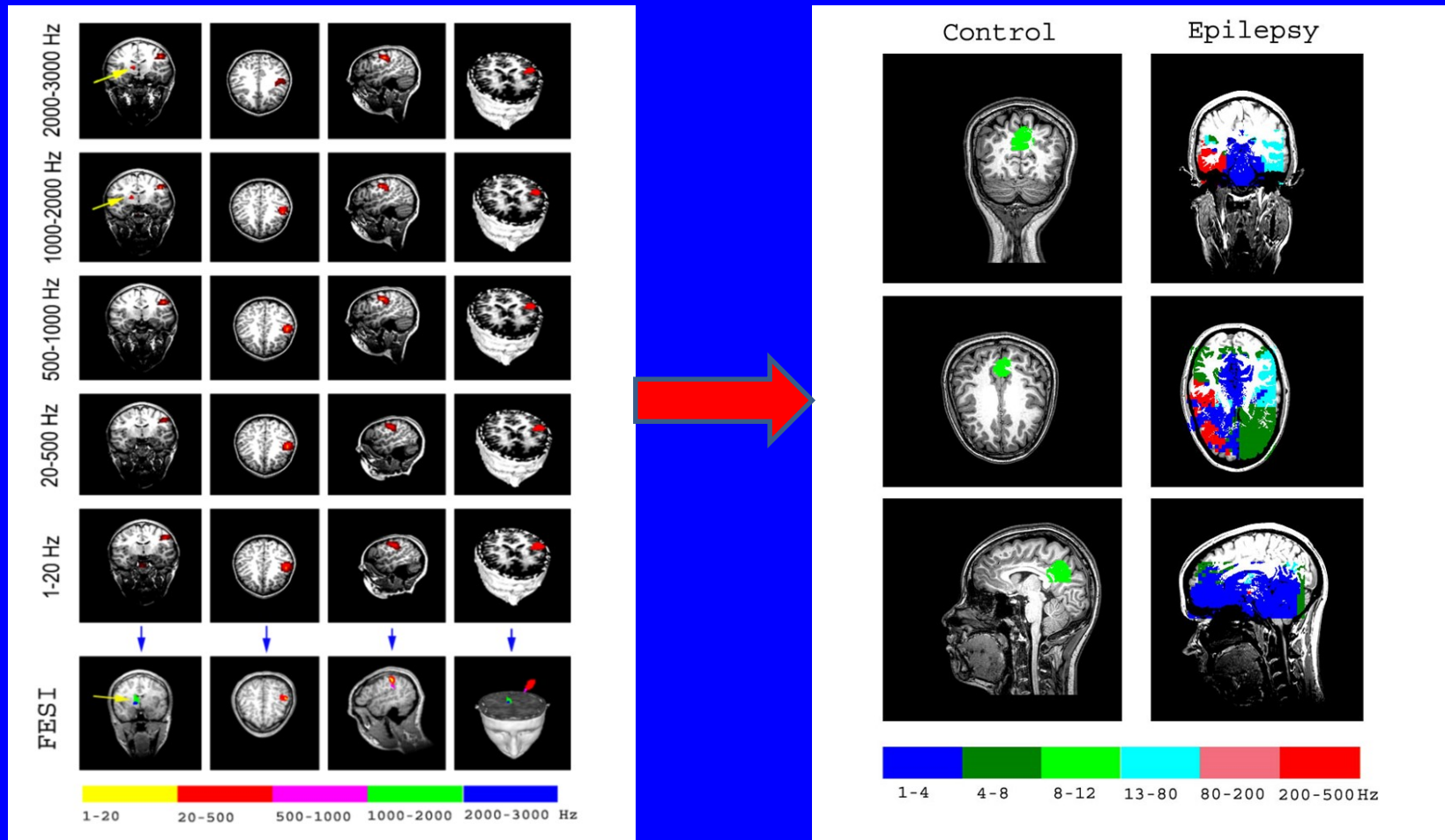
Neural Network Analysis



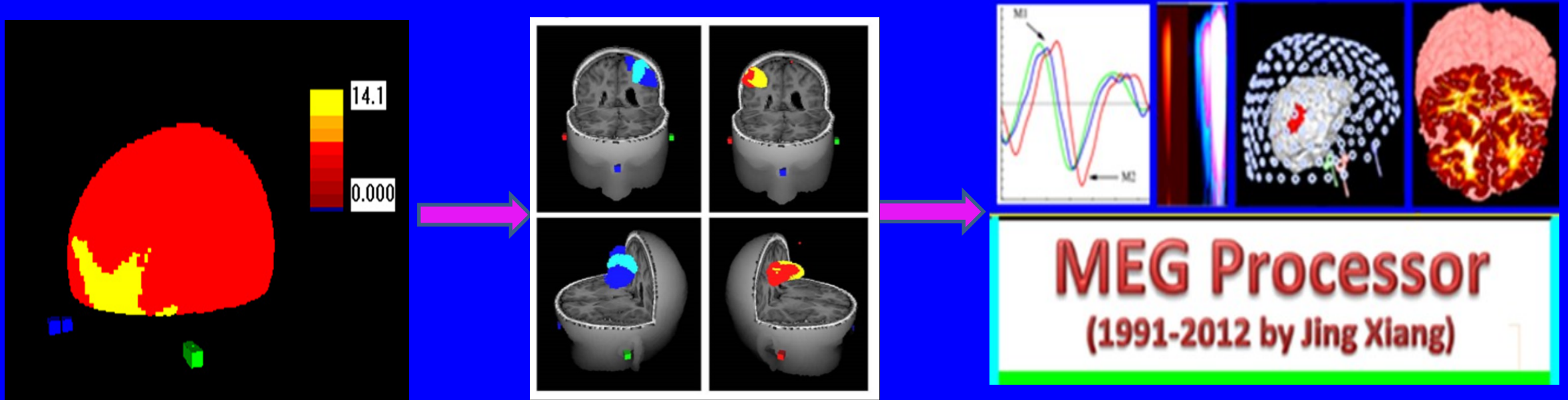
Volumetric Source Estimation



Frequency-Encoded Source Imaging(1)



Goal : Using All HFBS to Solve Clinical Problems



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Clinical Applications(Focus on 3)

Epilepsy (~800)

- Spike searching
- Presurgical planning
 - **Epileptic foci:** HFOs
 - **Functional mapping:** high gamma
- Generalized epilepsy
- Cortical organization
 - consequence of seizures
 - consequence of medication
 - relationship to co-morbidities
- Post-traumatic epileptogenesis
- Withdrawal of treatment
- Pharmacoresistance
- more...

Psychiatry (~275)

- Schizophrenia: high gamma
- Depression
- Anxiety
- OCD
- PTSD
- Drug effects: new drug targeted at HFOs

Other Neurological Diseases (~450)

- **Migraine**
 - **Acute :** HFOs
 - **Chronic:** HFOs
- Normal Aging
- Mild cognitive impairment
- Alzheimer's
- Cerebrovascular disease
- Functional reorganization
- Multiple sclerosis
- Tinnitus
- Migraine and Headache
- Traumatic Brain Injury
- Brain Tumor: HFOs

Neurodevelopment (~200)

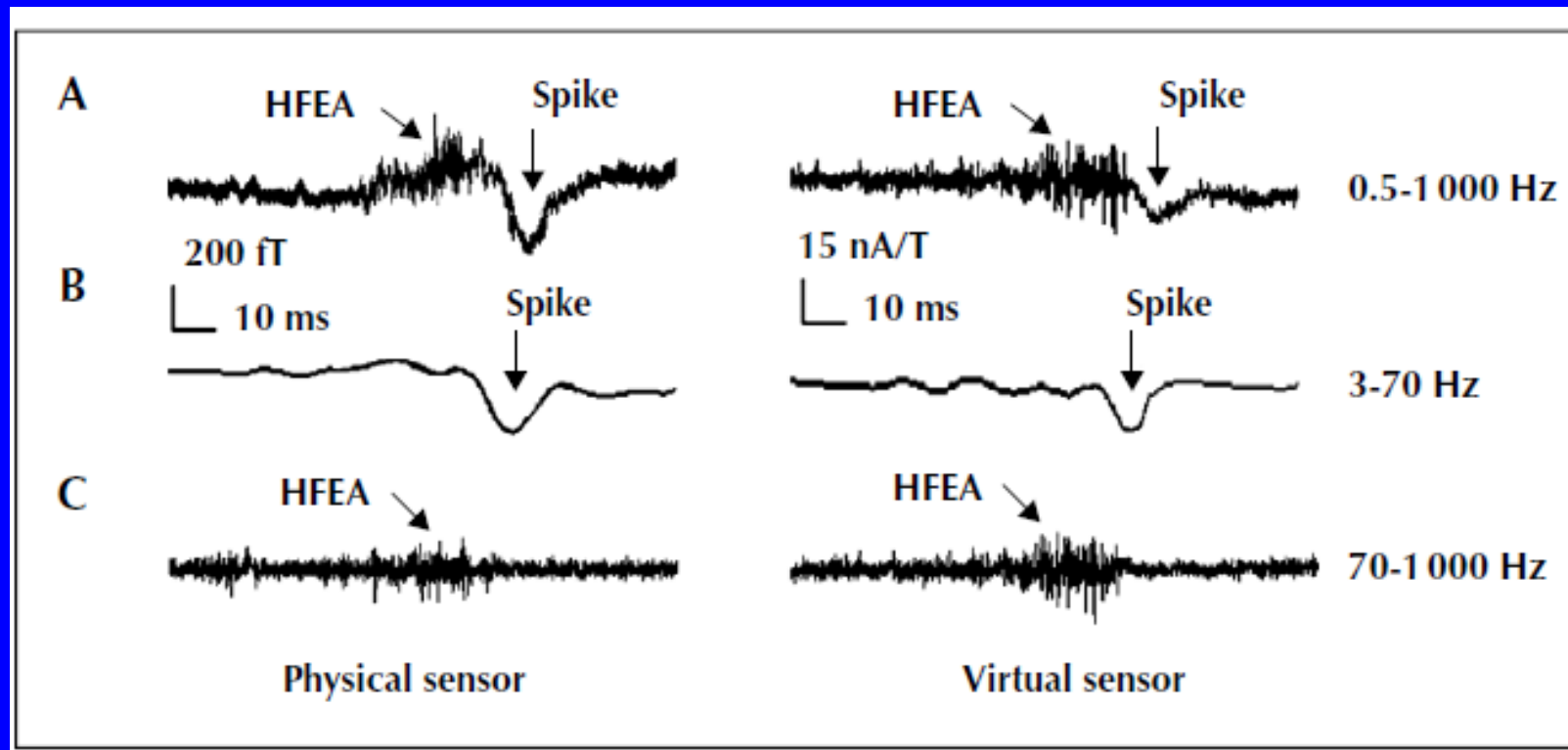
- Fetal
- Neonatal
- Autism: high gamma
- ADHD
- **Functional (re)organization**
- Brain Tumors

	Epileptic HFOs	Physiological HFOs	Artificial HFOs*	
Waveforms	Oscillations	>4	>4	
	Amplitudes	>1.5 SD of baseline†	<1.5 SD of baseline†	>10 SD of baseline
	Overlap on spikes	Yes†	No	No
	Ride on slow wave	Yes†	No	No
	Visible in both raw and filtered data	Yes†	Yes	No
	Inter-event interval	>25 ms	>25 ms	any
Spectrograms	Time	Irregular burst, 5-30 ms	Rhythmic, ~70 ms	Random/constant
	Frequency	80-250 Hz (ripples); 250-600Hz (fast ripples); 600-2500 Hz (HFOs)	Elicited: 70-150 Hz Endogenous: 102 Hz	< 100 Hz >2500 Hz 60 Hz or 50 Hz
	Pattern	Isolate island or horizontal	Connected or vertical	Straight lines
	Power	Very high power > 3 μV	Low median power -0.95 μV	Fixed
	Ratio (HFOs/alpha)	>0.30†	<0.27*	>4.0*
Source Imaging	Location	Within the brain (cortex, gray matter)	Within the brain (cortex, gray matter)	Out of the brain (around neck, eyes)
	Source strength	>3 SD of the global mean	> 1 SD of the global mean	> 10 SD of global mean
	Pattern	Peak with propagated activation	Activation without clear peaks	Typically irregular
	Relation to MRI/CT	Mimic anatomical shape	Mimic anatomical shape	No relation
Networks	Hub Location	Within the brain	Within the brain	Out of the brain
	strength	Increased*	Normal*	No connection
	Clustering index	Increased*	Normal*	Not available
Modulation	Path	Shortened*	Normal*	Not available
	NREM Sleep	Decrease*	No change*	No change
	REM Sleep	No change*	Ripple increase*	No change
	Sleep stage	Large extent (NREM)*	Small extent (REM)*	No change
	Sleep cycle	High rate in first cycle*	Low rate in first cycle*	No change
	Task induced	No*	Yes*	No
	Sleep time	Decrease with time during NREM	Increase with time during REM	
Clinical Correlations	High rates in SOZ	Yes*	No*	No relationship
	Increase with Seizure frequency	Yes*	No*	No relationship
	Anti-epileptic drug	Reduce HFOs	No	No relationship
	Removal HFO foci	Good surgical outcomes	No	No relationship
	Hyperventilation	Elicit HFOs (absence epilepsy)	No	No relationship

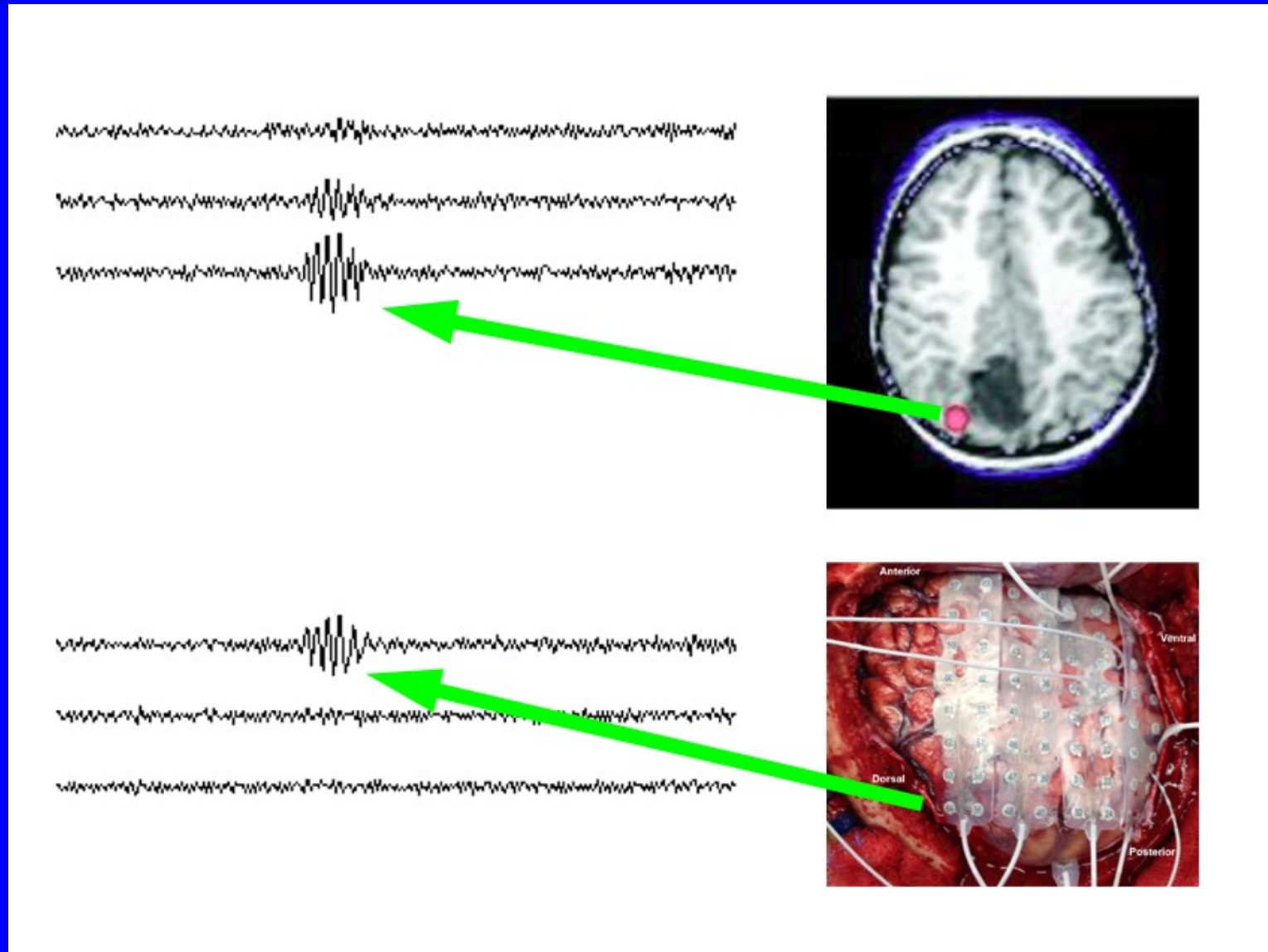
†NO: standard deviation; SOZ: seizure onset zone; AED: anti-epileptic drug
 *Compared to normative database: ~100 healthy children
 †Compared to pediatric epilepsy database: ~300 pediatric epilepsy patients
 *Artificial HFOs: power-line noise, cardiac signals, muscle activity, eye movement, Gibbs filter artifact

HFOs in Epilepsy

(Detectable at both sensor and source levels)



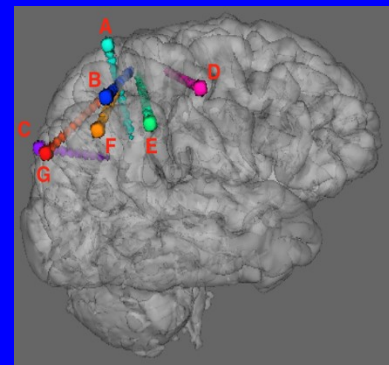
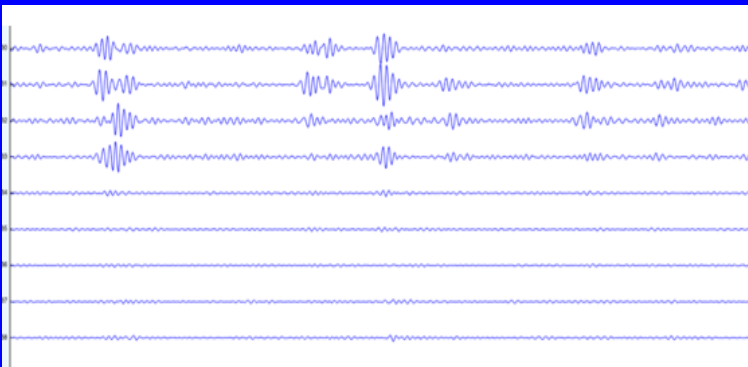
HFOs on Virtual Sensors and ECoG



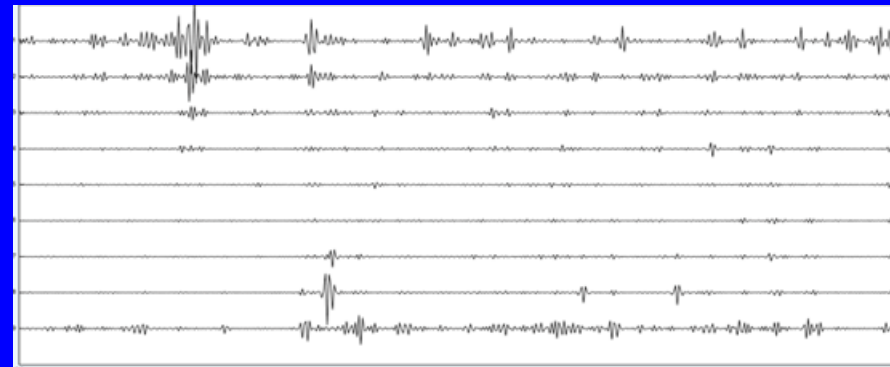
HFOs on Virtual Sensors vs. SEEG (250-500 Hz)



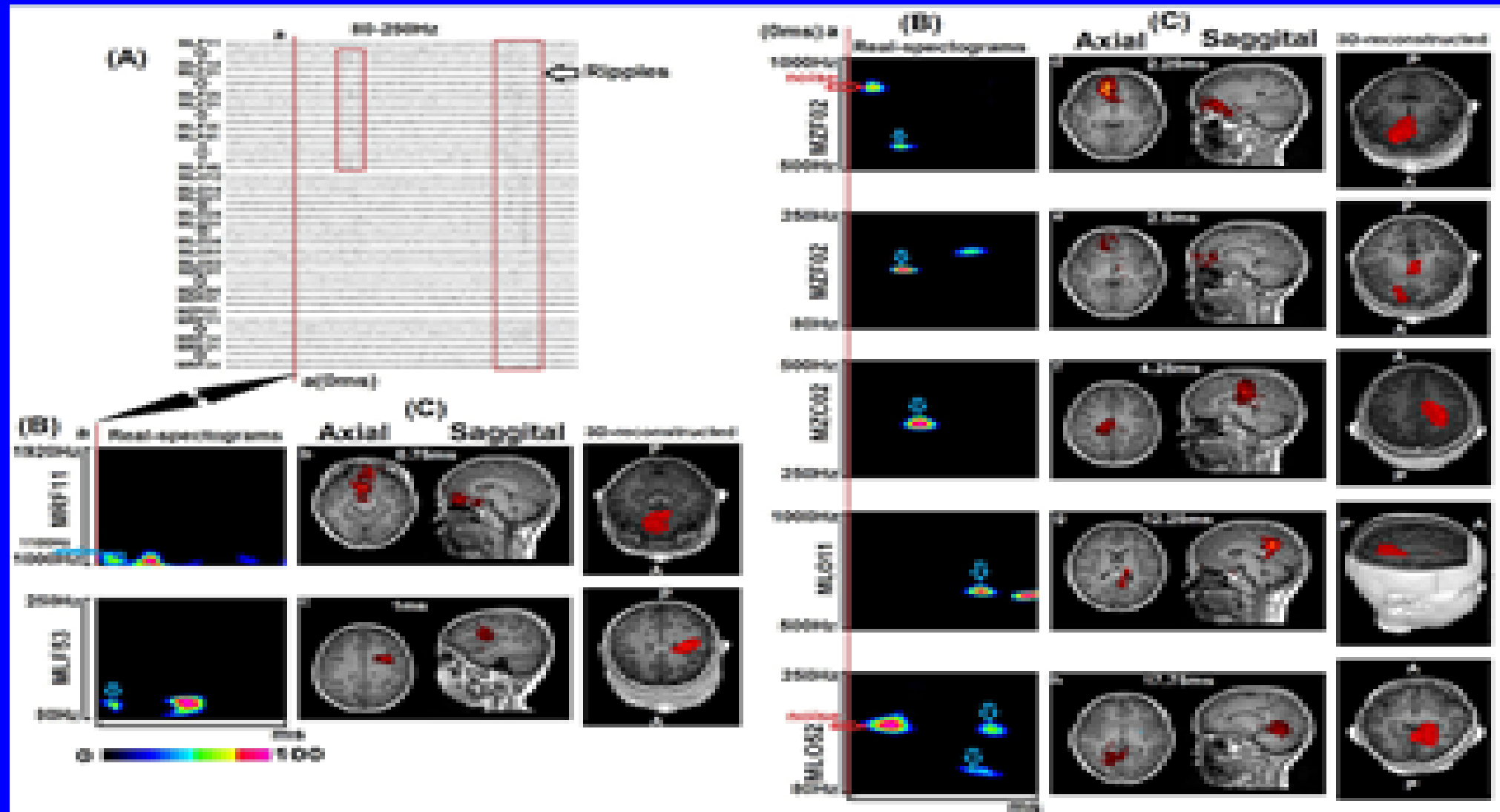
SEEG



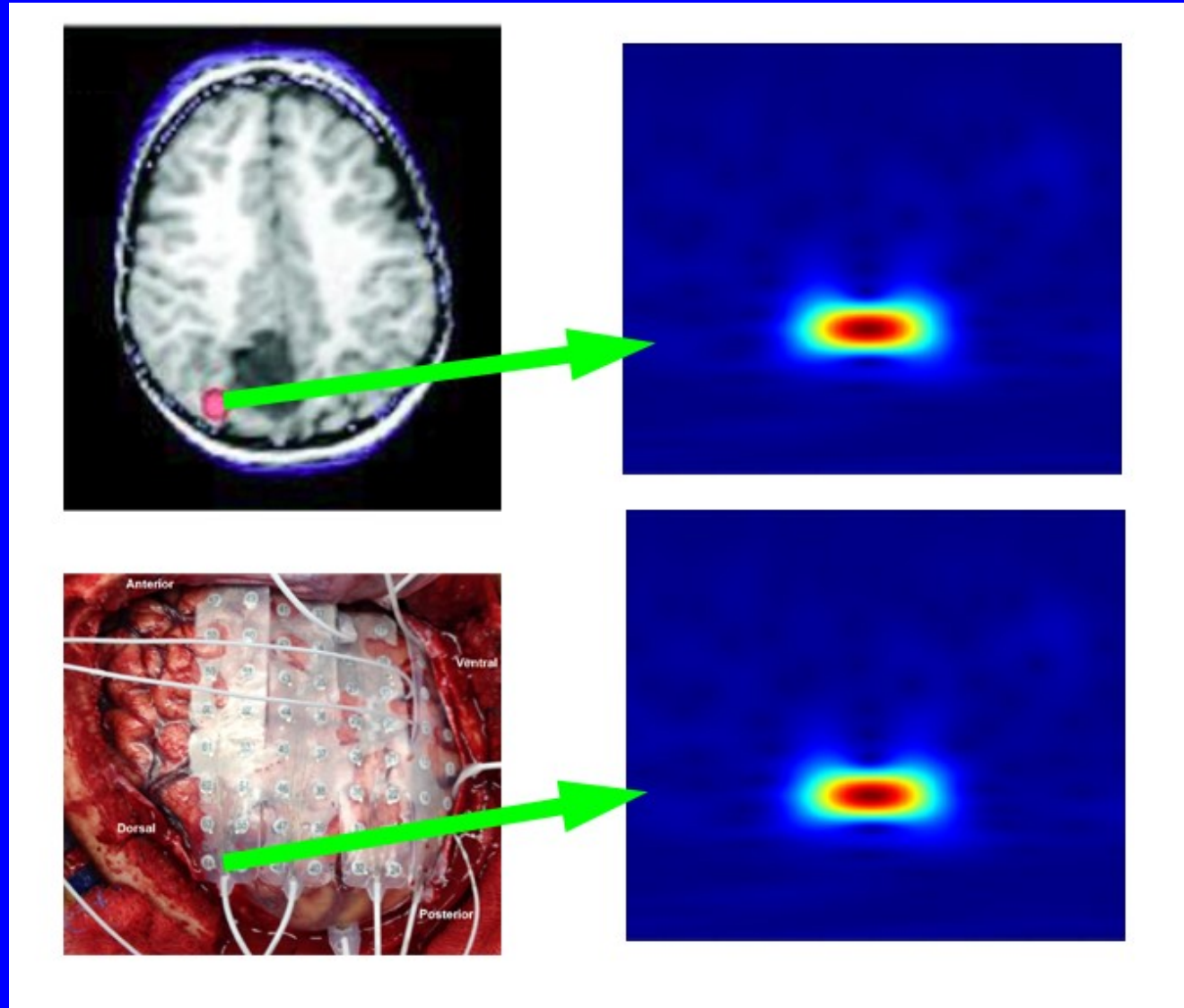
MEG Virtual Sensor



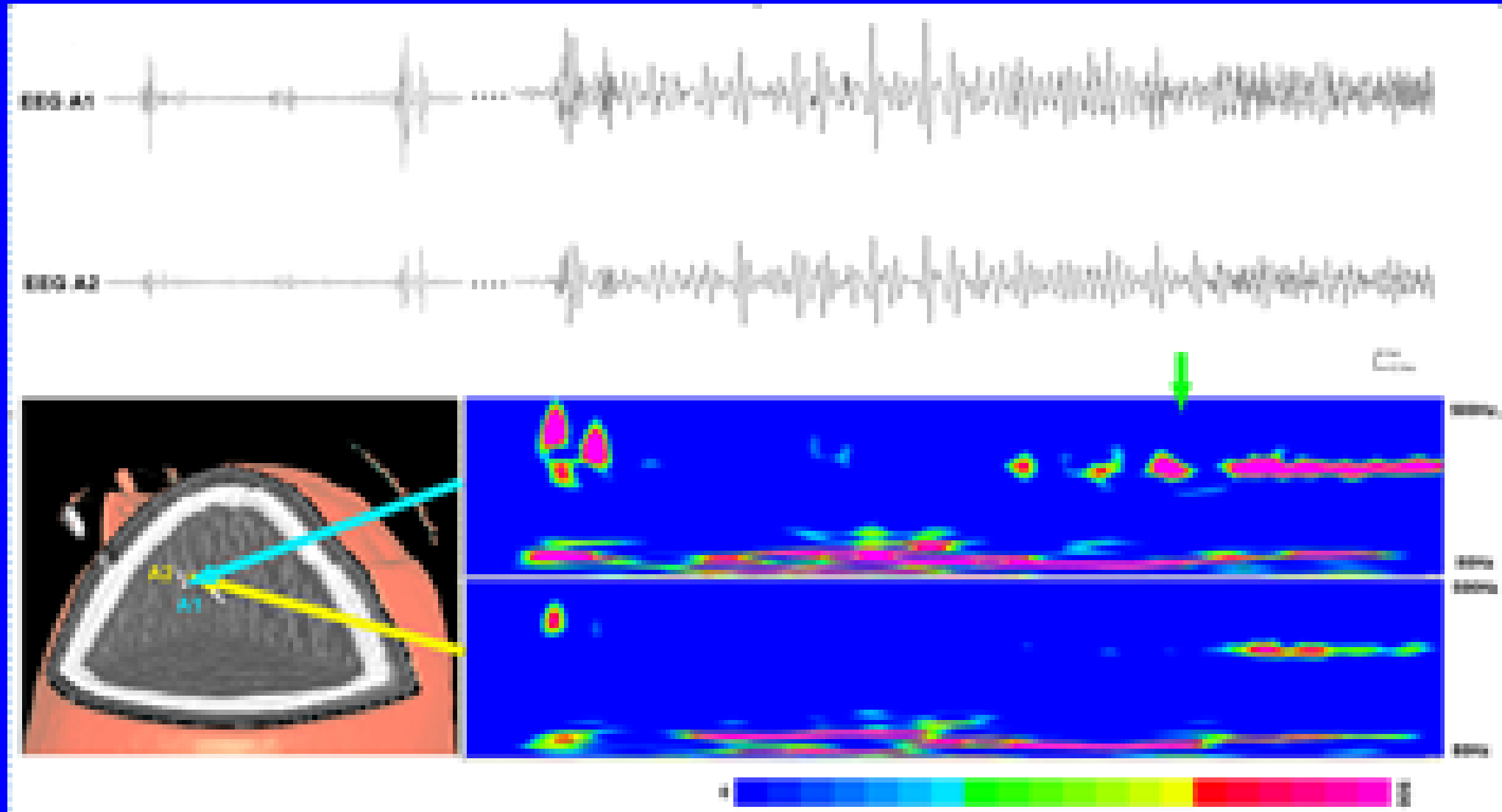
HFOs Appear Before, During and After Seizures



Virtual Sensor Spectrogram

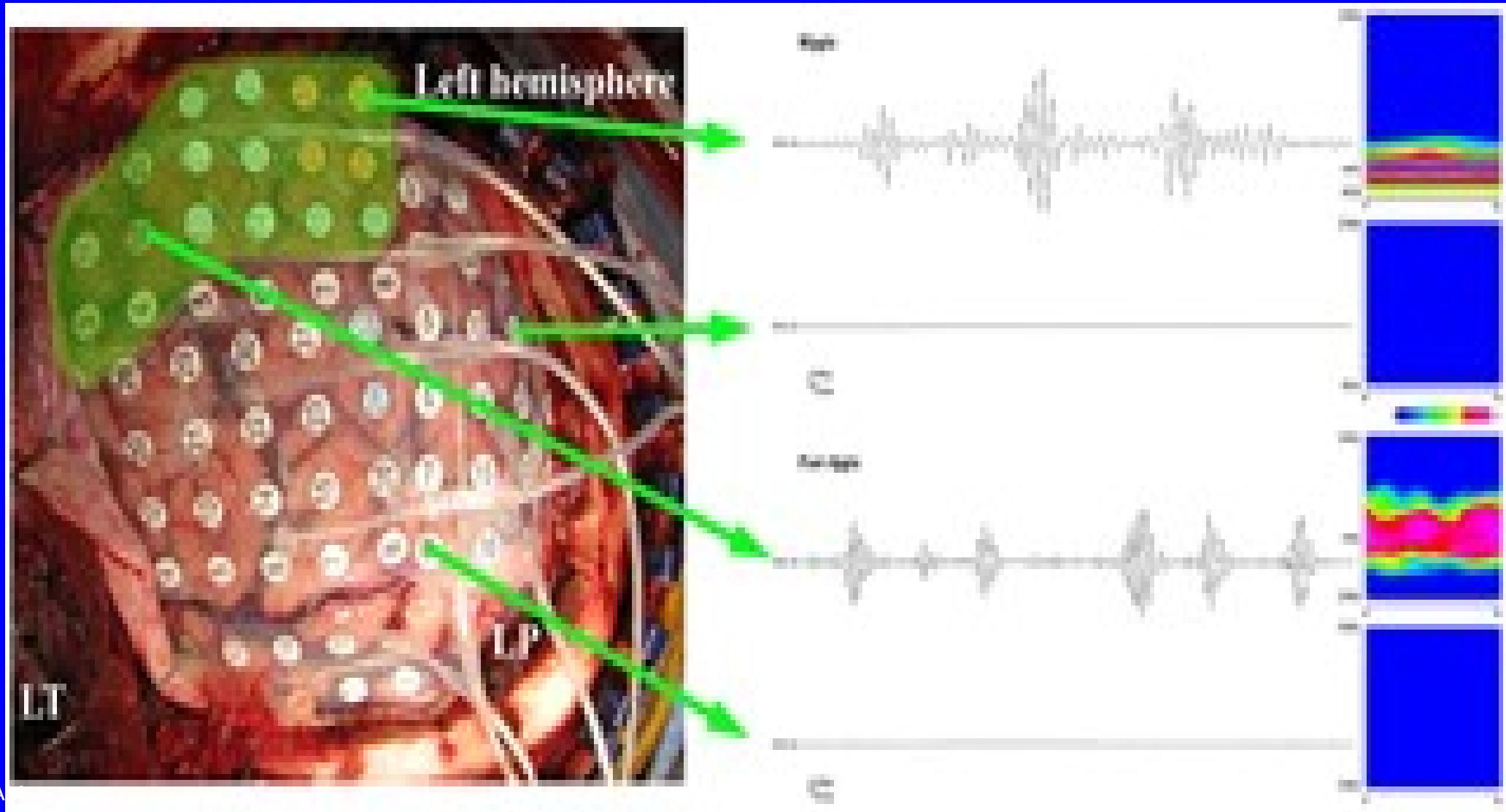


HFOs in Waveform and Spectrograms



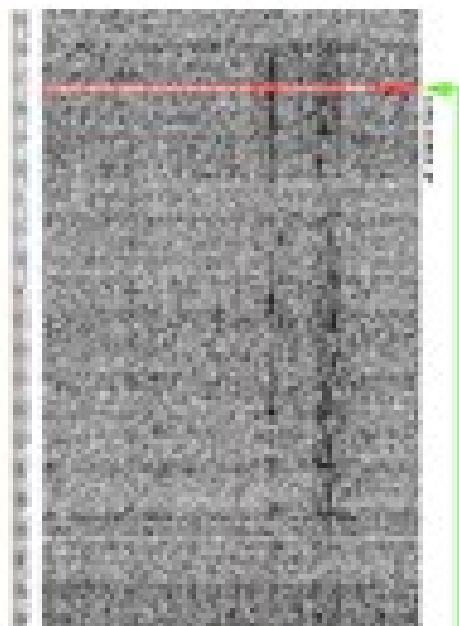
HFO Propagation

(higher frequency -> onset)



Waveform

MEG



Locations of Epileptic HFSS

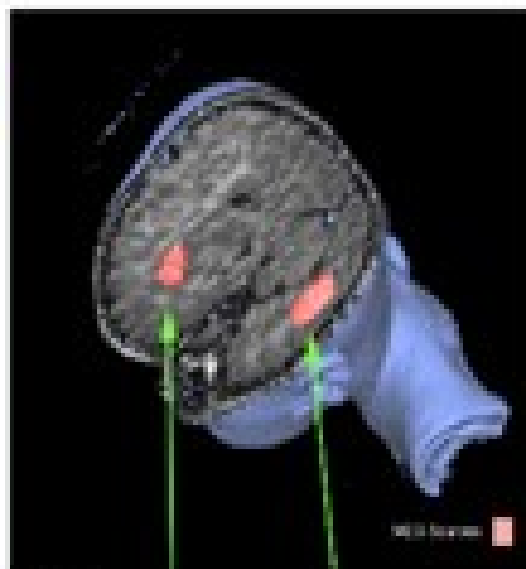
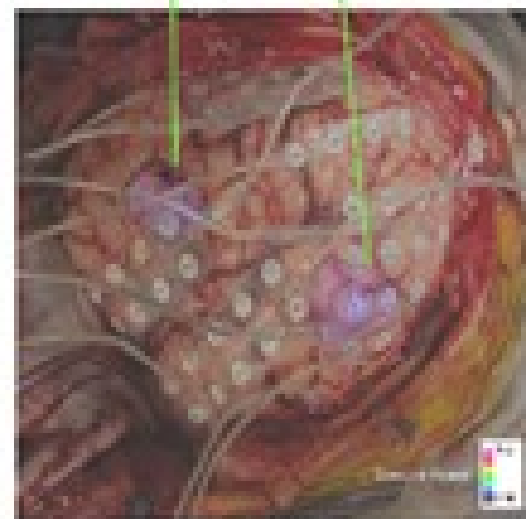
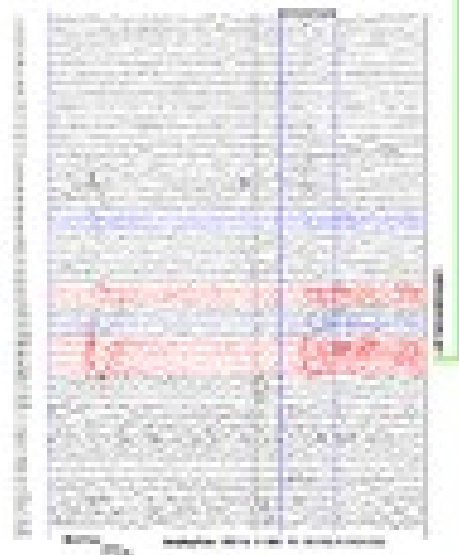
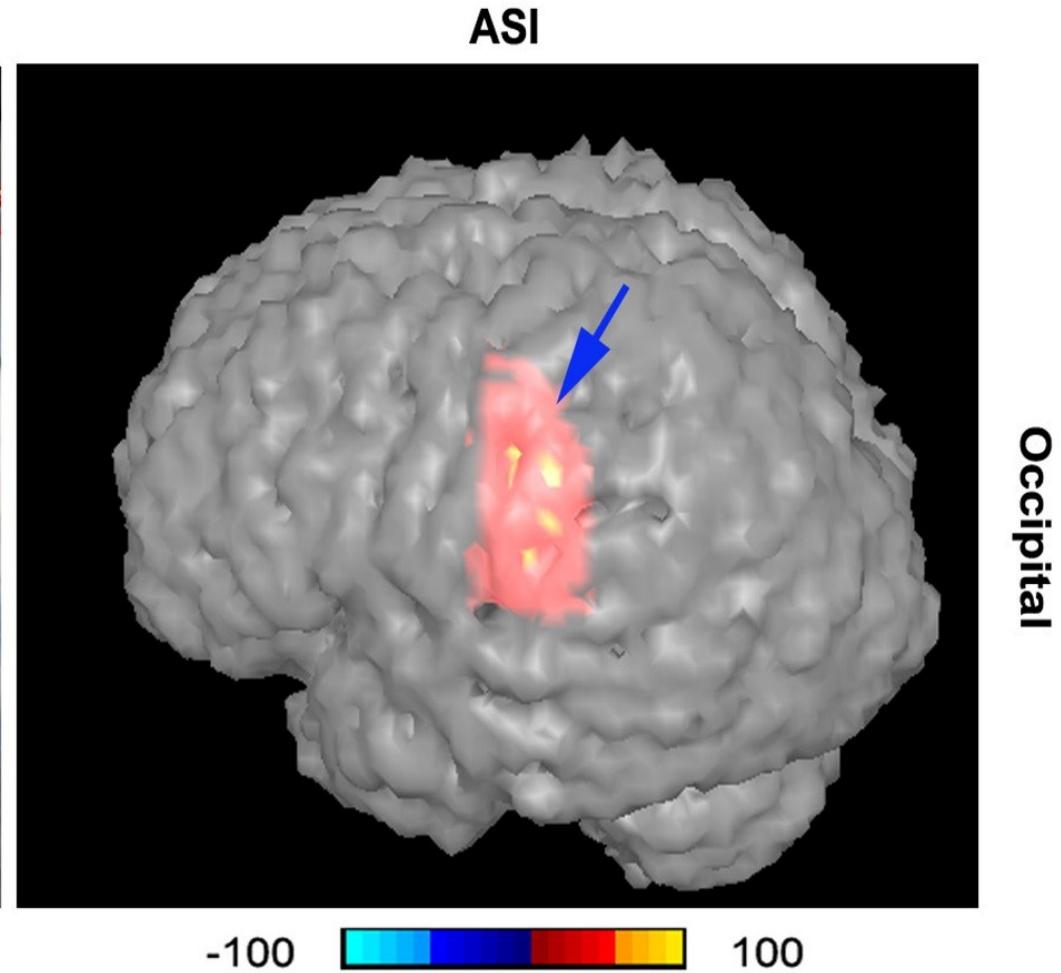
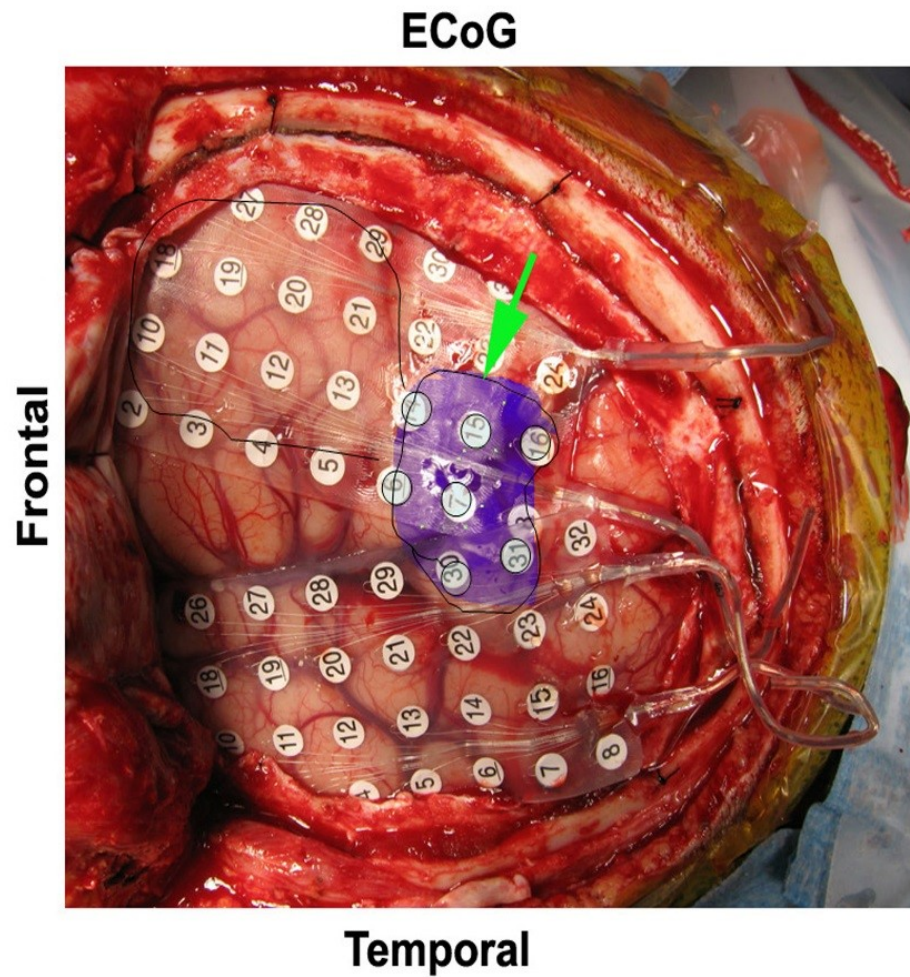


Figure 1.10

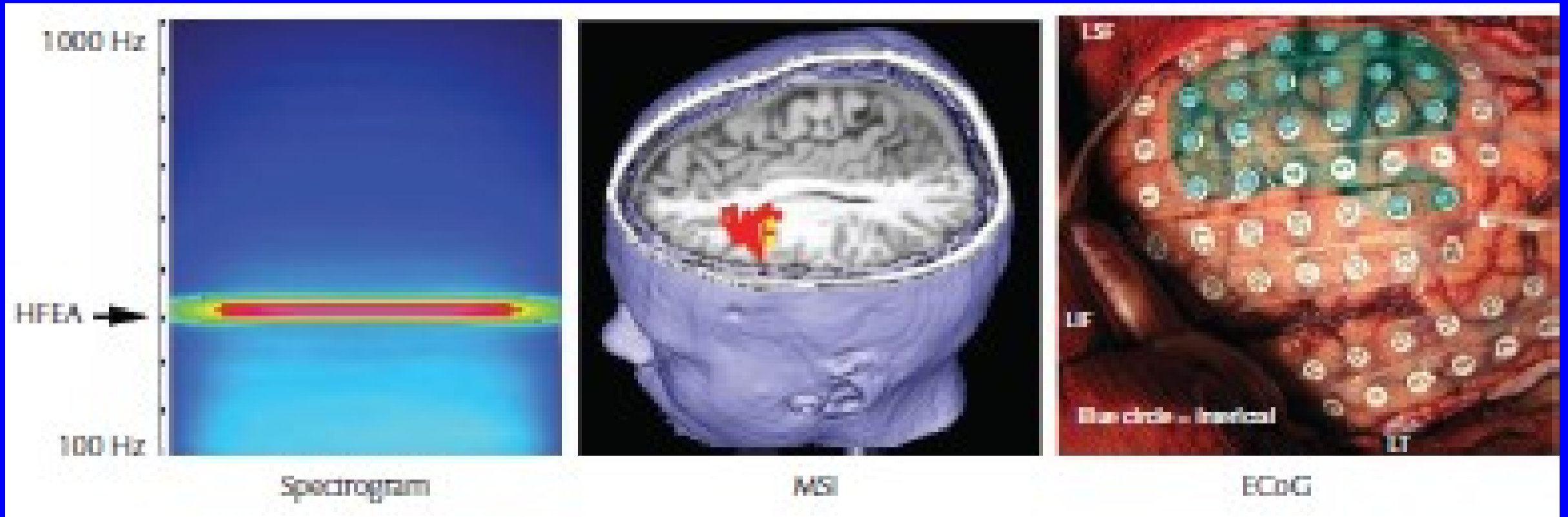
ECoG



MEG Can Localize HFOs Noninvasively



Identify and Localize HFOs for ECoG (MEG-Guided ECoG)

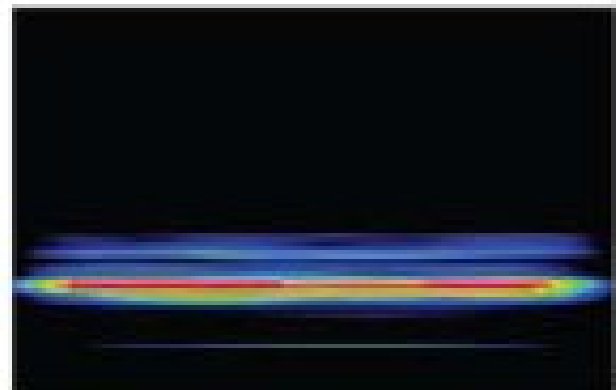
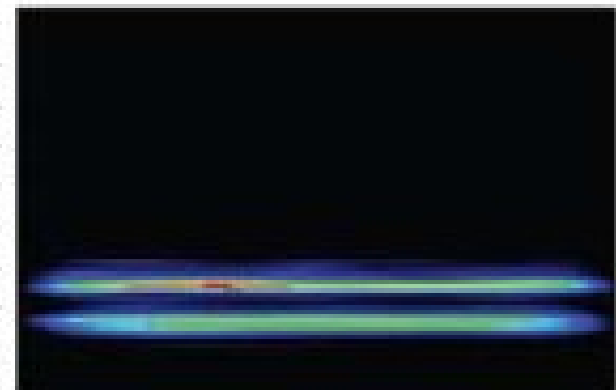




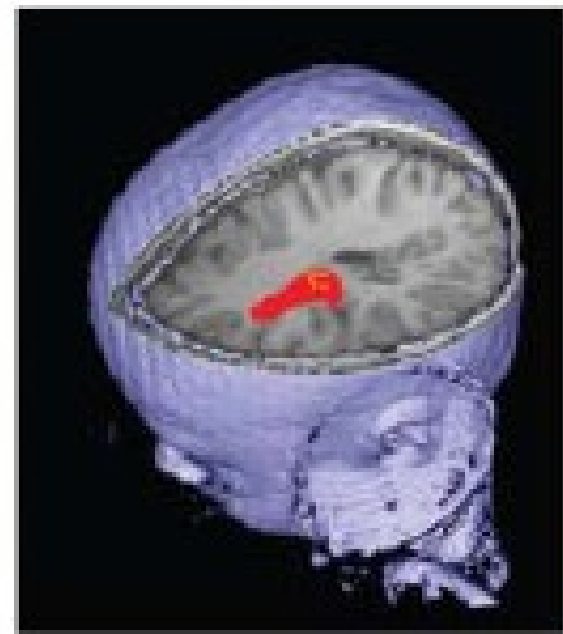
Interictal

Ictal

1000 Hz
100 Hz



310 Hz

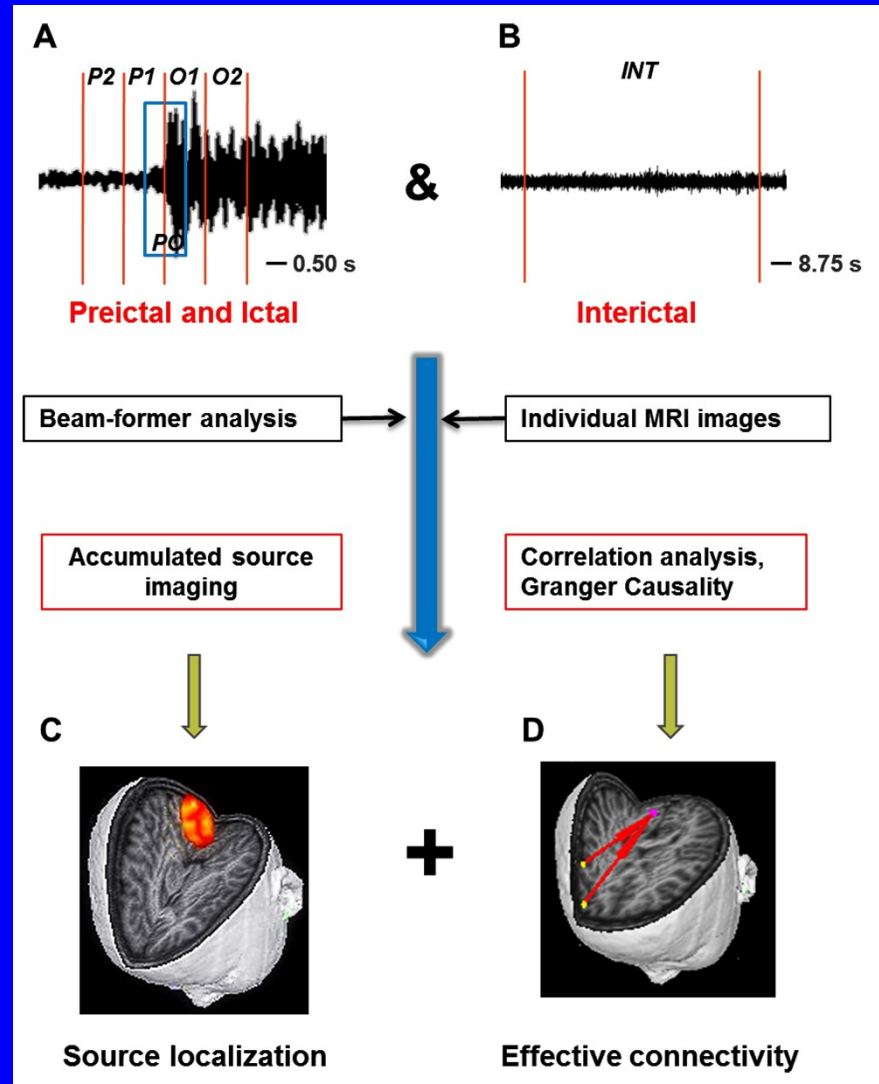


MSI

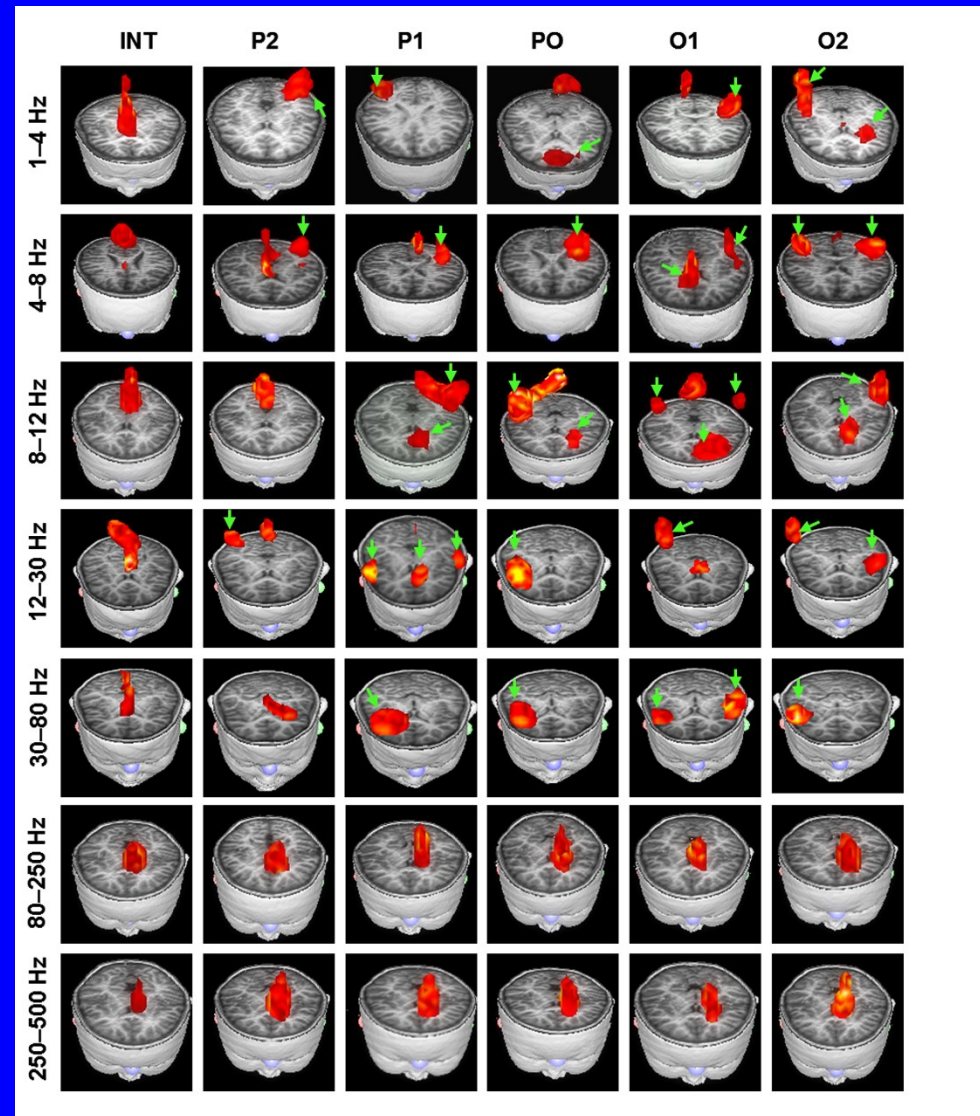


ECoG

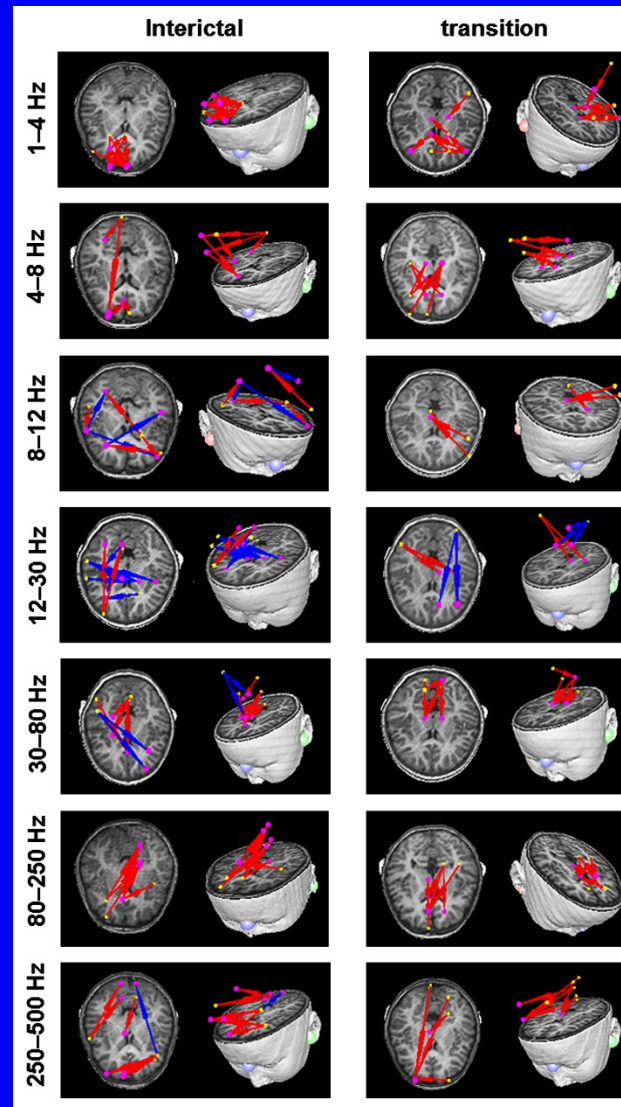
HFBS and Network (Connection)



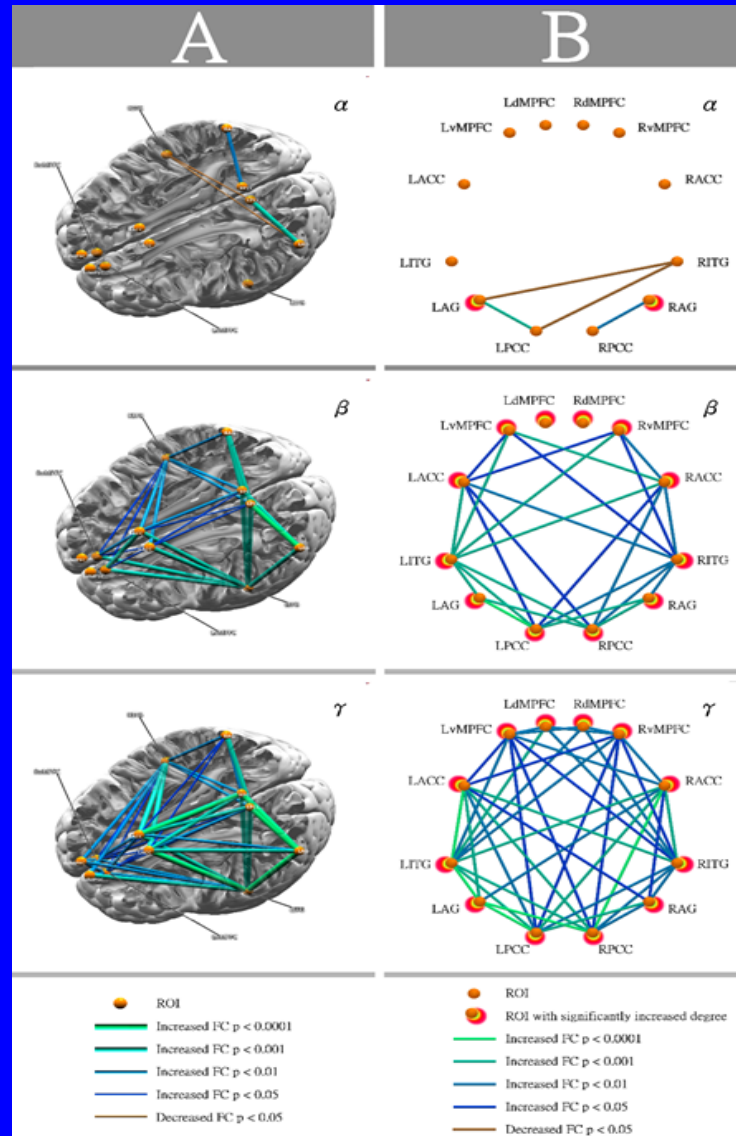
Source Imaging of Low-High Frequency Signals



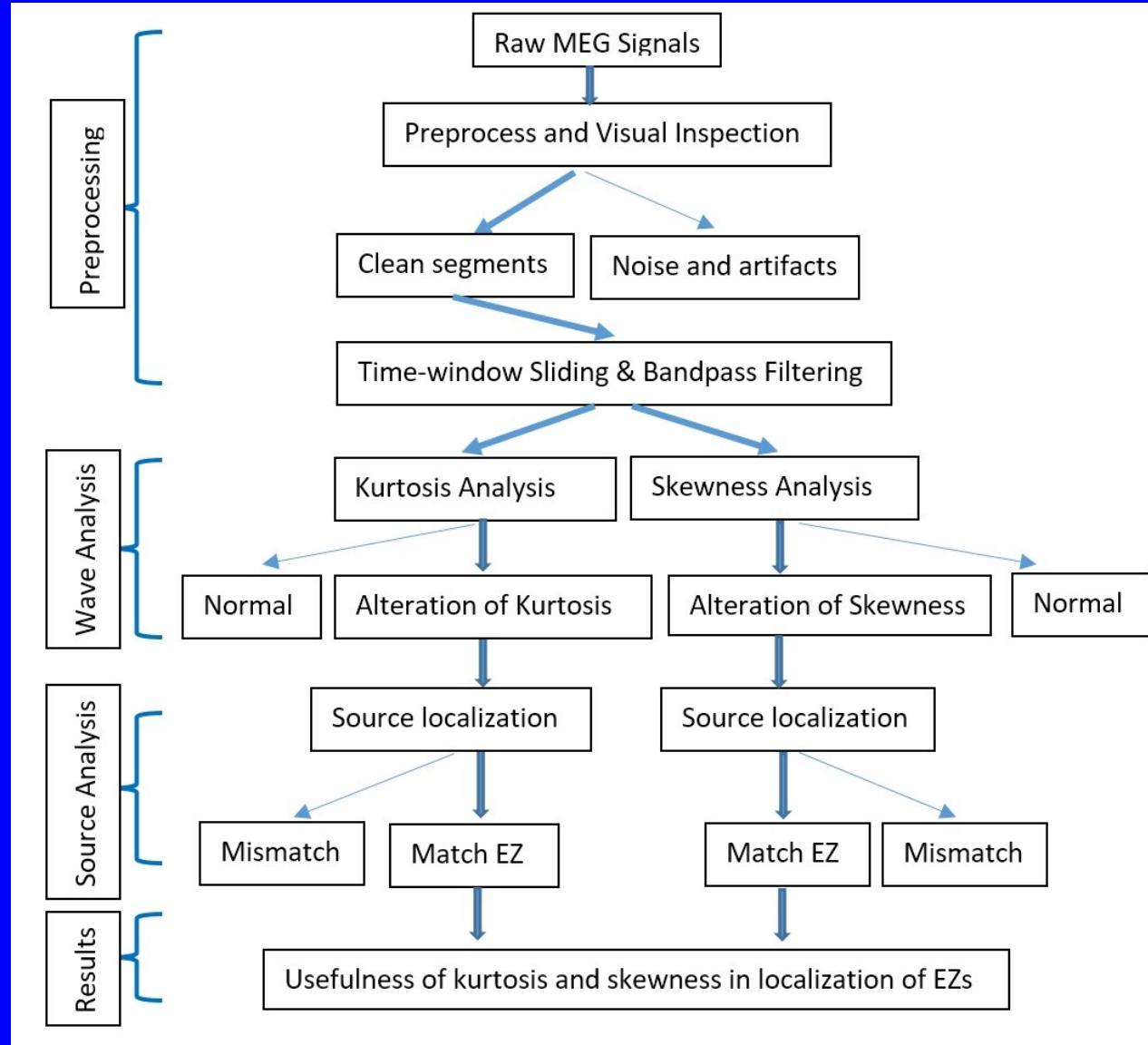
Source Networks of Low and High Frequency Signals



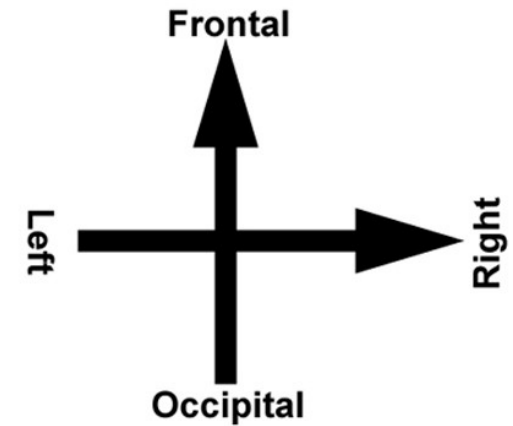
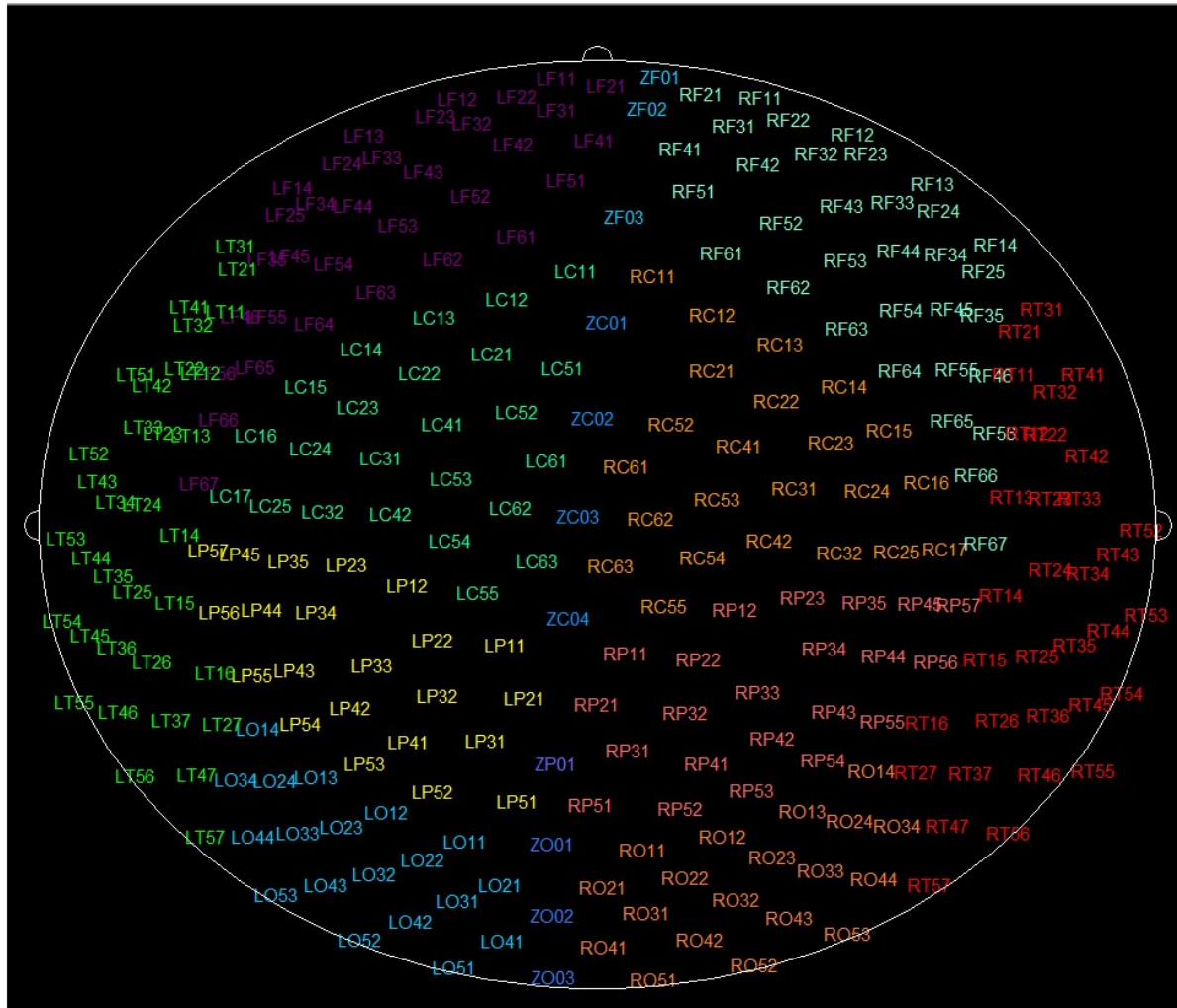
Network of HFBS



Kurtosis/skewness Based Source Imaging

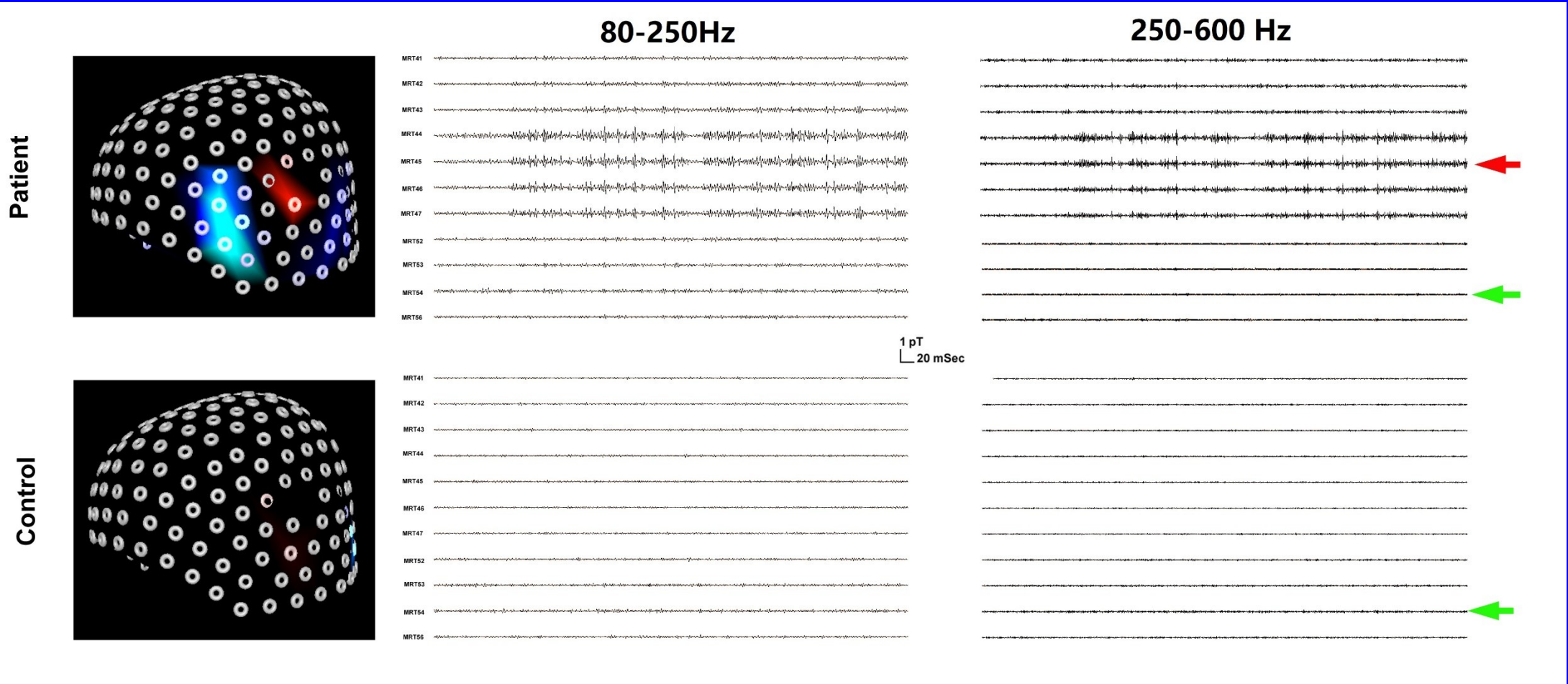


Kurtosis/Skewness at Sensor Levels

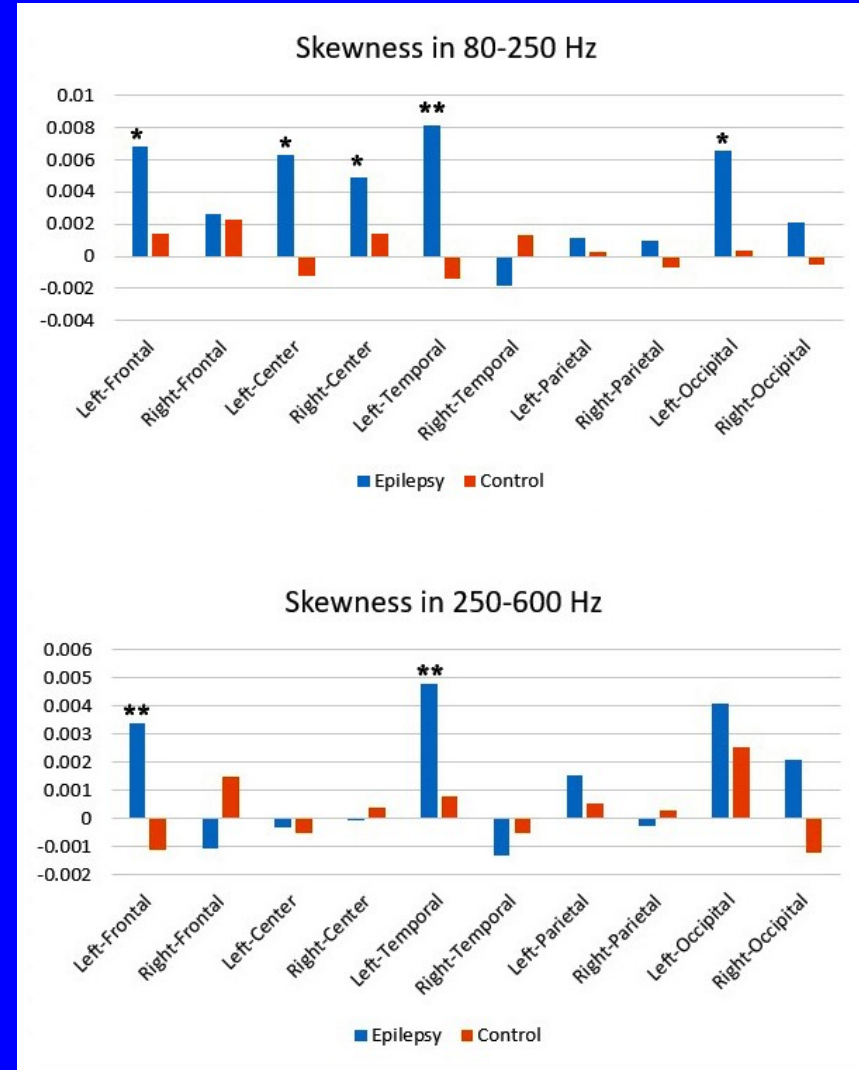
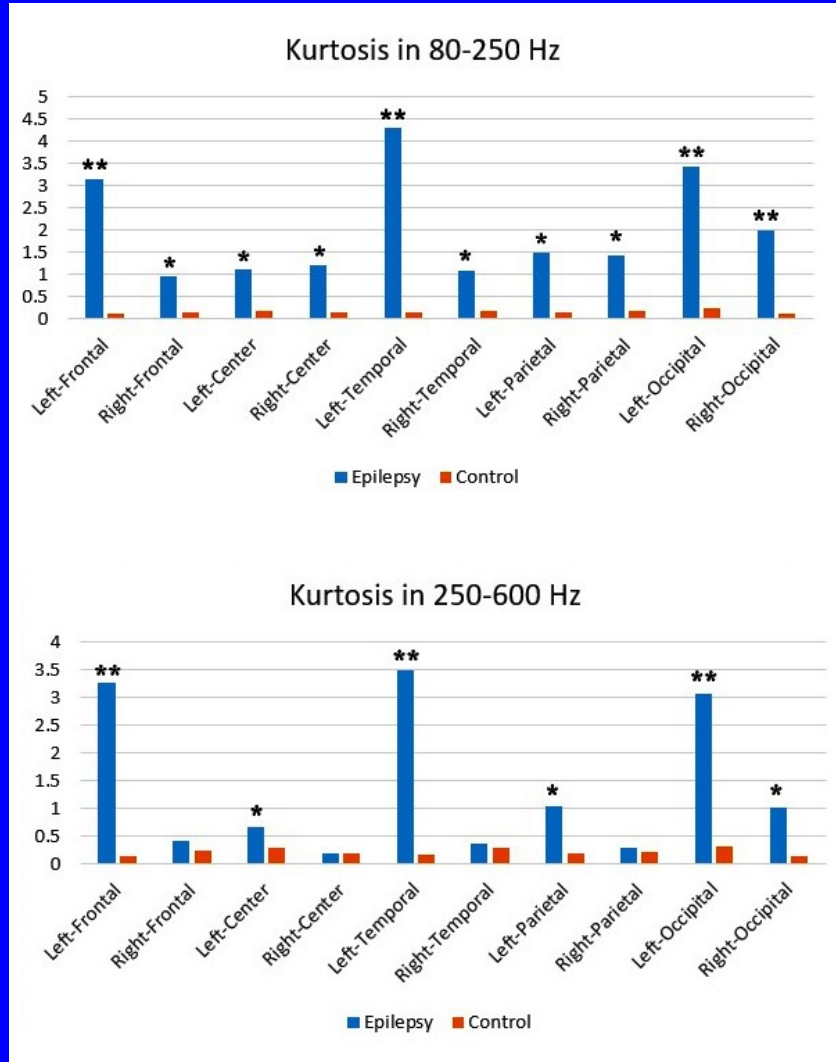


- LF: Left Frontal Sensors**
- RF: Right Frontal Sensors**
- LC: Left Central Sensors**
- RC: Right Central Sensors**
- LT: Left Temporal Sensors**
- RT: Right Temporal Sensors**
- LP: Left Parietal Sensors**
- RP: Right Parietal Sensors**
- LO: Left Occipital Sensors**
- RO: Right Occipital Sensors**

HFOs (Ripples and Fast Ripples)

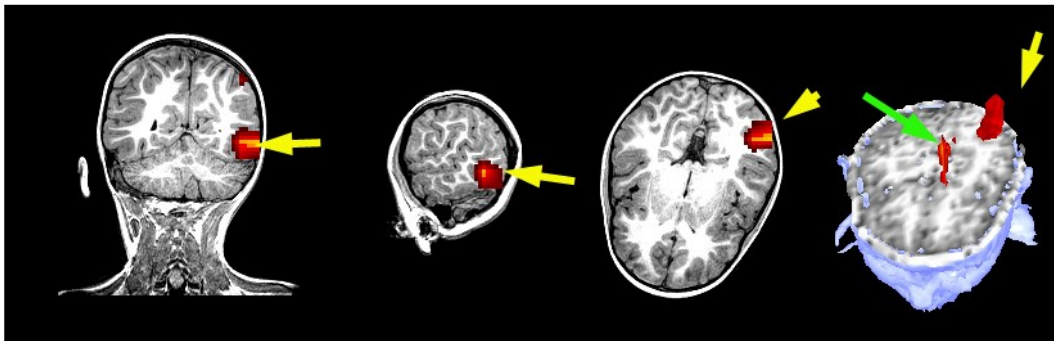


Measurements of Kurtosis

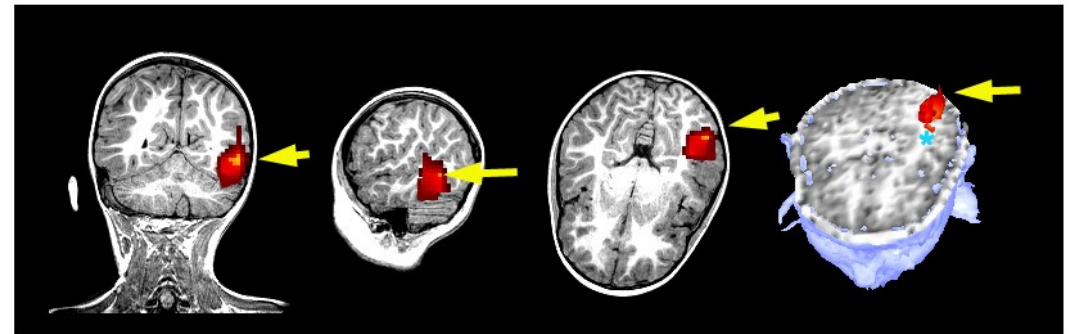
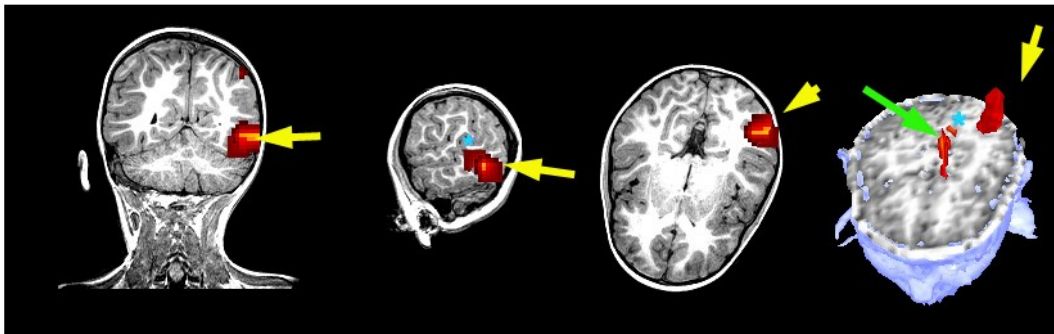
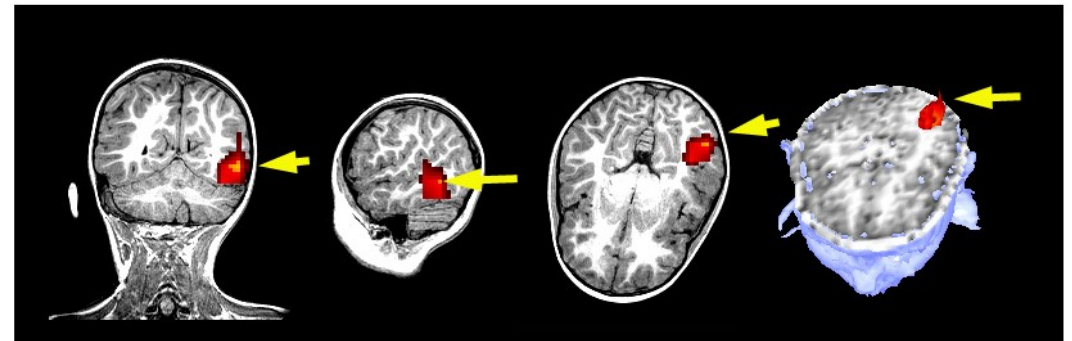


Kurtosis/Skewness Source Imaging

80-250 Hz



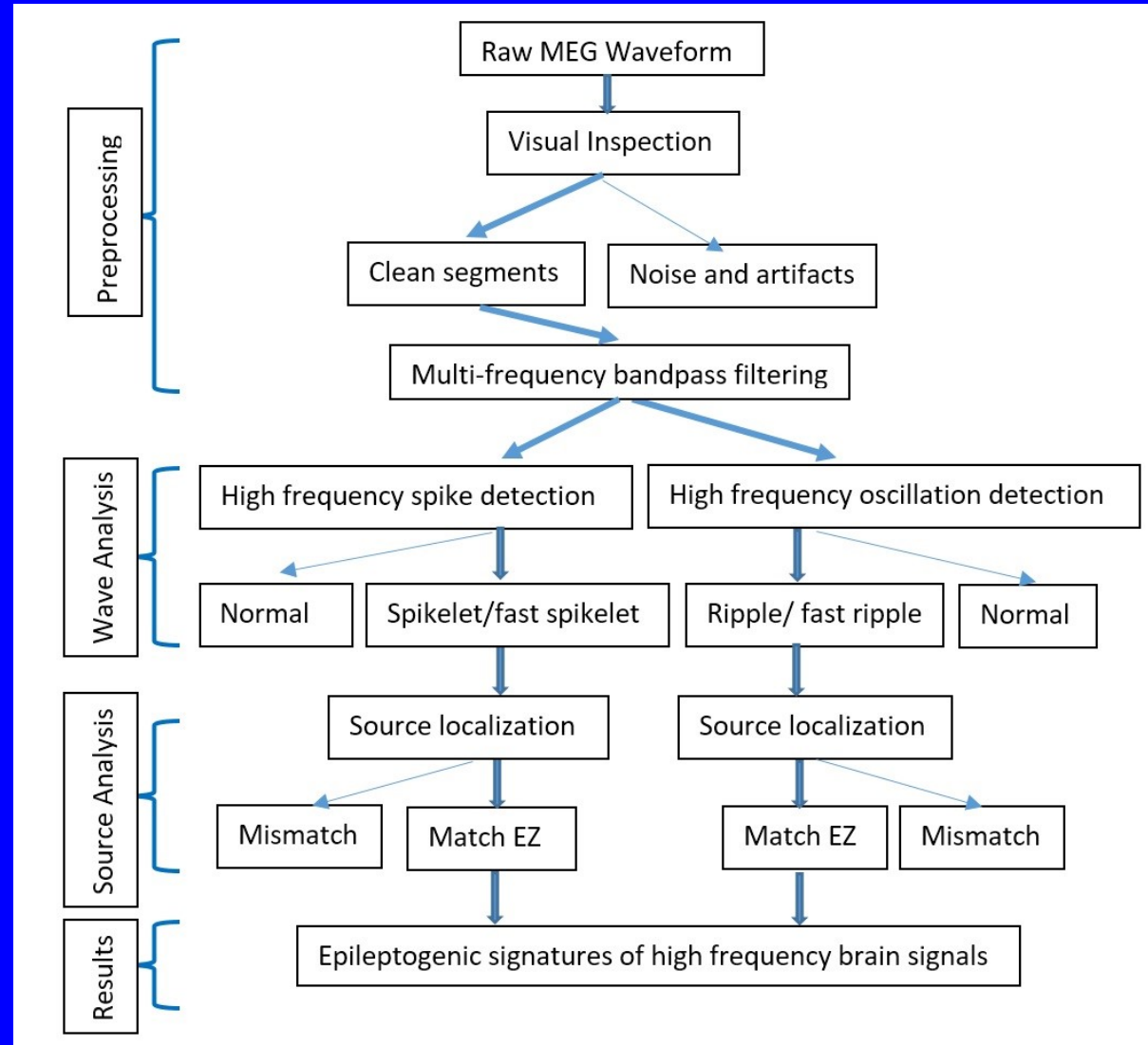
250-600 Hz



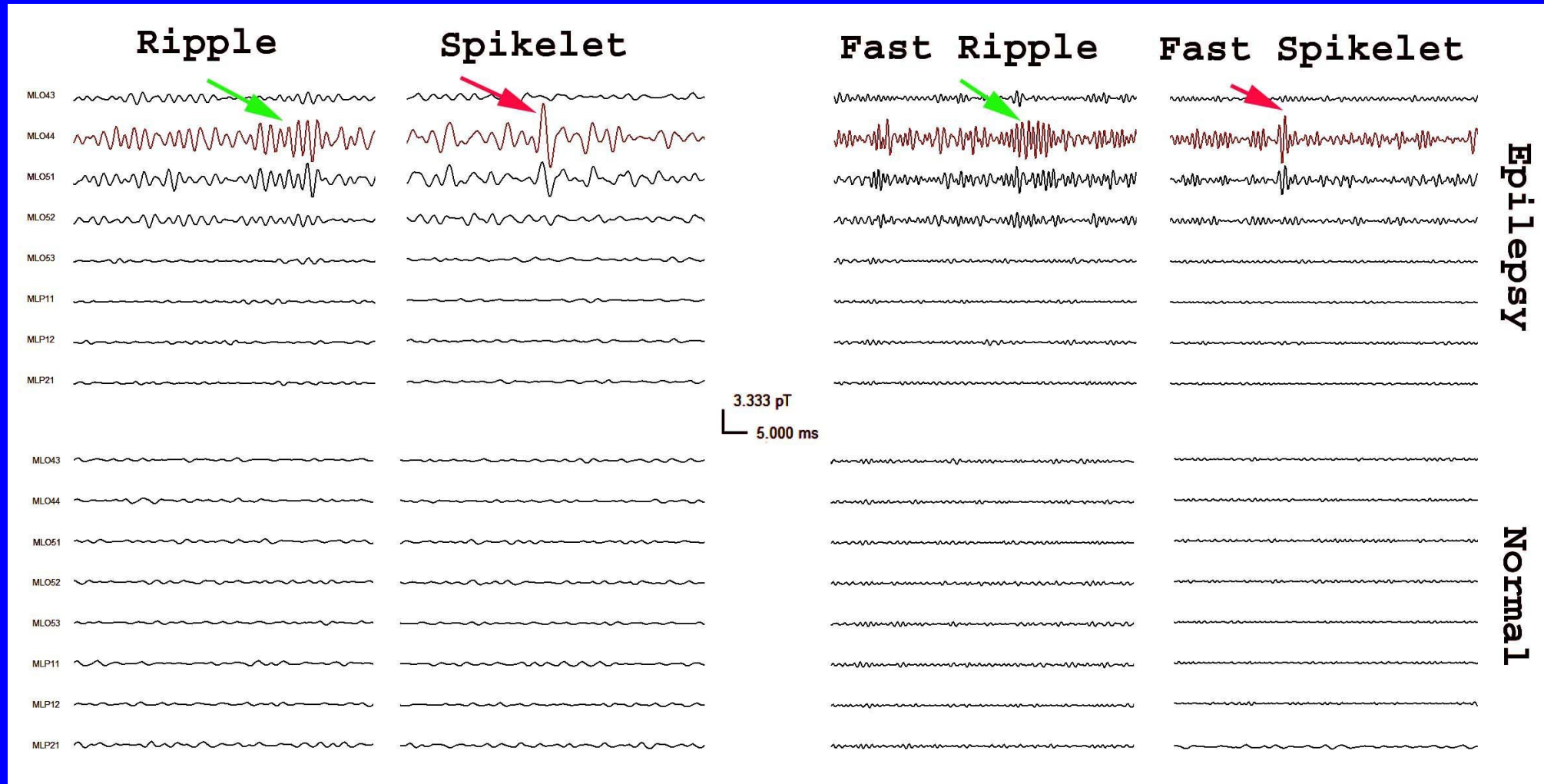
MEG HFBS and Kurtosis/Skewness

- ❑ Epileptic HFBS have significantly elevated kurtosis and skewness.
- ❑ Kurtosis and skewness based source imaging can localize EZs
- ❑ Kurtosis and skewness of HFBS provide quantitative indication of epileptic activity
- ❑ MEG HFBS kurtosis/skewness is novel approach
 - ❖ Better than visual identification (time-consuming and subjective)
 - ❖ Better than invasive recordings (risky and costly)

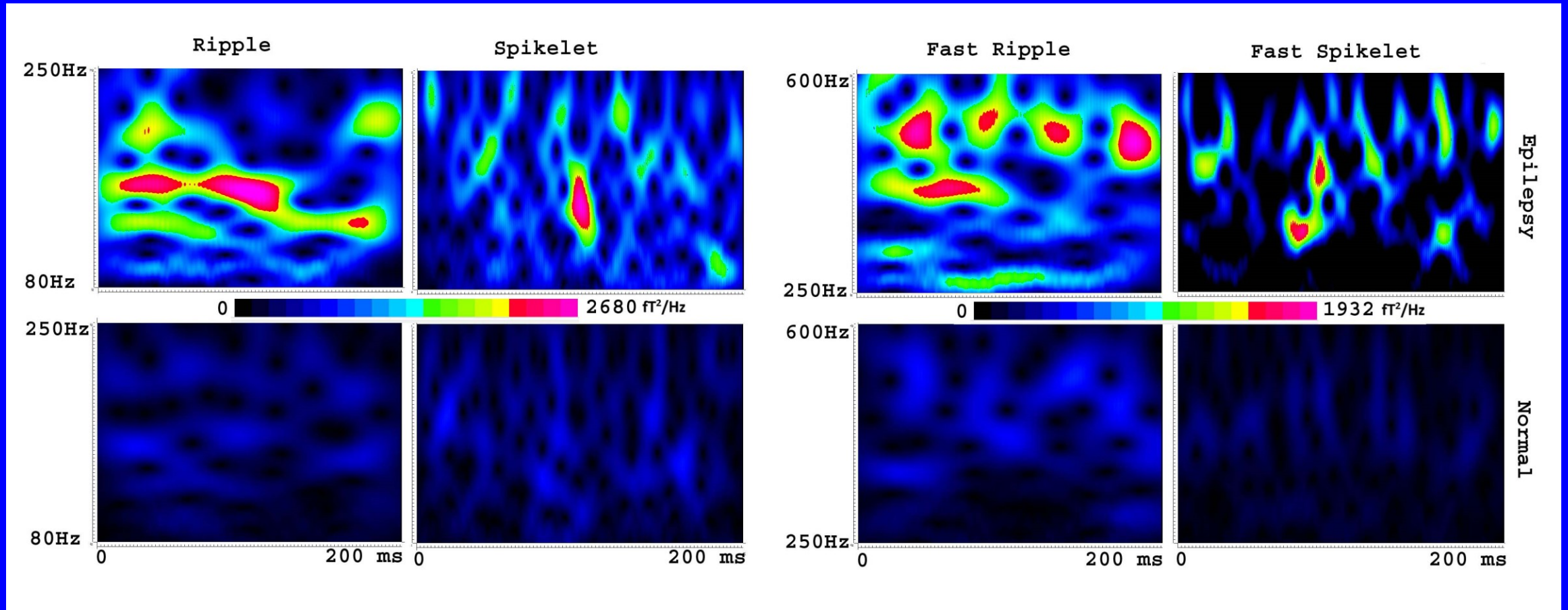
Neuromagnetic High Frequency Spikes



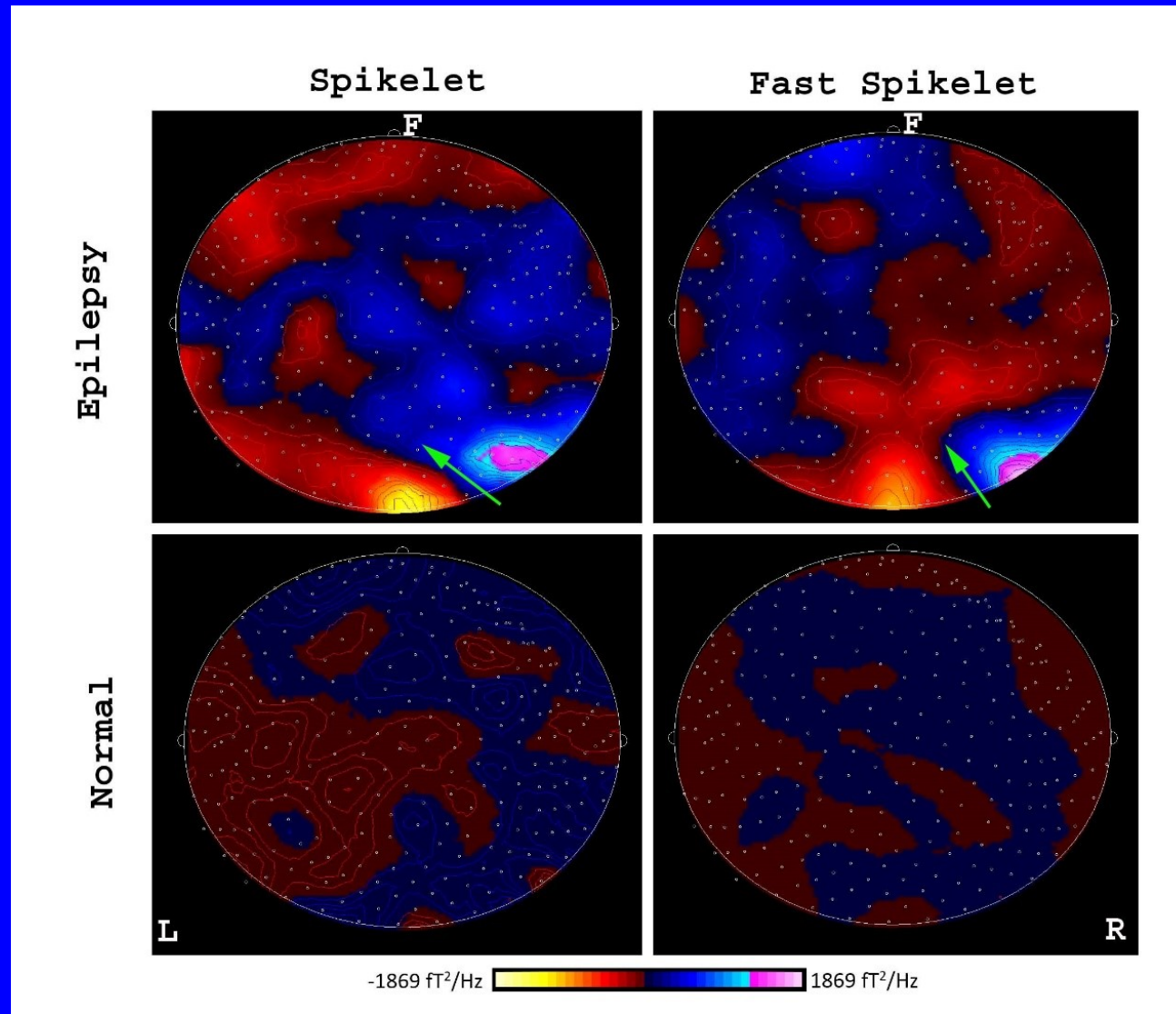
Ripples/Fast Ripples vs. Spike/Fast Spikelets



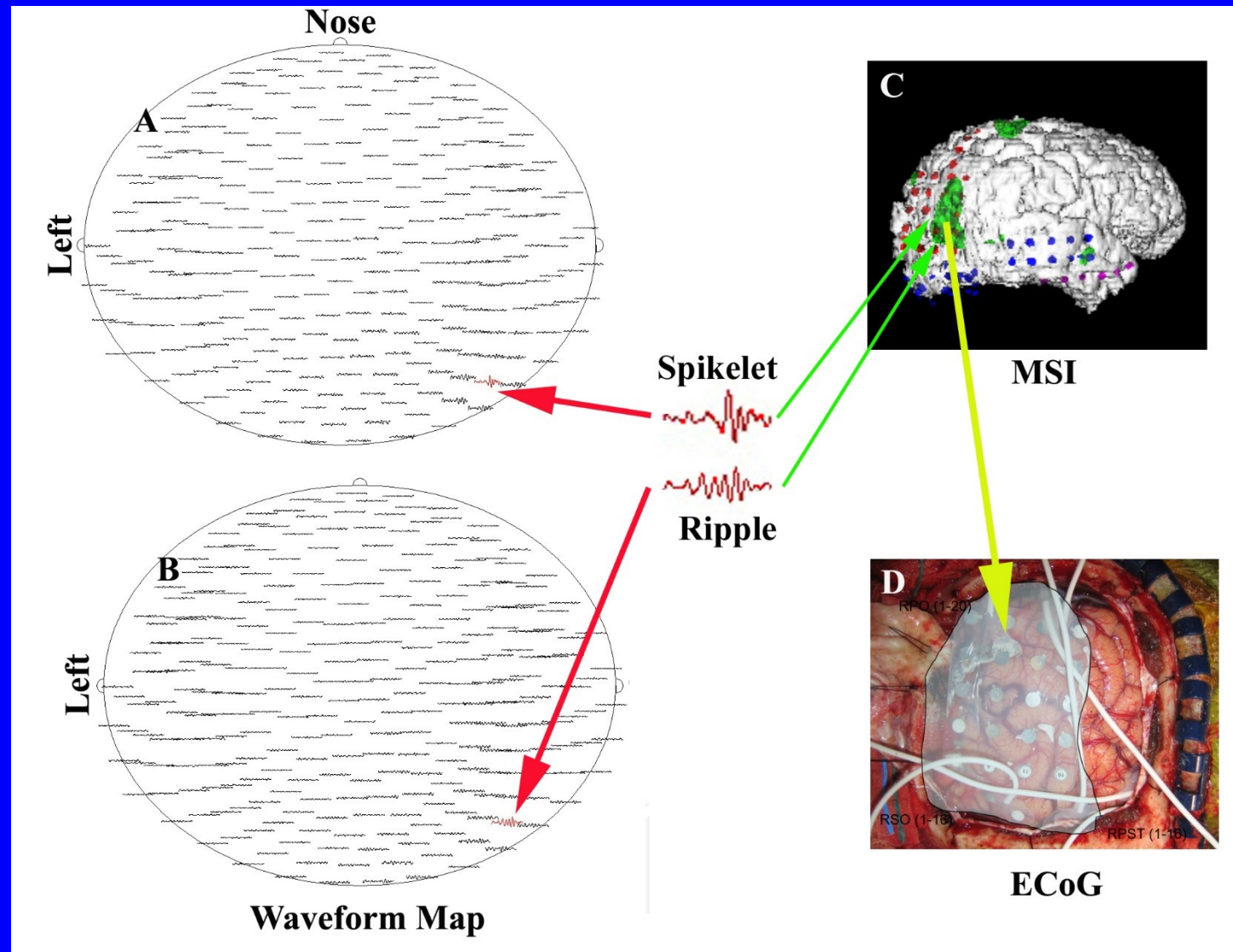
Spectrograms of HFOs and HFSs



Spectral Map of HFSs



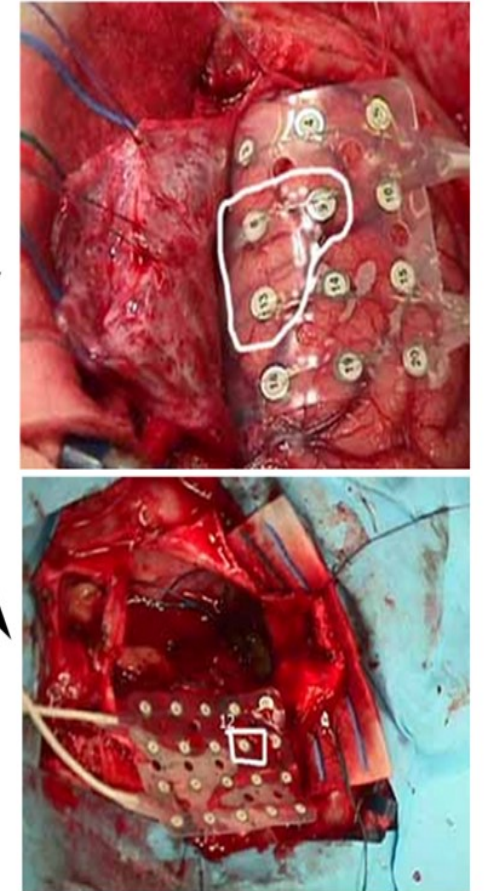
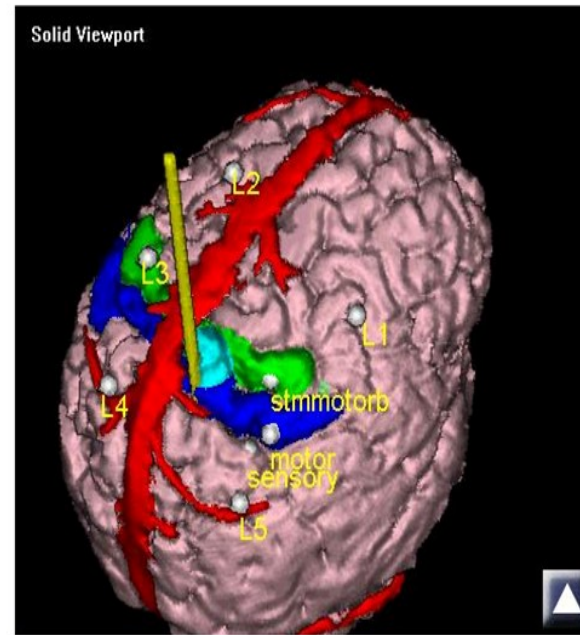
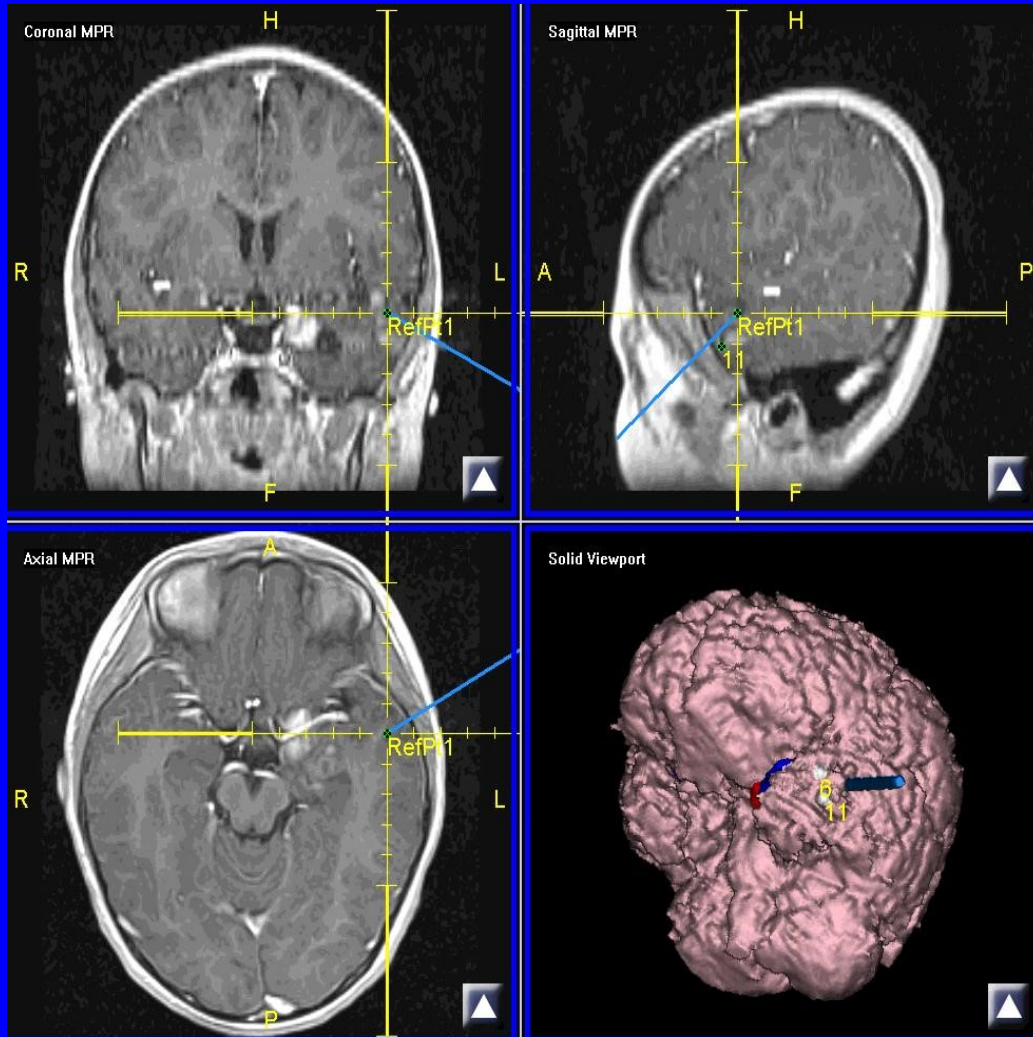
MEG HFSs and ECoG HFSs



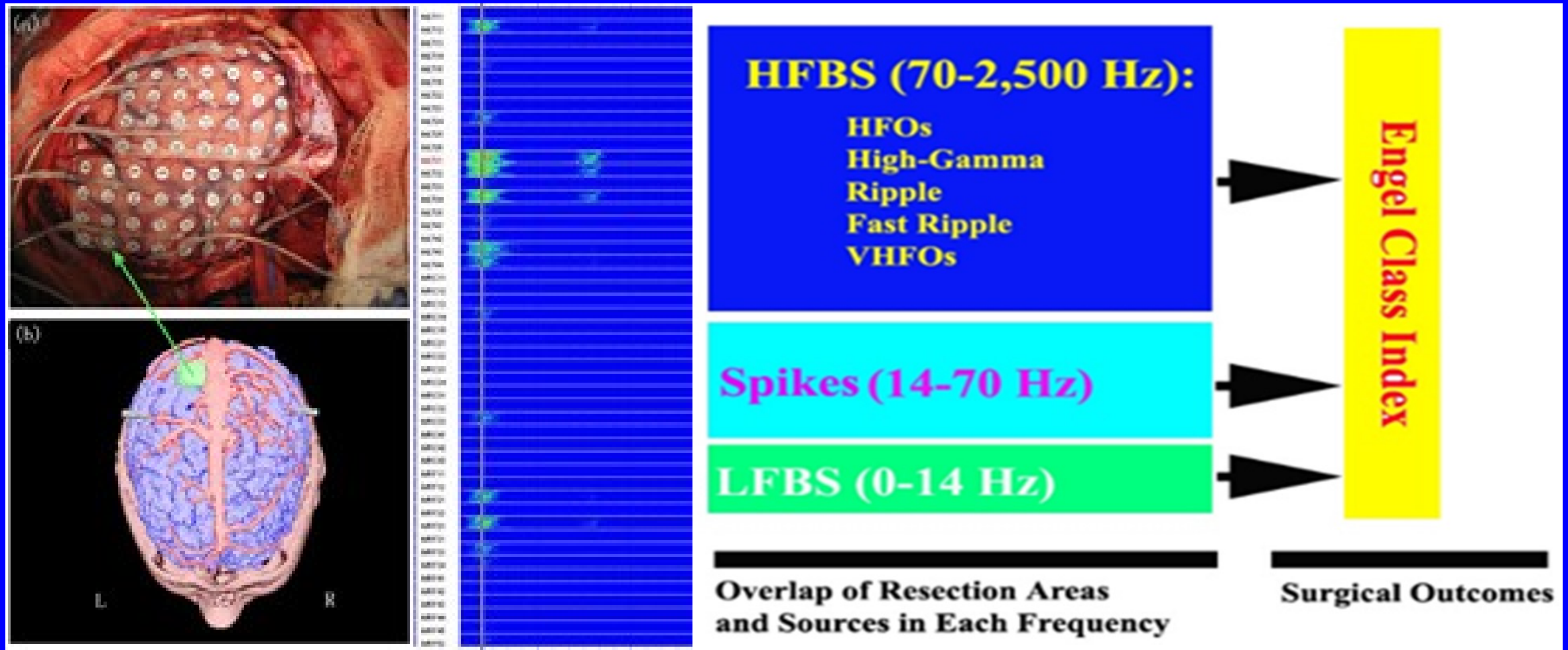
MEG Detection of Epileptic HFSs

- Epileptic brain generates high frequency spikes (HFSs) in 80-600 Hz
- HFSs include spikelets (80-250 Hz) and fast spikelets (250-600 Hz)
- HFSs are a new epileptogenic biomarker for localizing epileptogenic zones
- HFSs can be noninvasively detected by MEG

Magnetic Source Imaging Guided Surgery



Resection Brain Areas Generating HFBS Predicts Favorable Outcomes



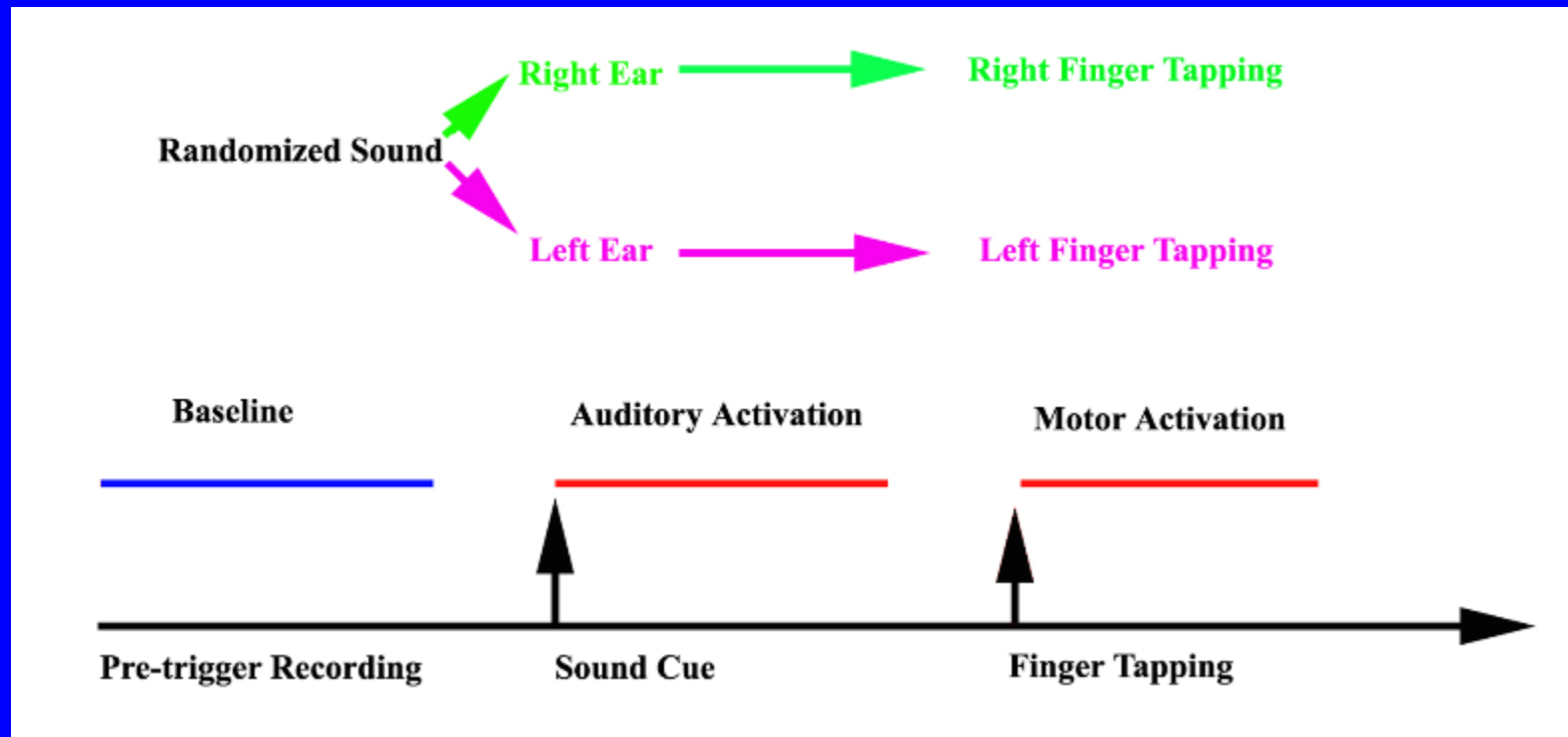
Content

- High Frequency Brain Signals (HFBS)
- Hardware development for detecting HFBS
- Software development for analyzing HFBS
- Clinical Applications of HFBS
 - Epilepsy
 - Migraine
 - Functional mapping and others
- Discussion

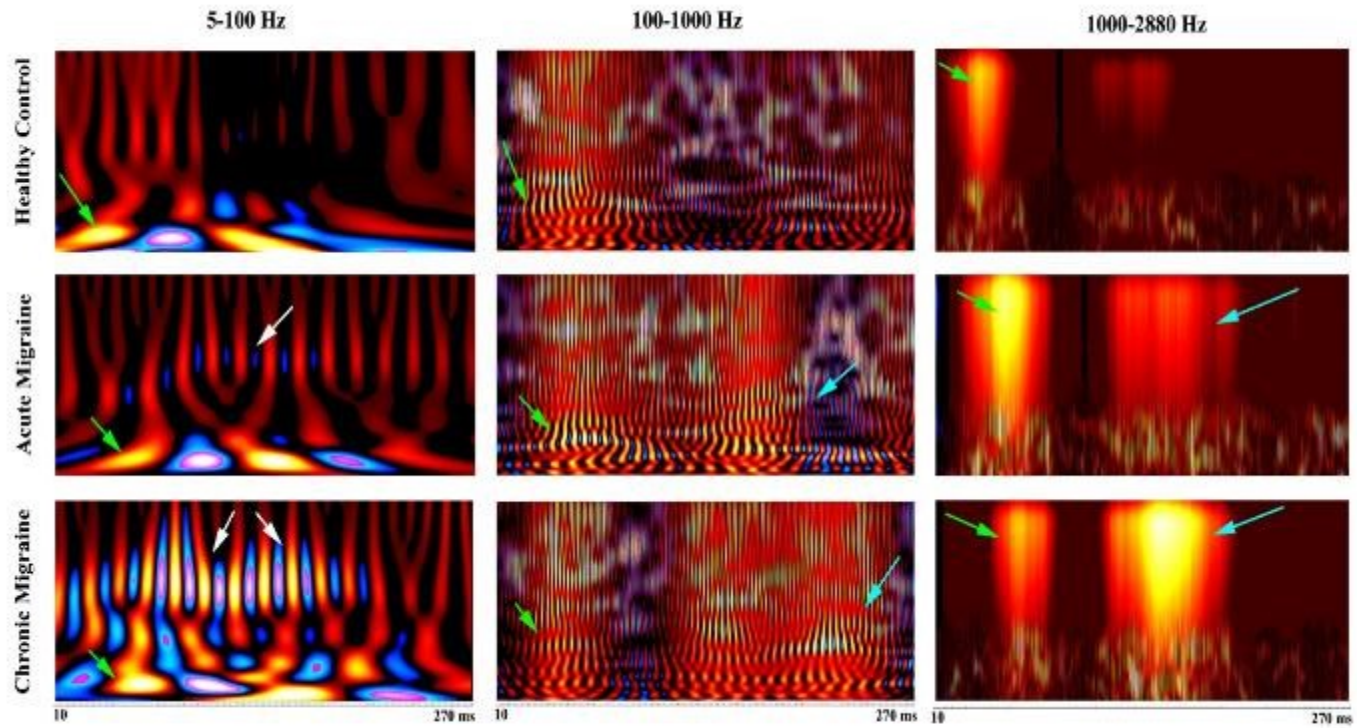
MEG Study of Acute Migraine

(Subjects and Methods)

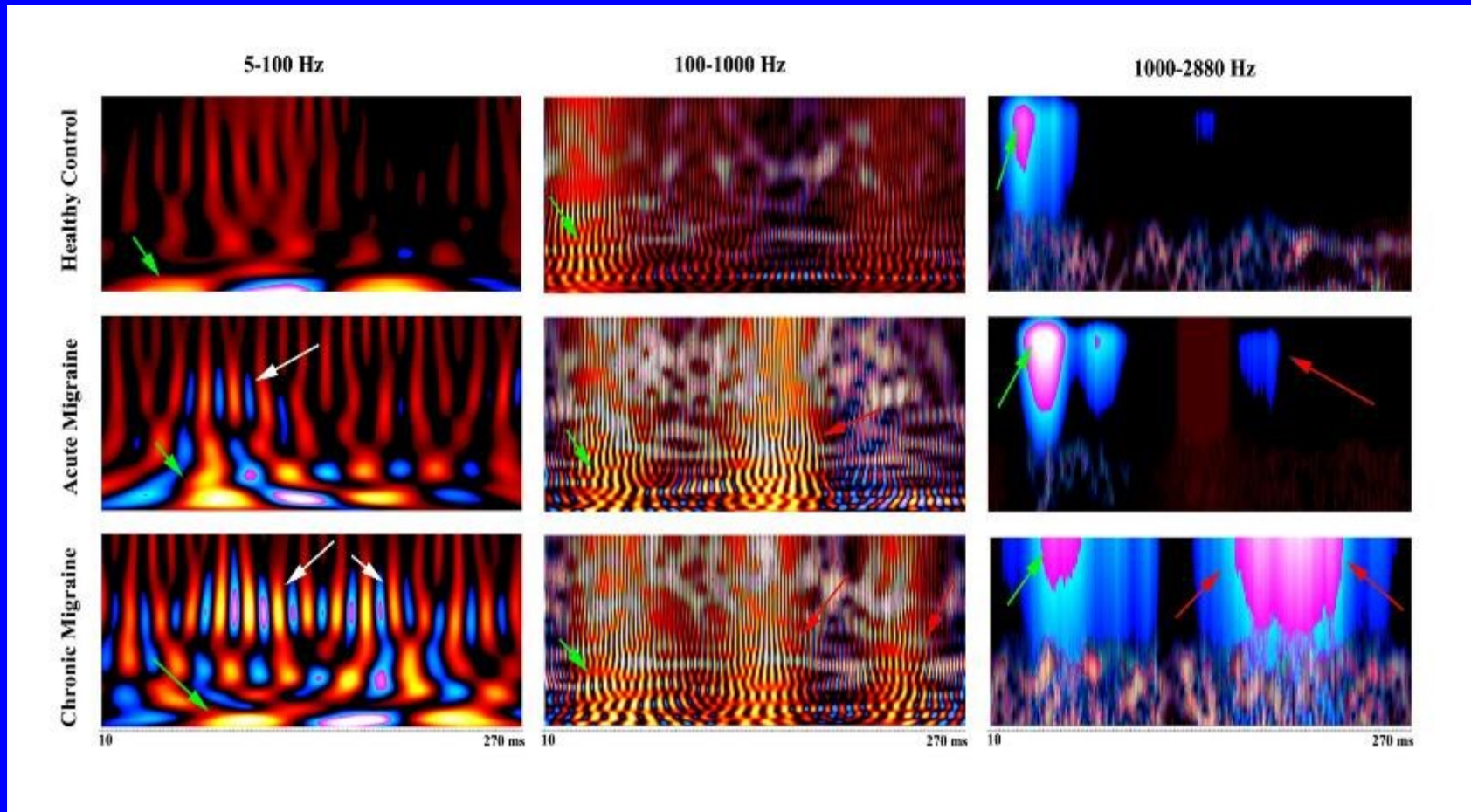
- **Auditory-motor paradigm:** Participants performed a brisk finger tapping task with both the right and the left index finger immediately after hearing a cue.



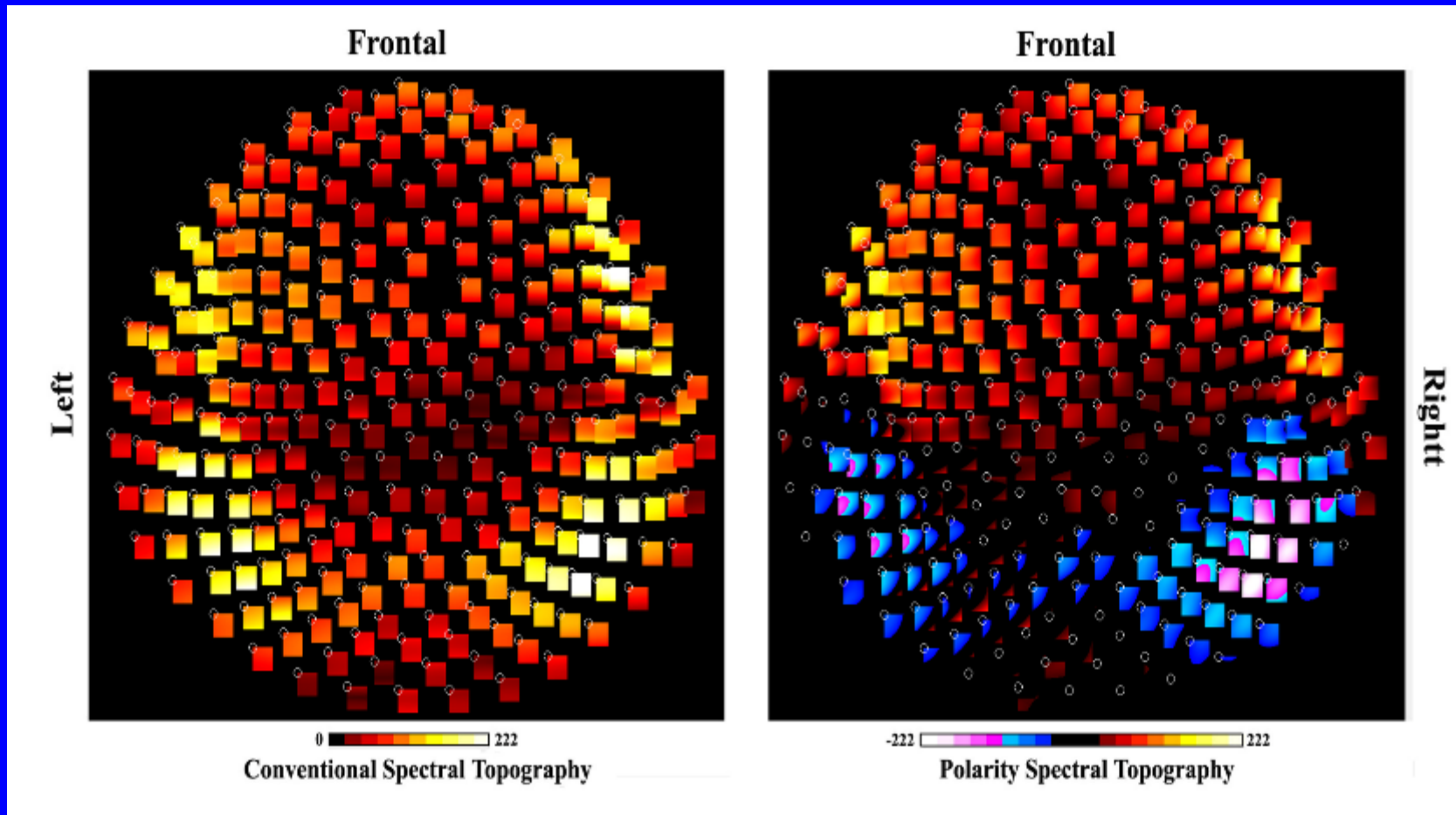
Average-> Time locked Signals Accumulation->Elicited Signals



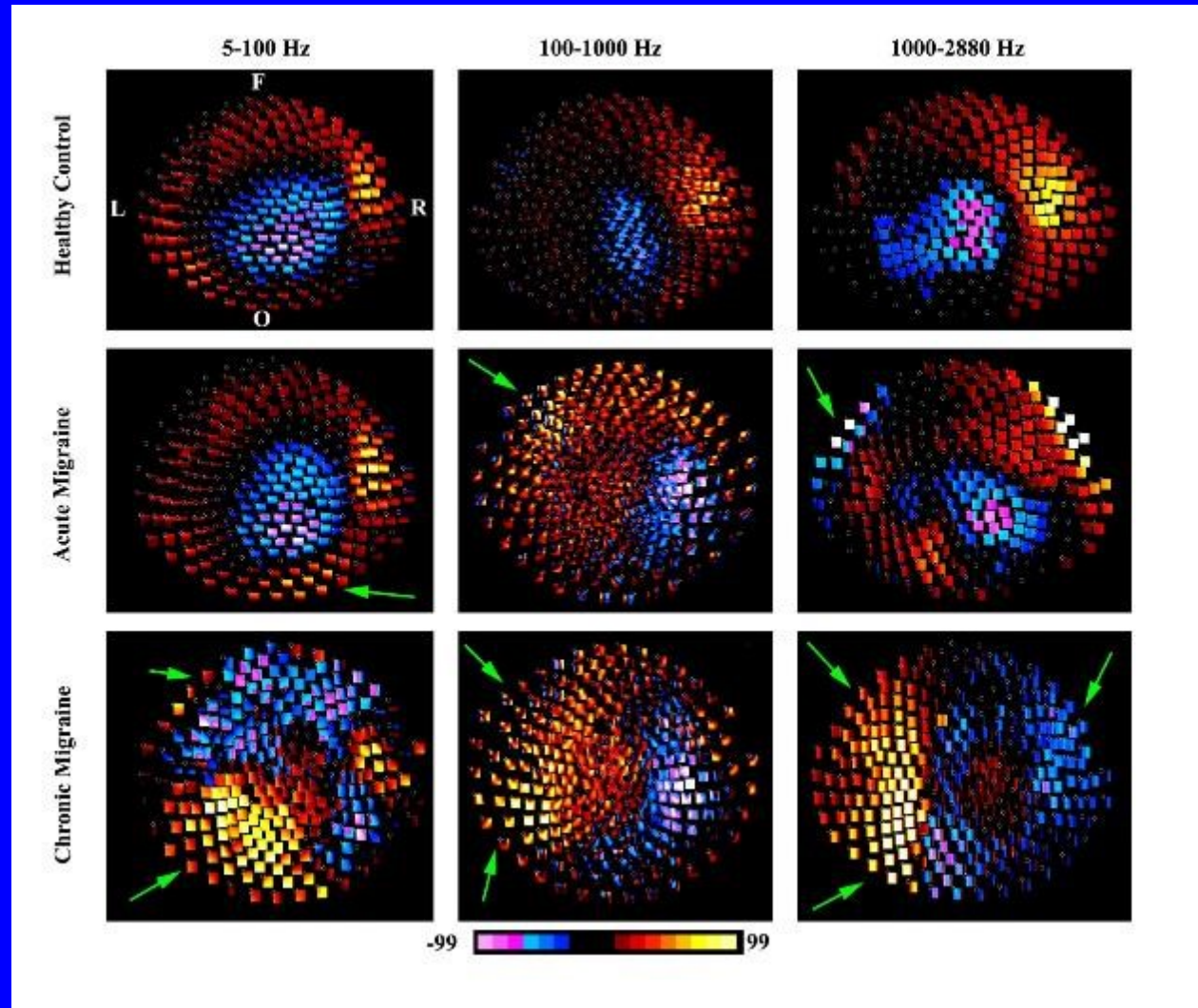
Average-> Time locked Signals Accumulation->Elicited Signals



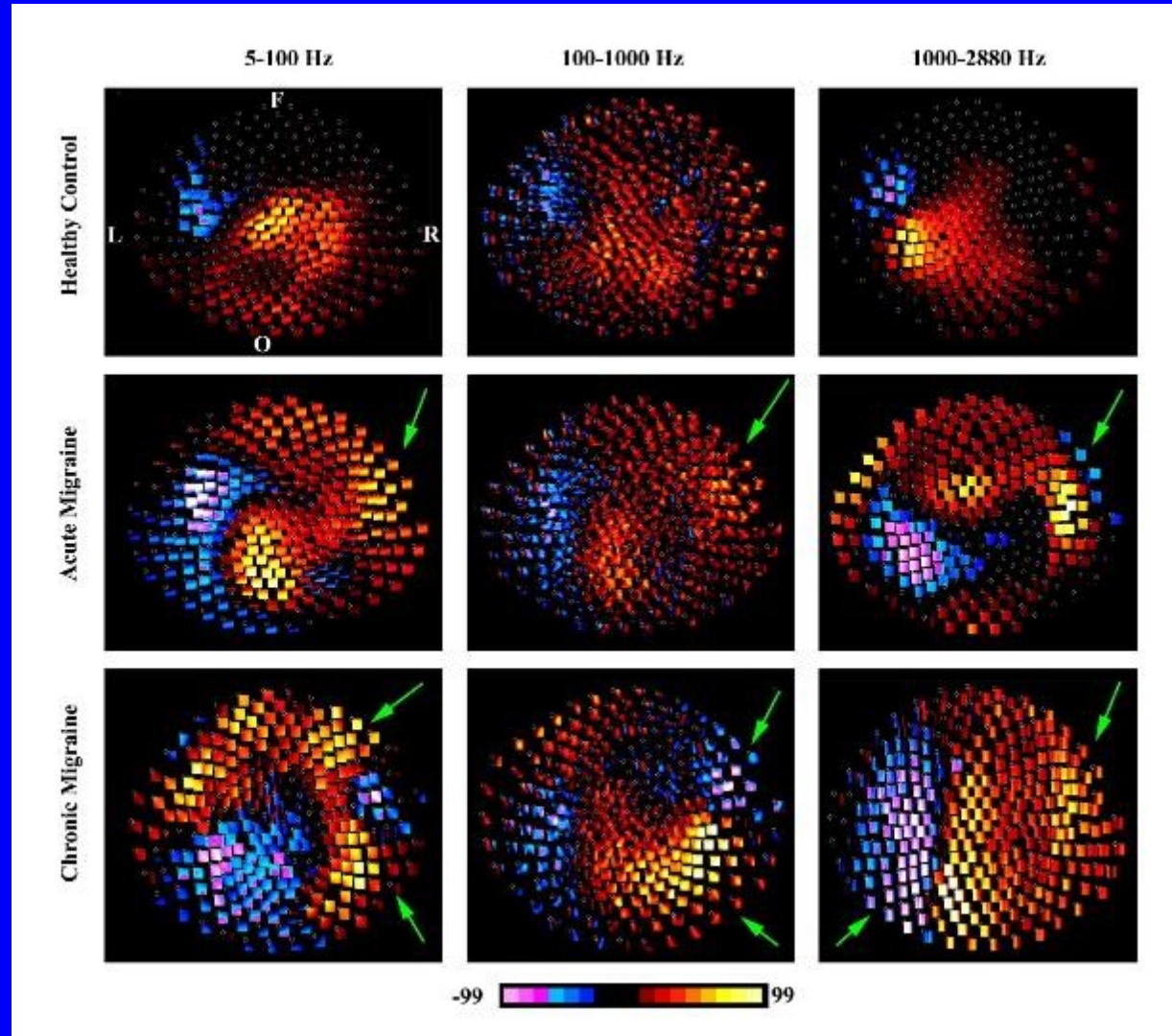
Spectrogram vs. Polarity Spectrogram



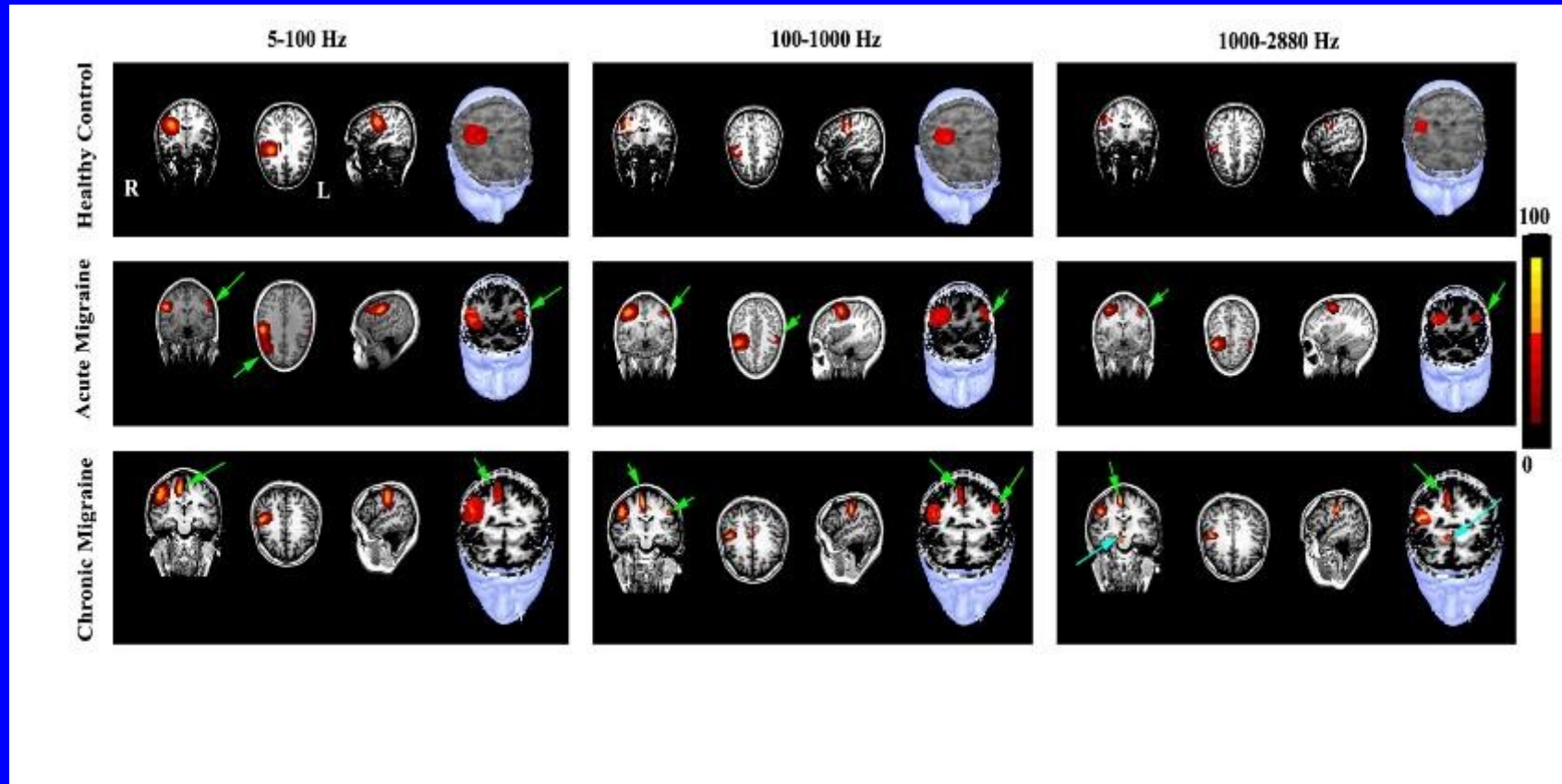
HFOs in Migraine



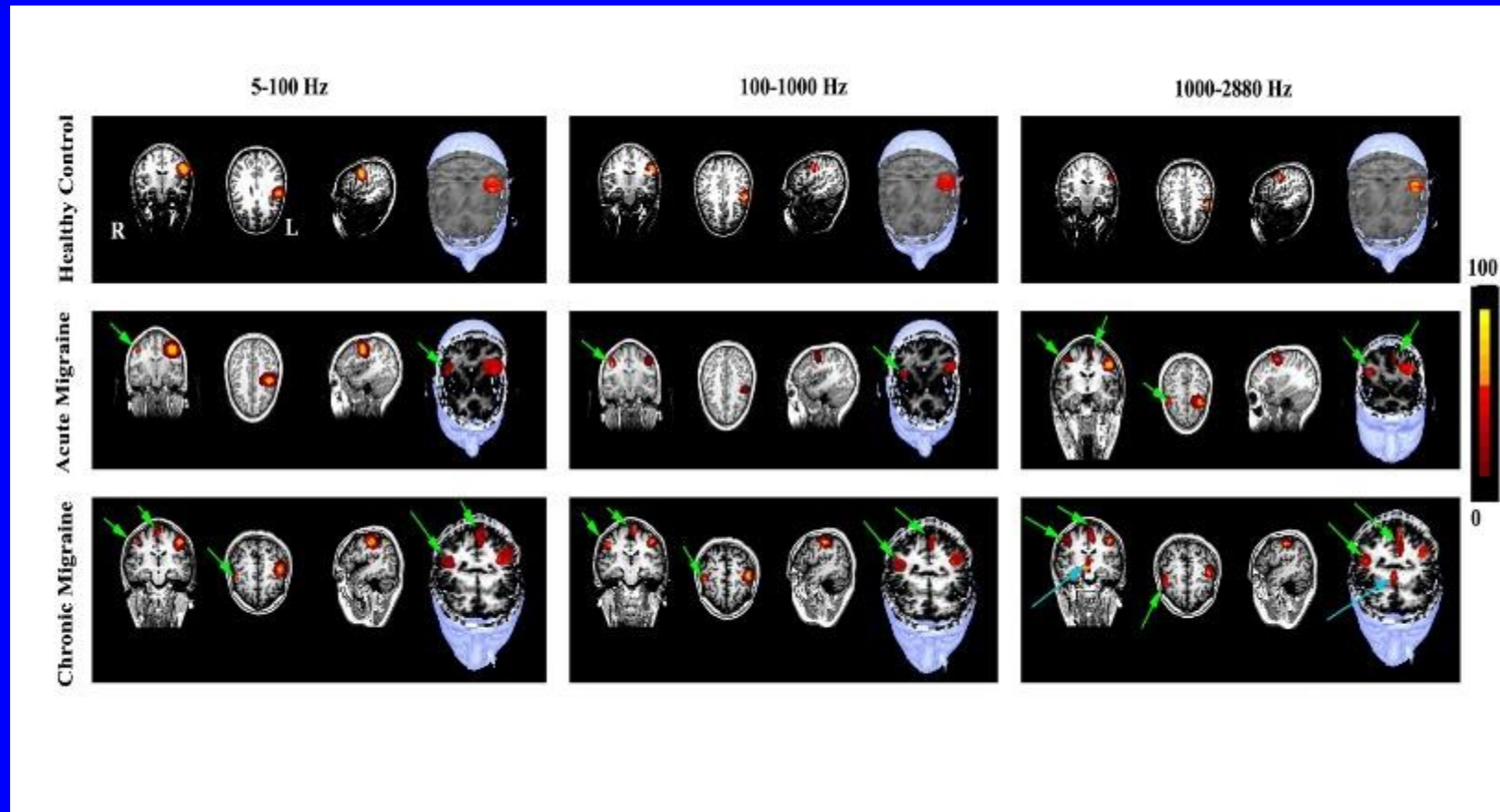
HFOs in Migraine



HFOs in Migraine

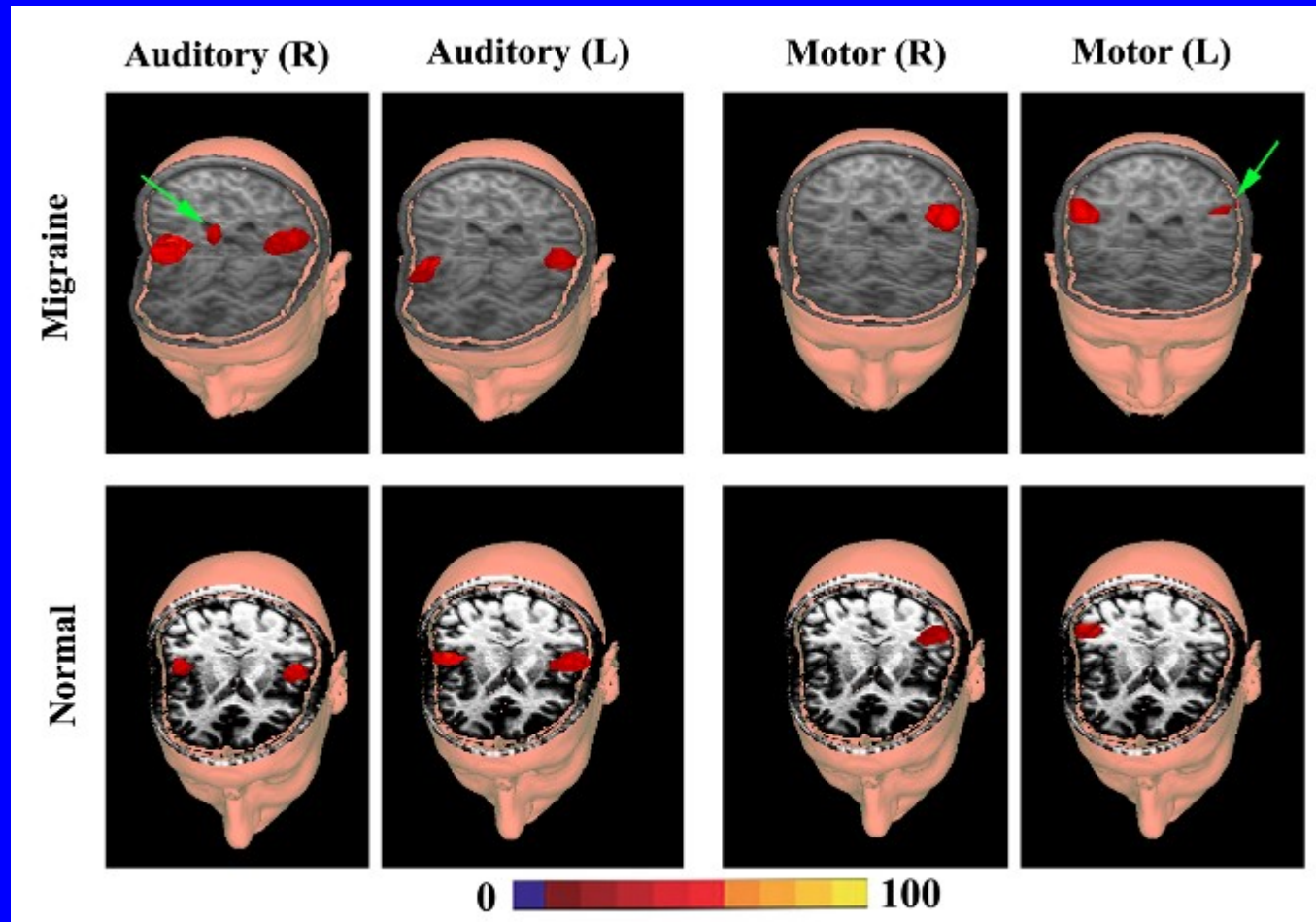


HFOs in Migraine



MEG Study of Acute Migraine

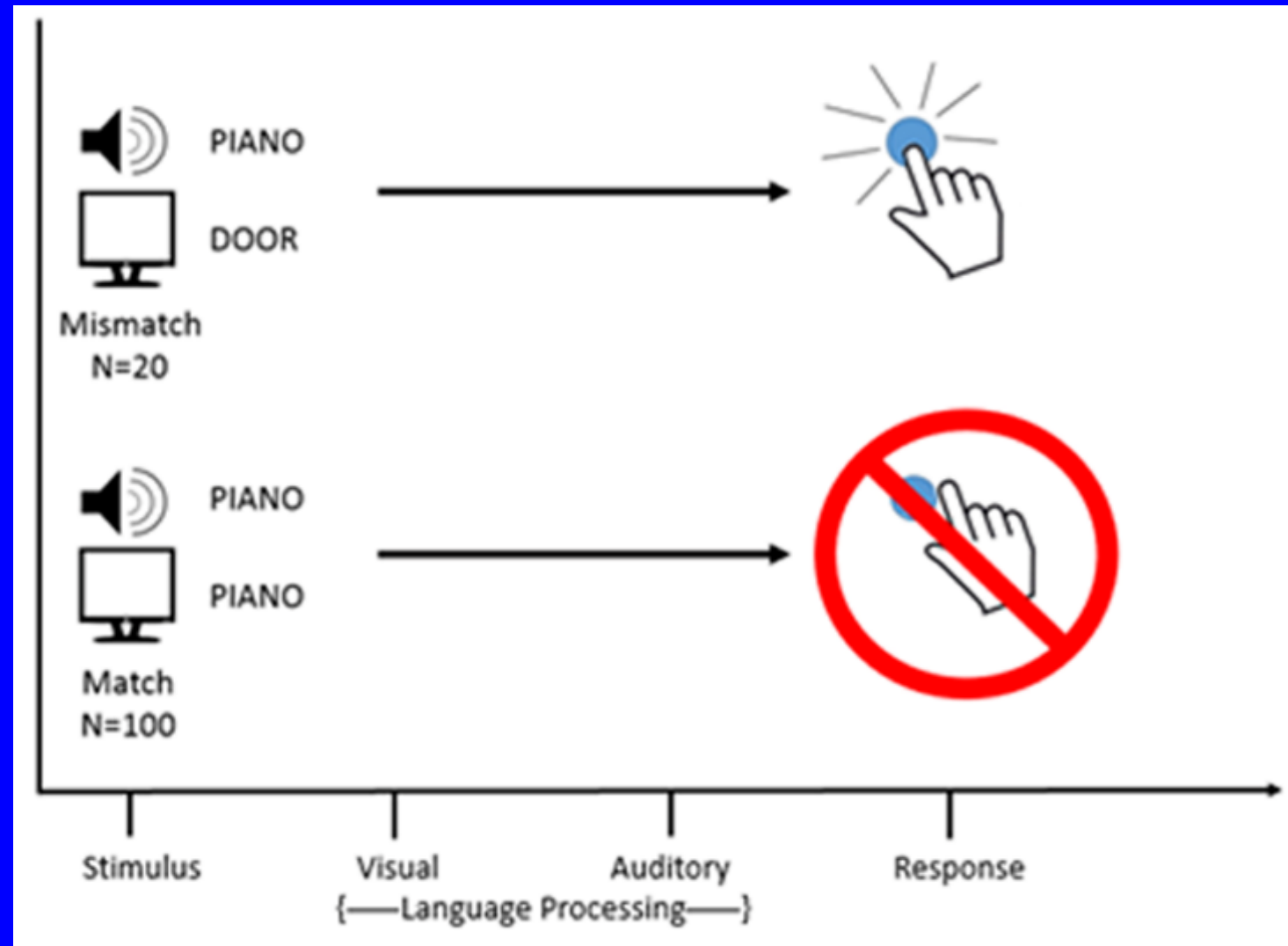
(Results-magnetic sources 100-1000 Hz)



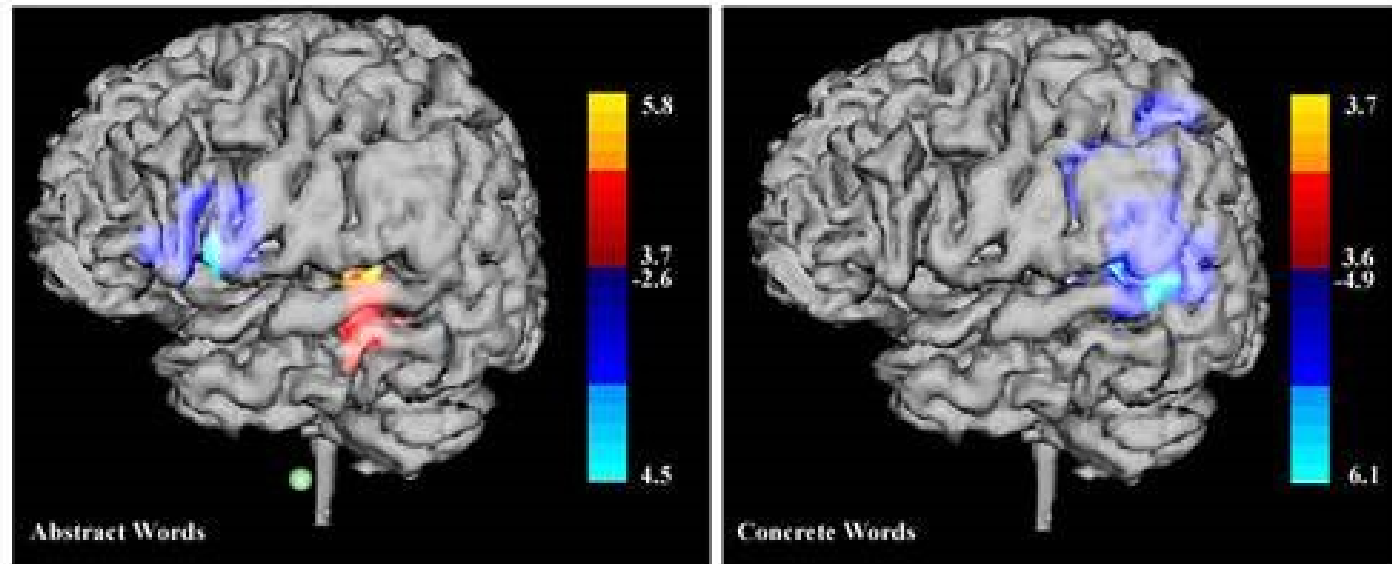
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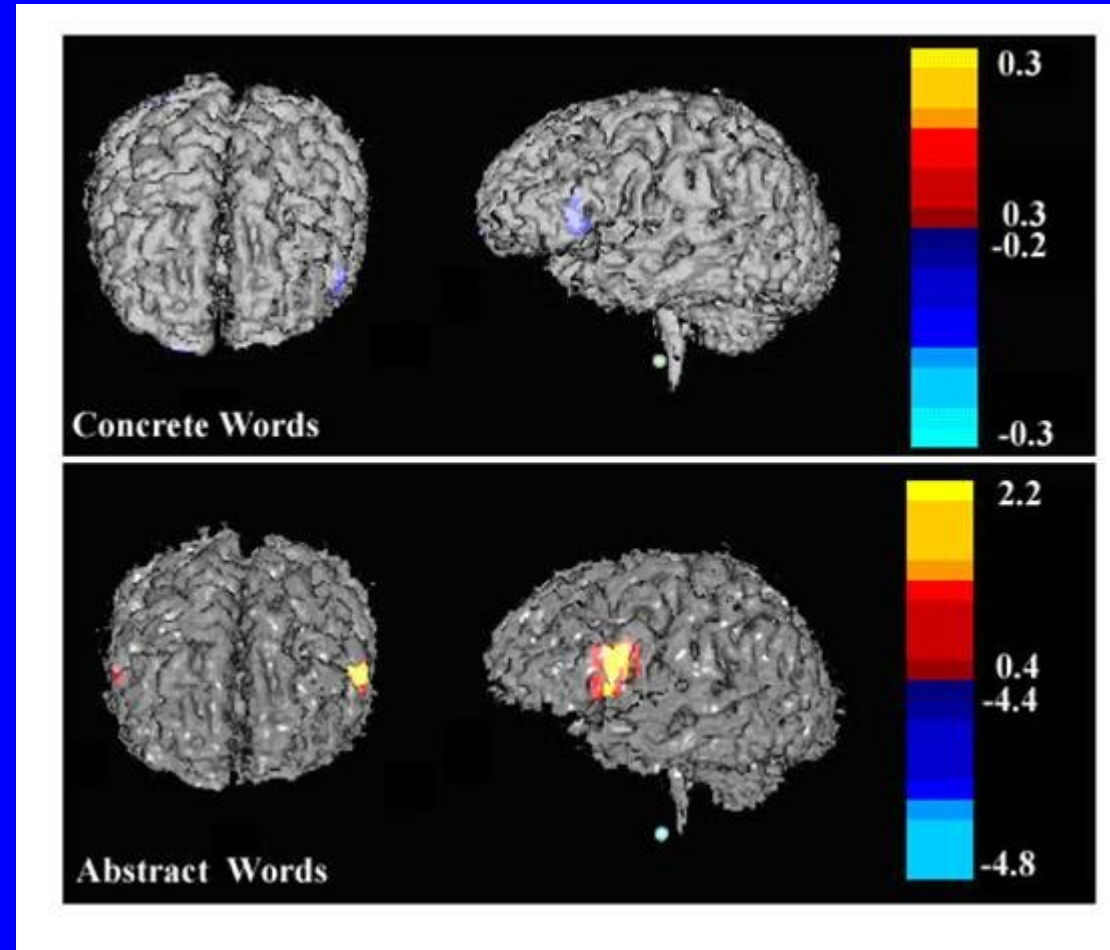
Word Comparison Task

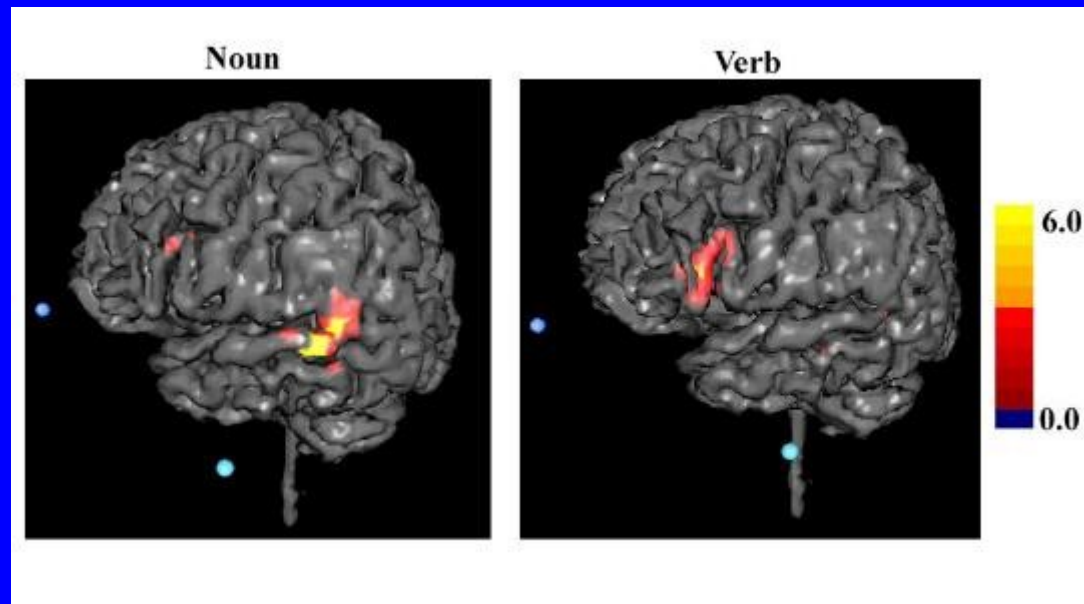
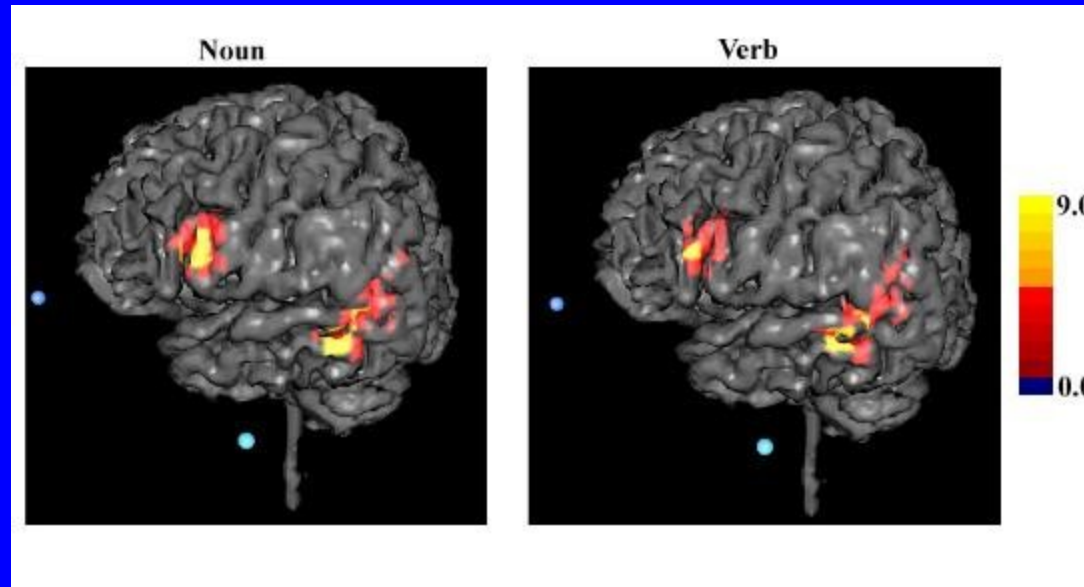


Results

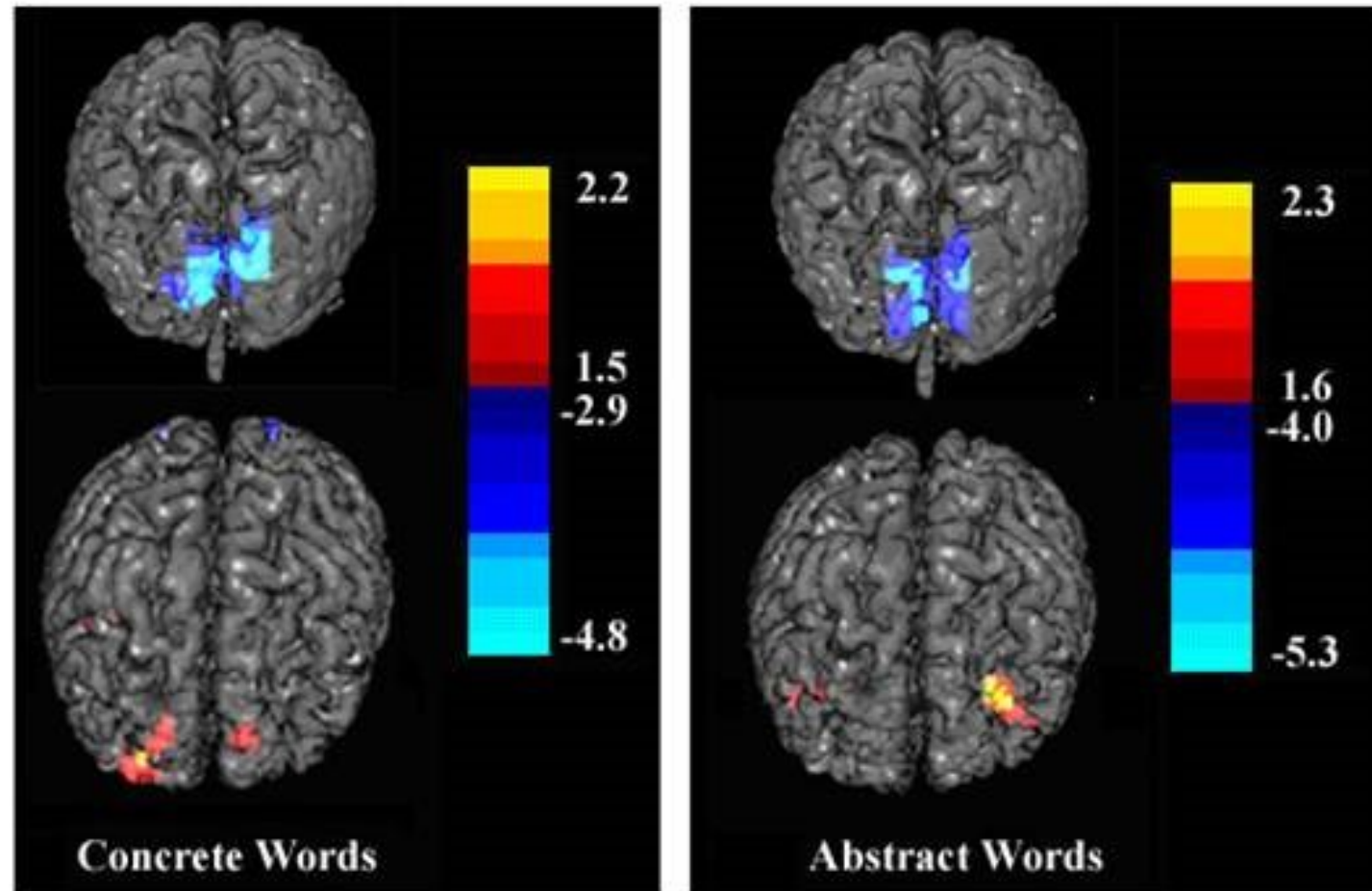


Results

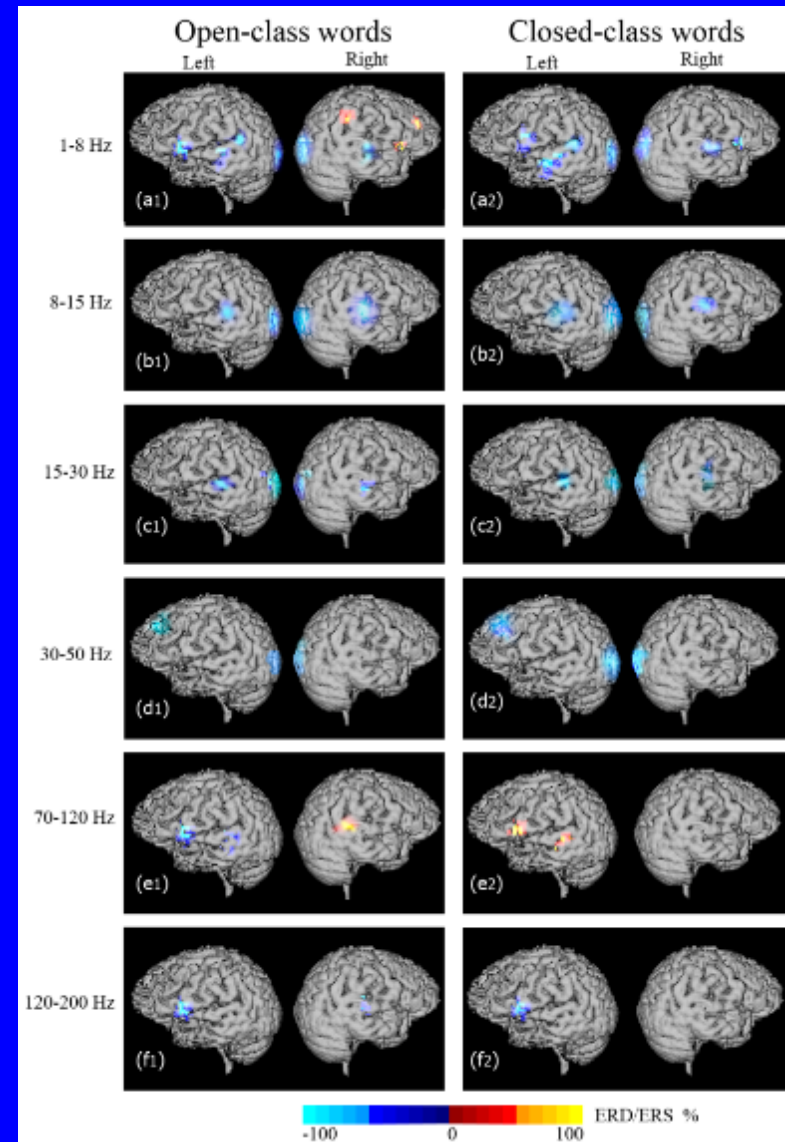




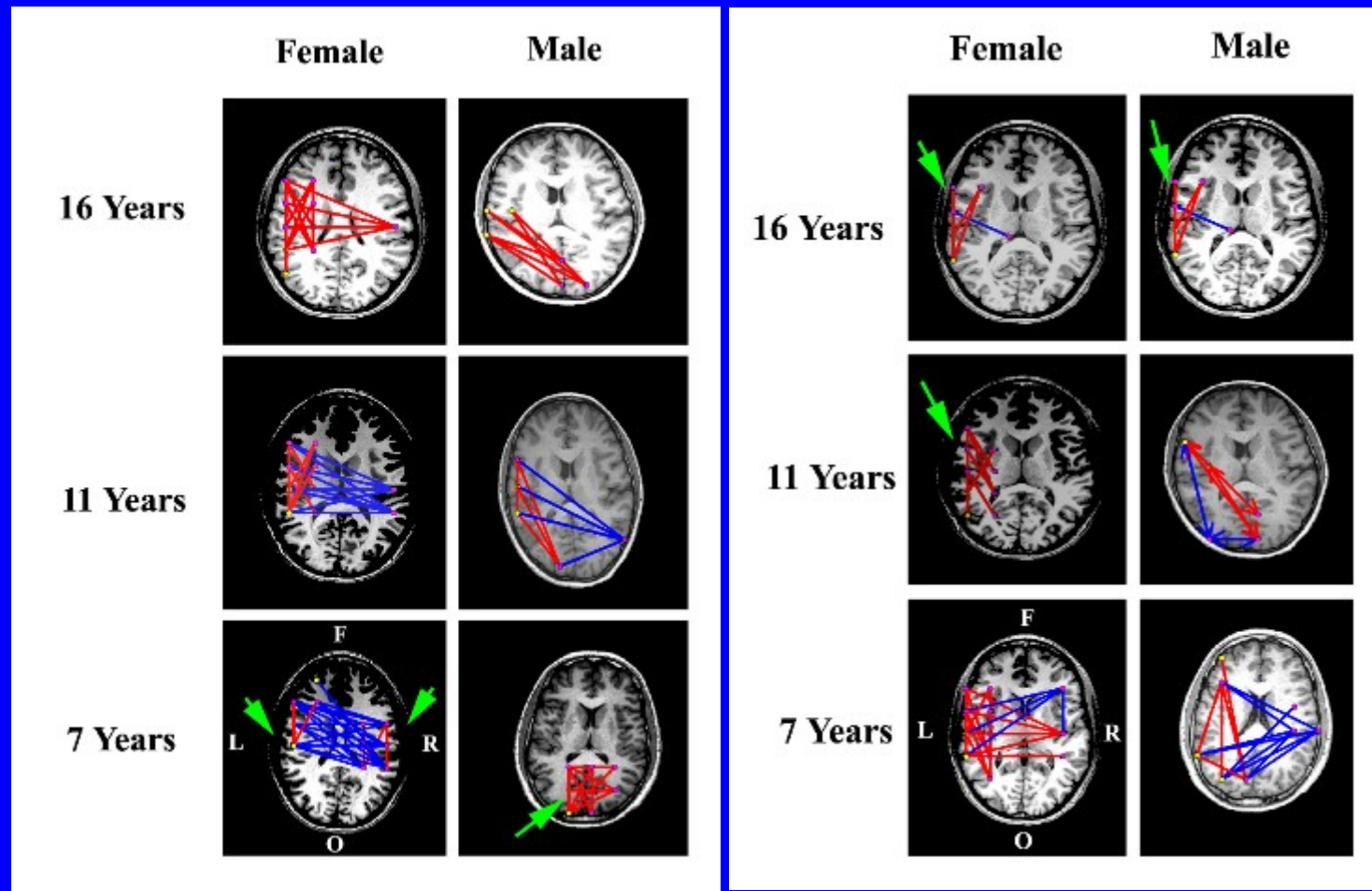
Results



HFOs in Language Mapping



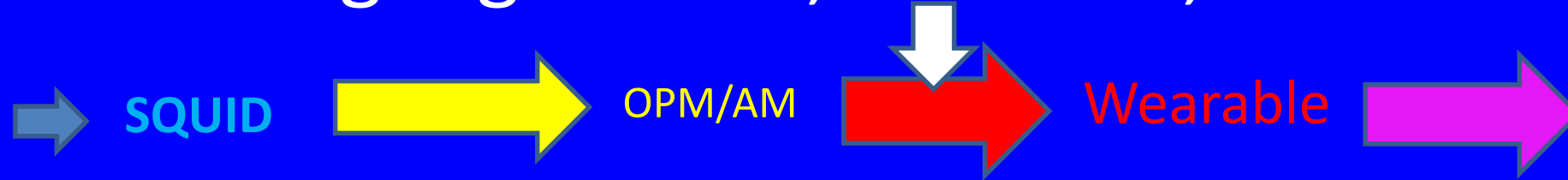
Development of Language Network



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 - Migraine
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New Technology for Brain Research Processing Algorithms, Software, Hardware



4 cm ↑ SQUID 300 ft
1 cm ↑ OPM 1600 ft

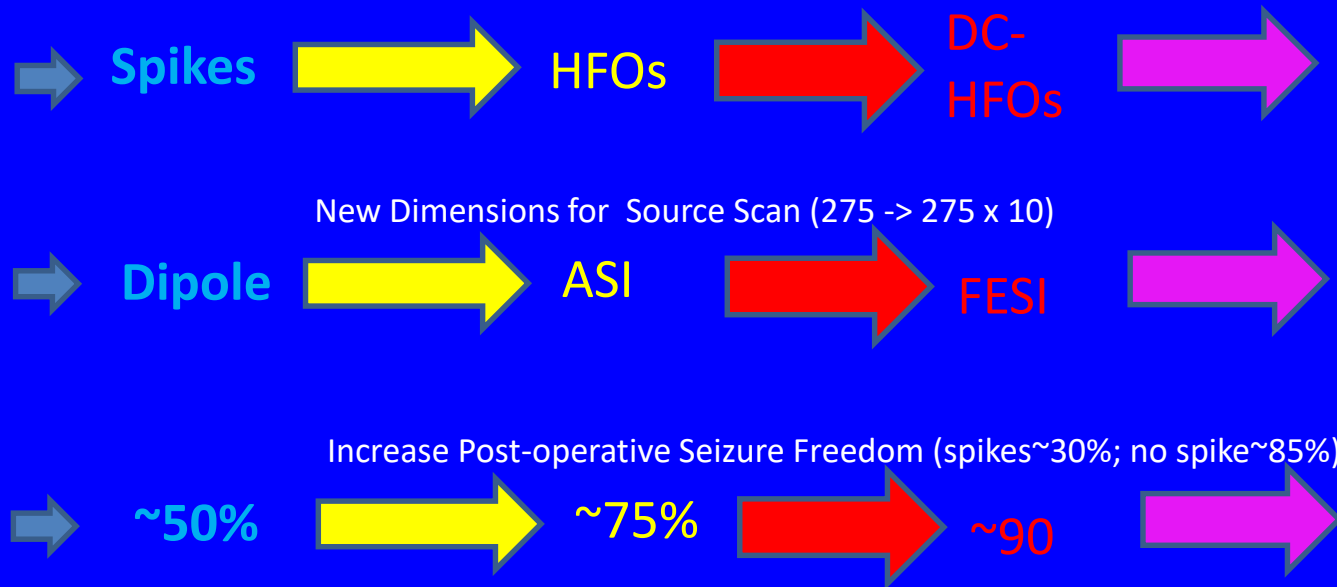
$$B_z = \frac{\mu_0}{4\pi} \frac{|\vec{Q}| \cdot |\vec{r} - \vec{r}_Q| \cdot \sin(\alpha)}{|\vec{r} - \vec{r}_Q|^3}$$

Hardware

Software and Algorithms

The Brain Generates HFBS

A New Frontier, Solve Clinical Problems



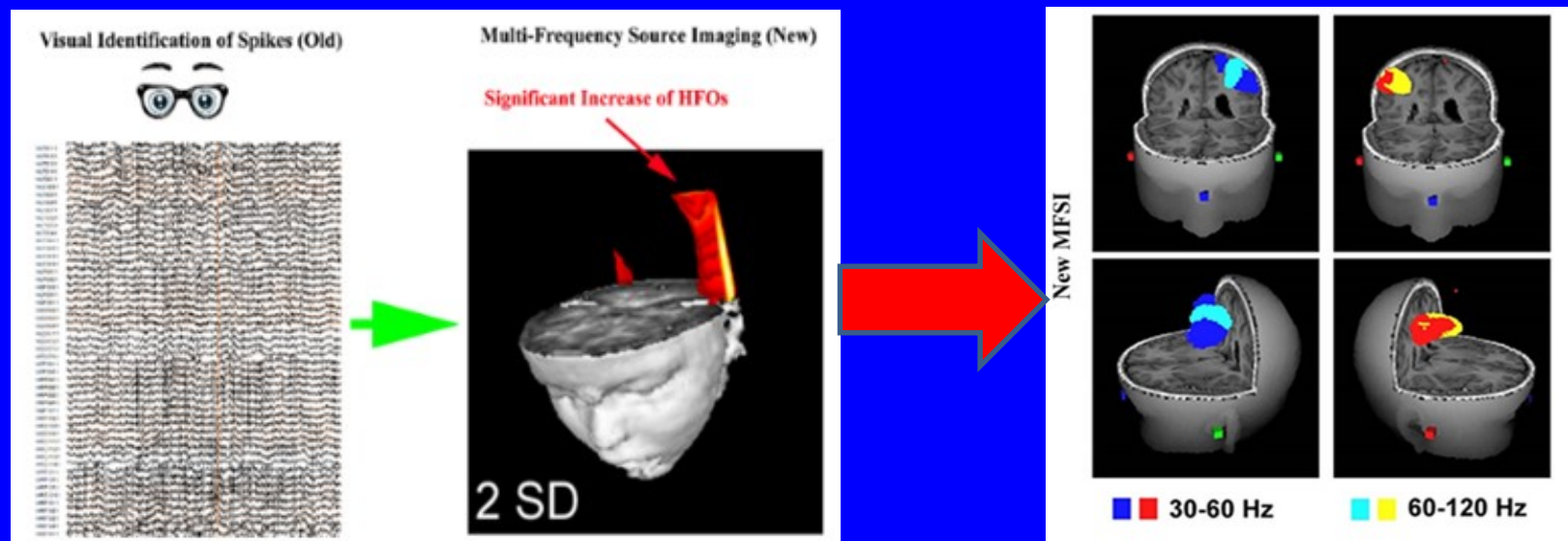
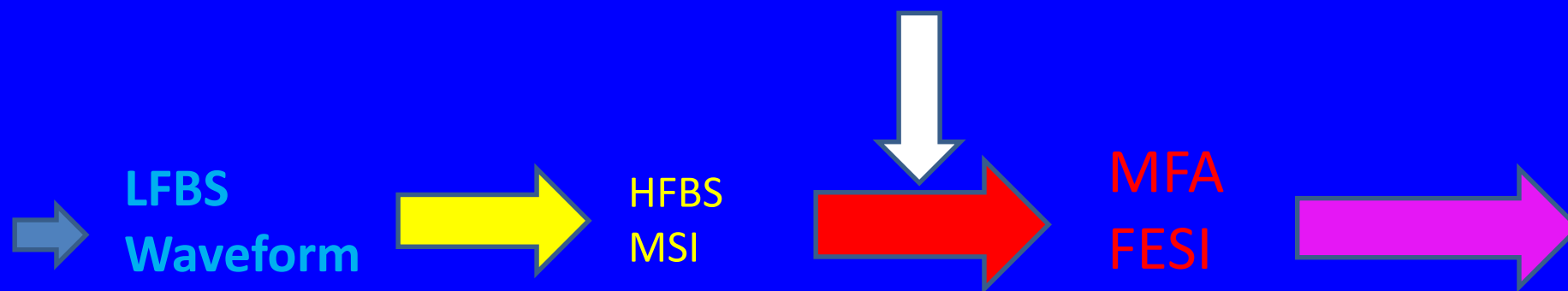
Epilepsy Success Stories

Puerto Rican Family...
At the near... wrong... a rare... uproc...

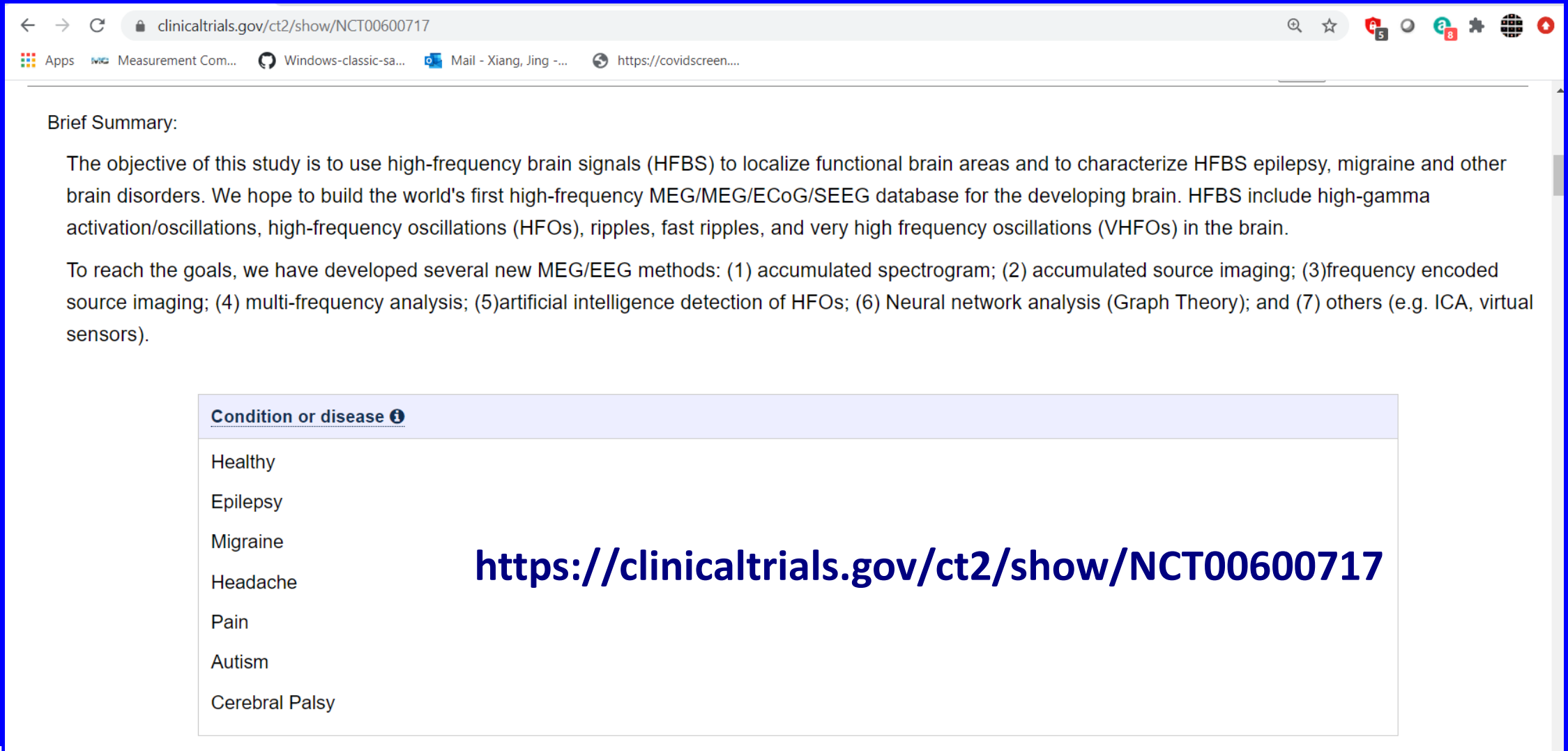
Stopping the Seizure...
At the them... used... free.

Frannie's Story
Frannie was born with tuberous s... different organs. When Fannie be... Cincinnati Children's for treatment

The Future of MEG Research



High Frequency MEG/EEG Database




The screenshot shows a web browser window with the URL clinicaltrials.gov/ct2/show/NCT00600717. The page content includes a "Brief Summary" section with two paragraphs of text. Below the summary is a table with a header "Condition or disease" and a list of conditions: Healthy, Epilepsy, Migraine, Headache, Pain, Autism, and Cerebral Palsy. A large blue URL is overlaid on the right side of the screenshot.

Brief Summary:

The objective of this study is to use high-frequency brain signals (HFBS) to localize functional brain areas and to characterize HFBS epilepsy, migraine and other brain disorders. We hope to build the world's first high-frequency MEG/MEG/ECOG/SEEG database for the developing brain. HFBS include high-gamma activation/oscillations, high-frequency oscillations (HFOs), ripples, fast ripples, and very high frequency oscillations (VHFOs) in the brain.

To reach the goals, we have developed several new MEG/EEG methods: (1) accumulated spectrogram; (2) accumulated source imaging; (3) frequency encoded source imaging; (4) multi-frequency analysis; (5) artificial intelligence detection of HFOs; (6) Neural network analysis (Graph Theory); and (7) others (e.g. ICA, virtual sensors).

Condition or disease 
Healthy
Epilepsy
Migraine
Headache
Pain
Autism
Cerebral Palsy

<https://clinicaltrials.gov/ct2/show/NCT00600717>

Acknowledgements

NIH R21 NS 104459

Ohio Third Frontier TEGG20170361

CCHMC Innovation Fund

NIH R21 NS081420-01A1

NIH R21 NS072817

NIH R01 HD38578

NIH K23 MH100640-01A1

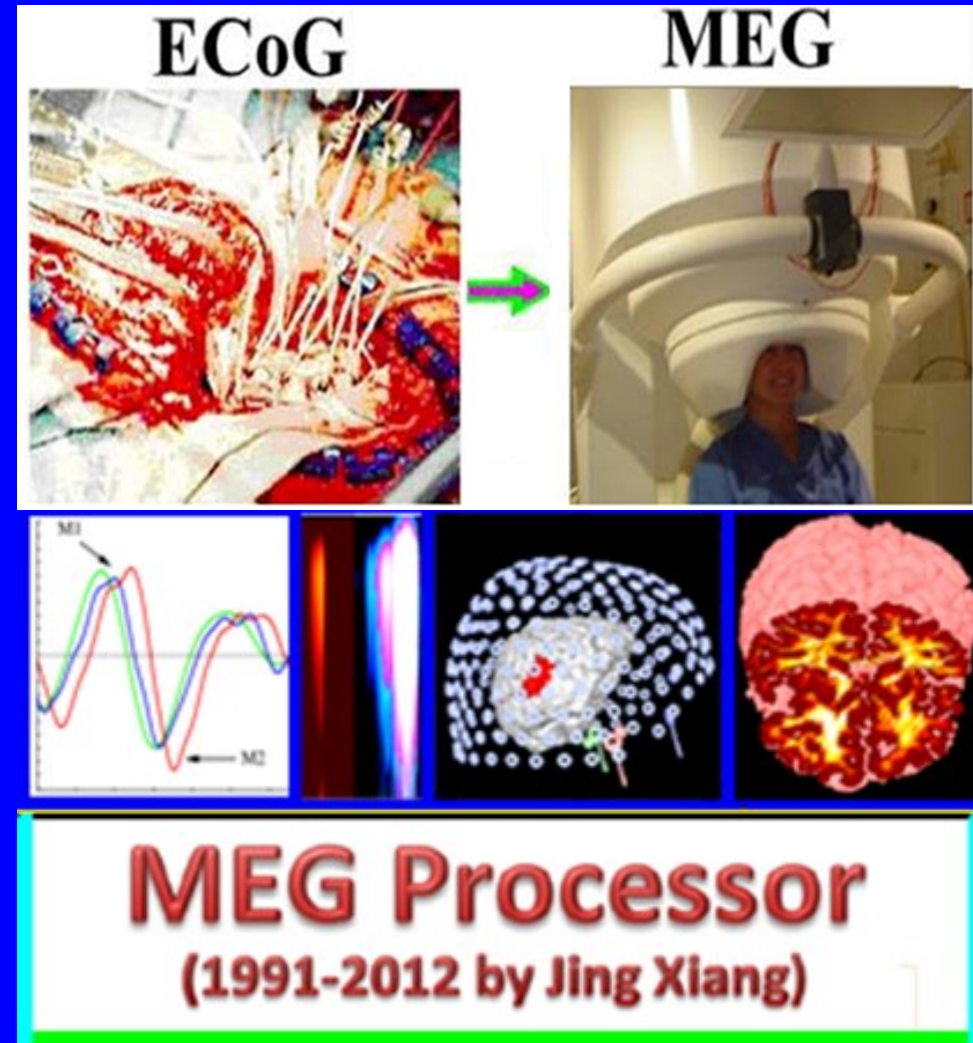
NIH 1K23MH108603-01

Shared Facility Discovery Award (SFDA)

Arnold Strauss Fellow Award

BRIMS Scholar

Trustee Grants CCHMC

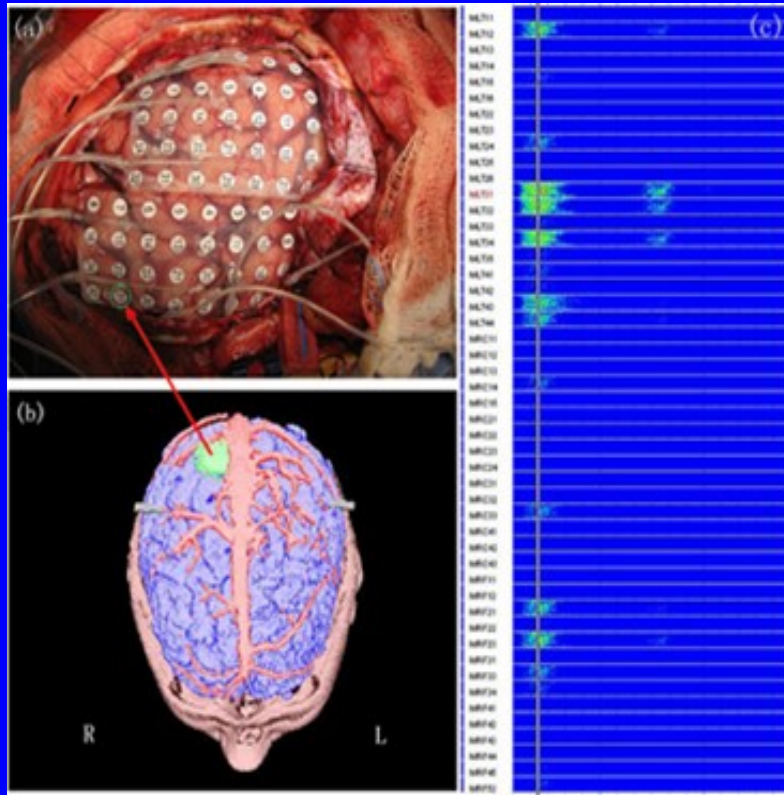


Thank you 😊



Discussion (New Area, Bright)

(Biomag, USA Clinical MEG, ASCMA)



2nd
international
workshop on
High Frequency
Oscillations in Epilepsy
A scientific and teaching workshop



10-12 • March • 2016
Freiburg im Breisgau
Germany

The New MEG Frontier?

Organizer: Jing Xiang

Room: # 104

Time: 13:30-14:30

Symposium Summary

Biomag2016

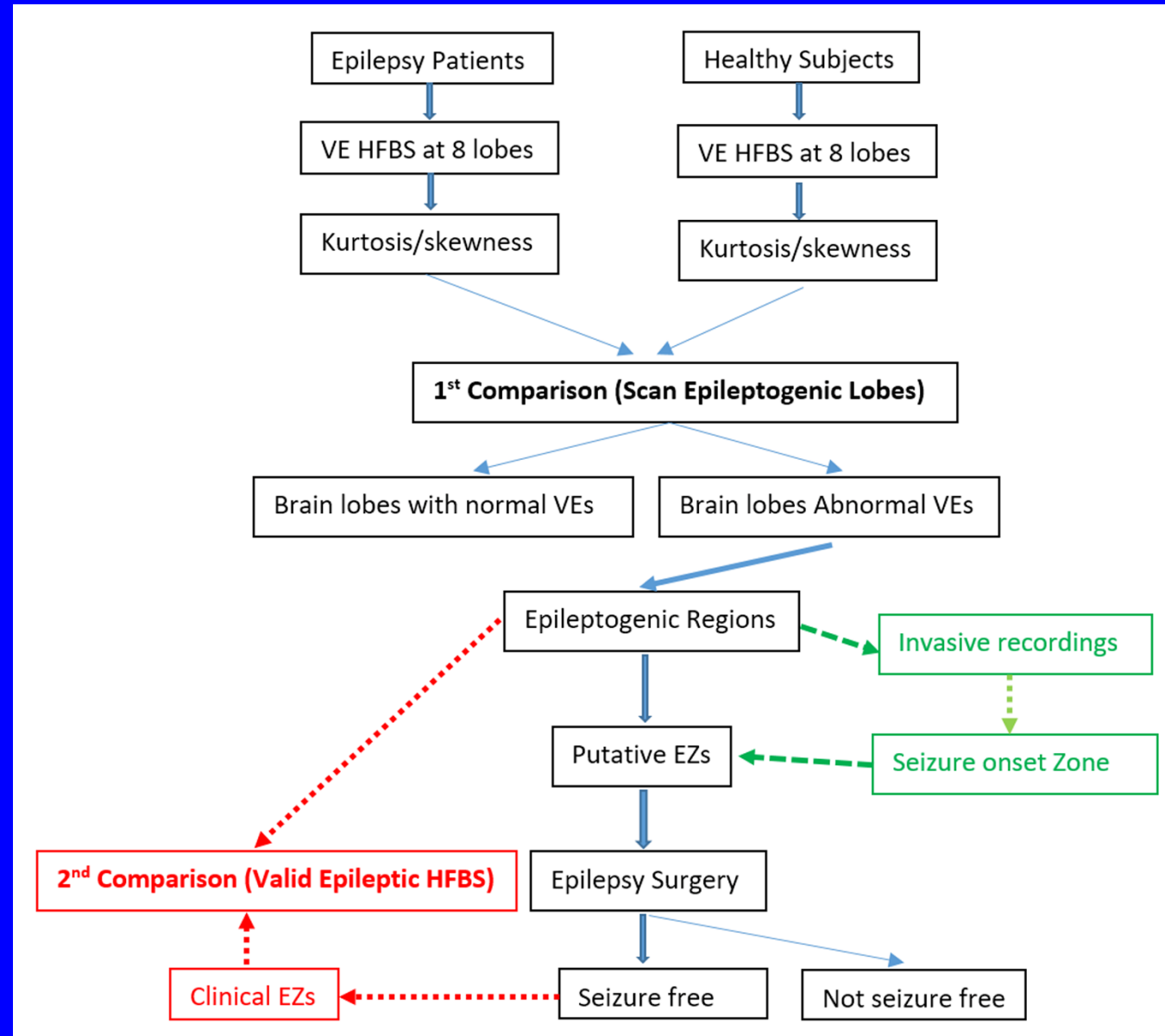
MEG Detection of Low to High Frequency Neuromagnetic Activity

Recent success in localizing low- (LFBS, 0-14 Hz) and high-frequency brain signals (HFBS, 70-2,8 of epilepsy, migraine and potentially many other disorders using magnetoencephalography is interesting because both clinicians and basic researchers can benefit from it. For example: (1) effectiveness of epilepsy surgery by approximately 30%. By promoting the applications of HF intractable epilepsy patients being seizure free. (2) By using LFBS and HFBS, MEG has revealed cortical excitability and that medications normalizing cortical excitability can reduce the incidence of m and HFBS can advance our understanding of the cerebral mechanisms of multi-frequency brain software developers may use LFBS and HFBS to create novel solutions for diagnosis and treatment.

Speakers:

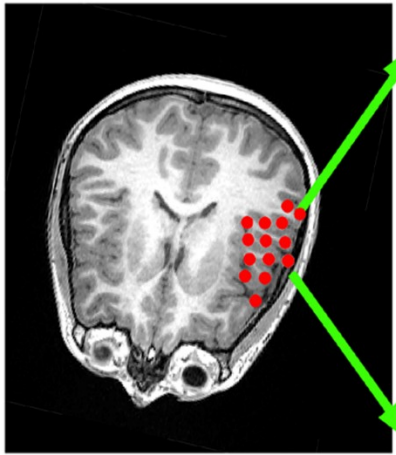
- Milena Korostenskaja (Florida Hospital for Children, USA)
"High Gamma Functional Mapping for epilepsy surgery"
- Kimberly A. Leiken (Cincinnati Children's Hospital Medical Center, USA)
"Assessment of Cortical Excitability in Migraine with Neuromagnetic High-frequency Signals"

Detect HFBS with VE and Kurtosis/Skewness



Virtual Sensor + Kurtosis/Skewness

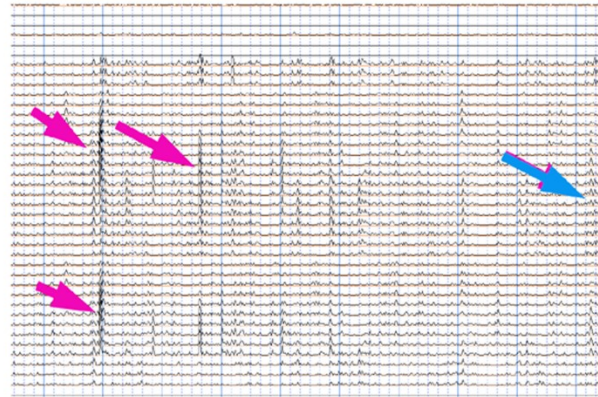
Epilepsy



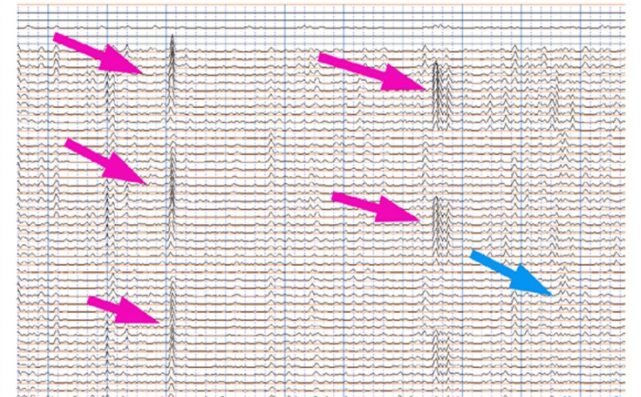
2-80 Hz (Spikes)



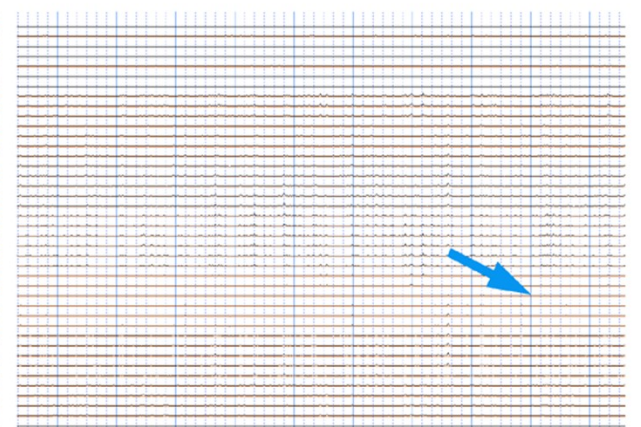
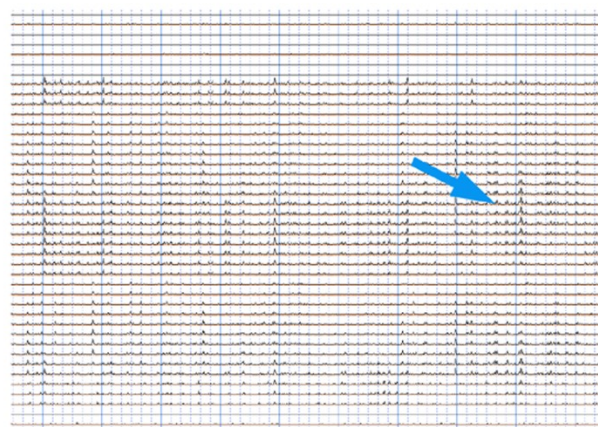
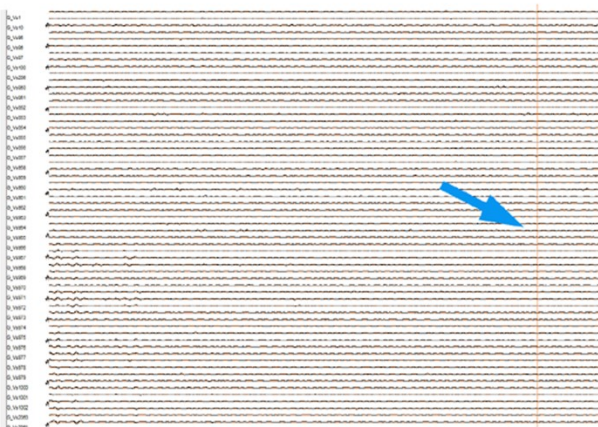
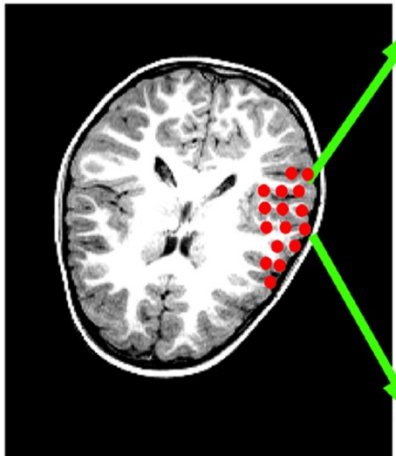
80-250 Hz (Ripples)

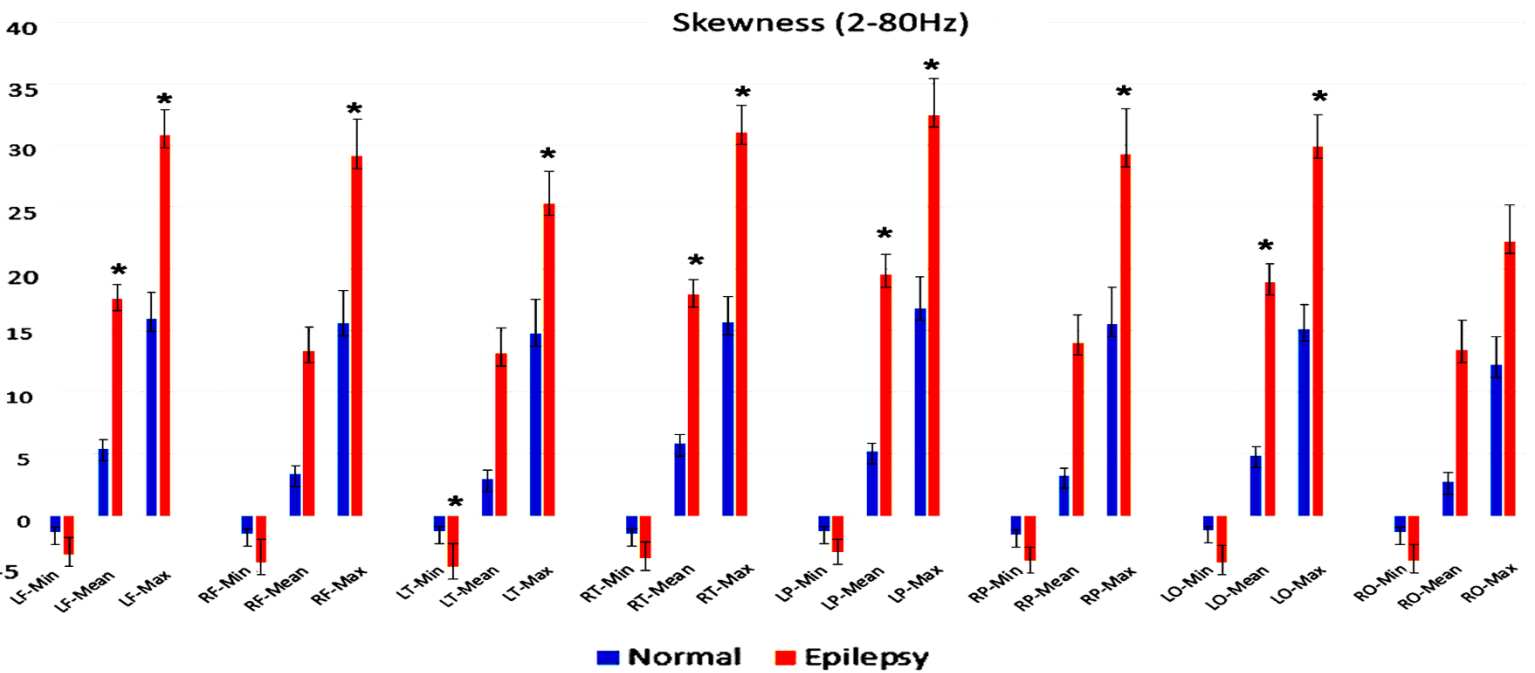
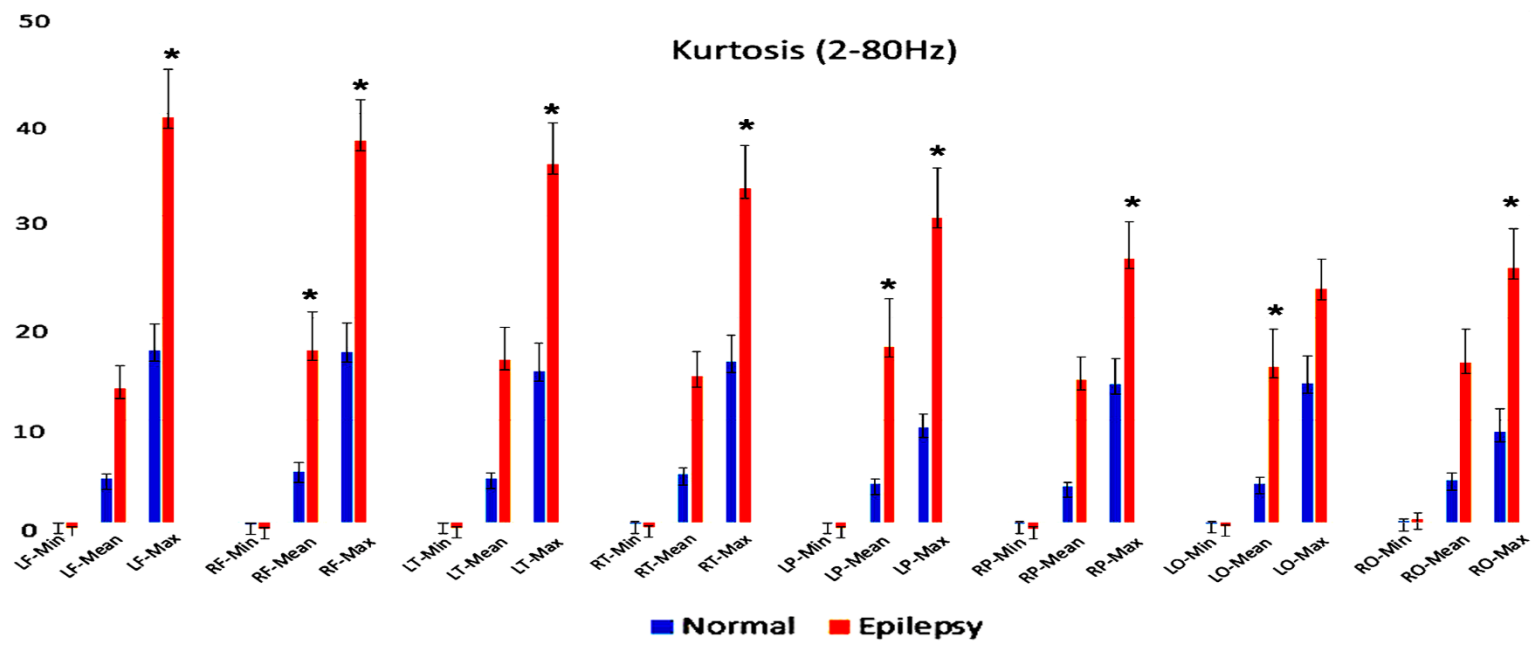


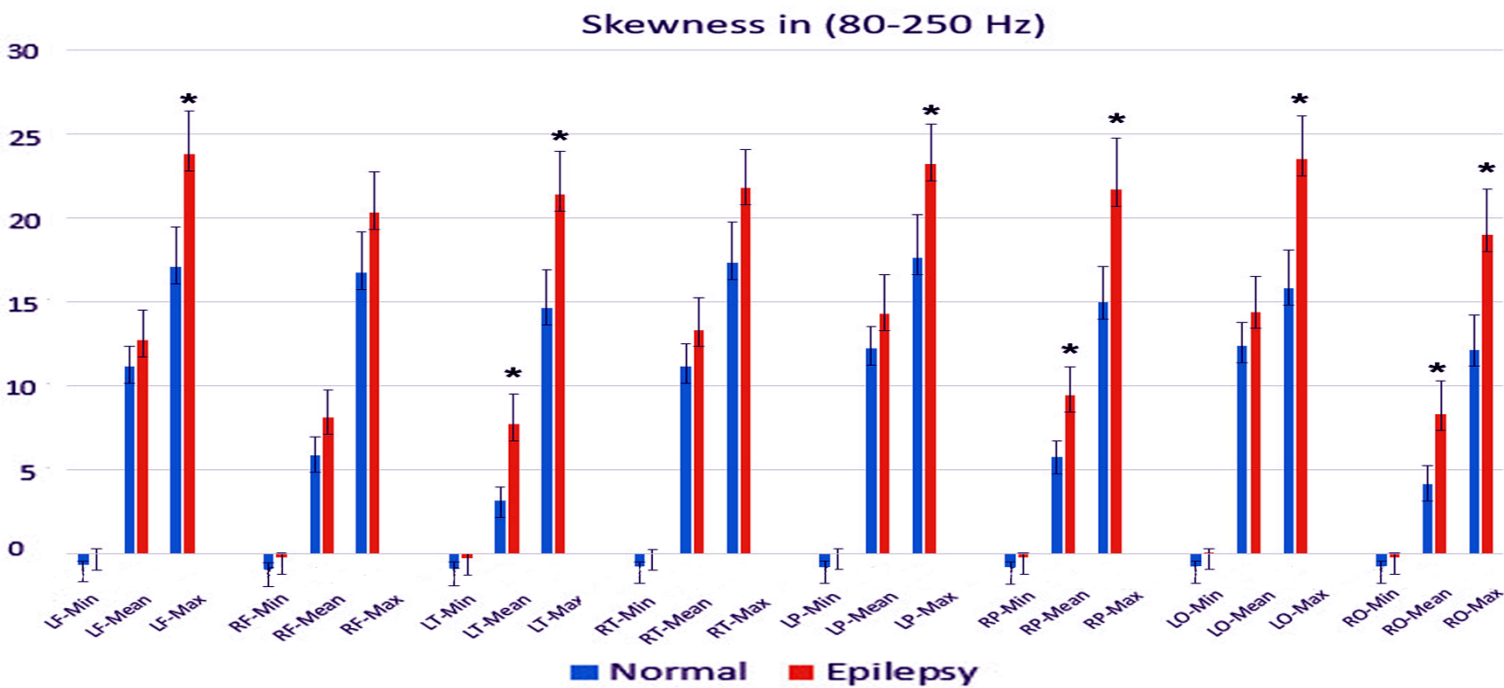
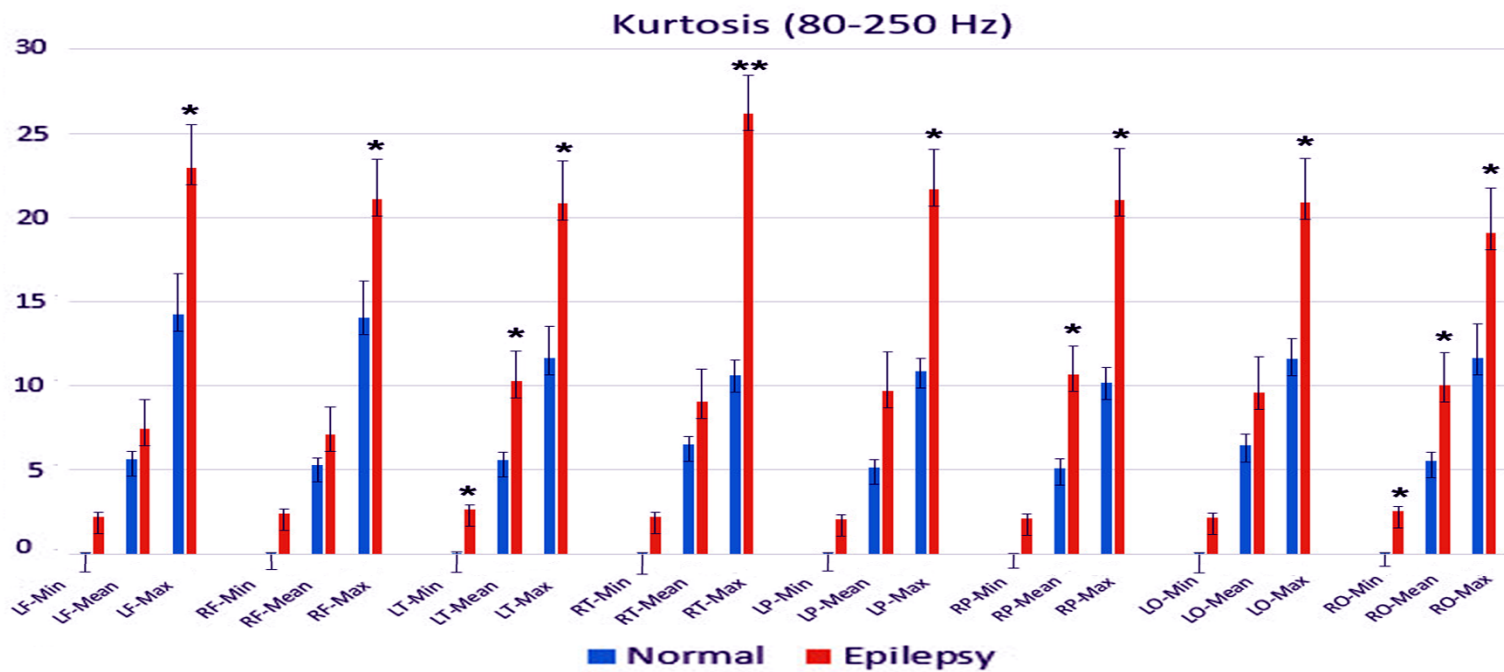
250-600 Hz (Fast Ripples)

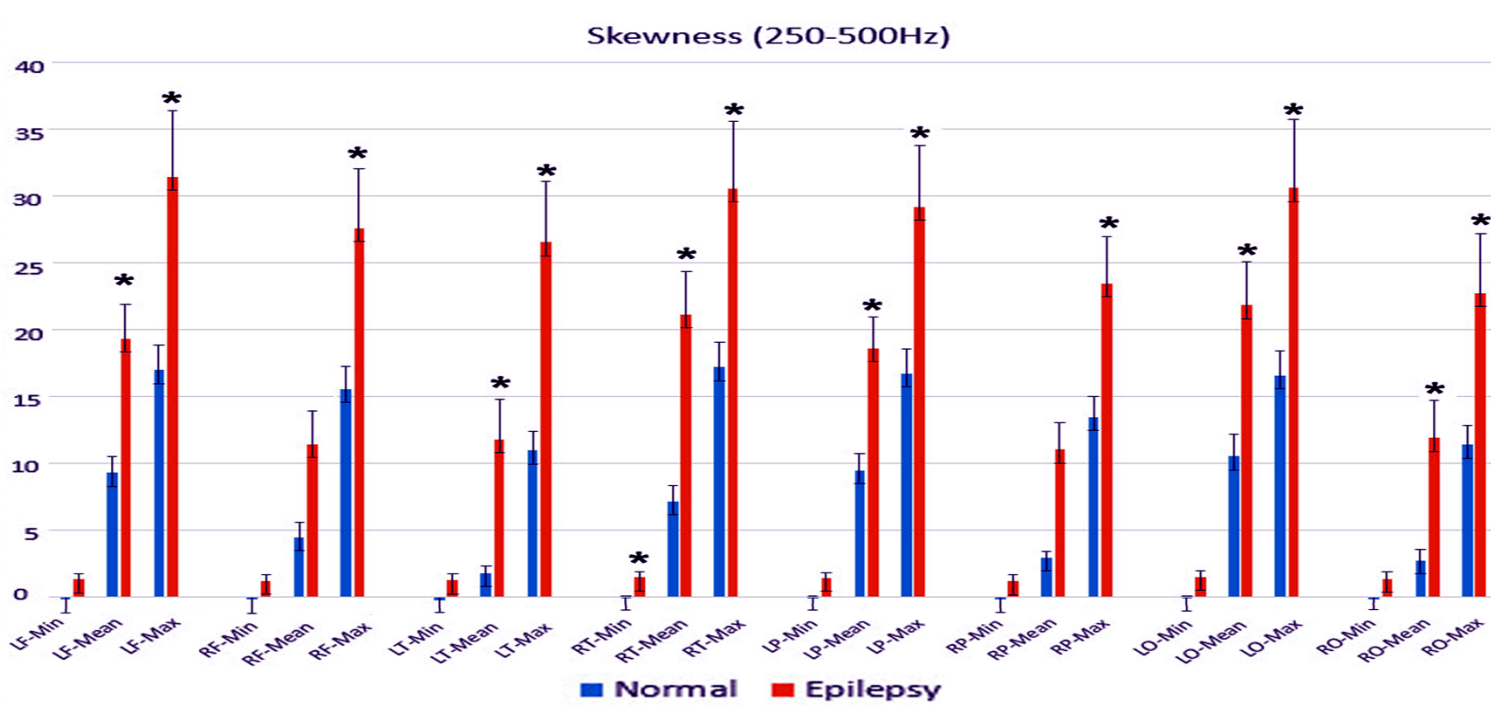
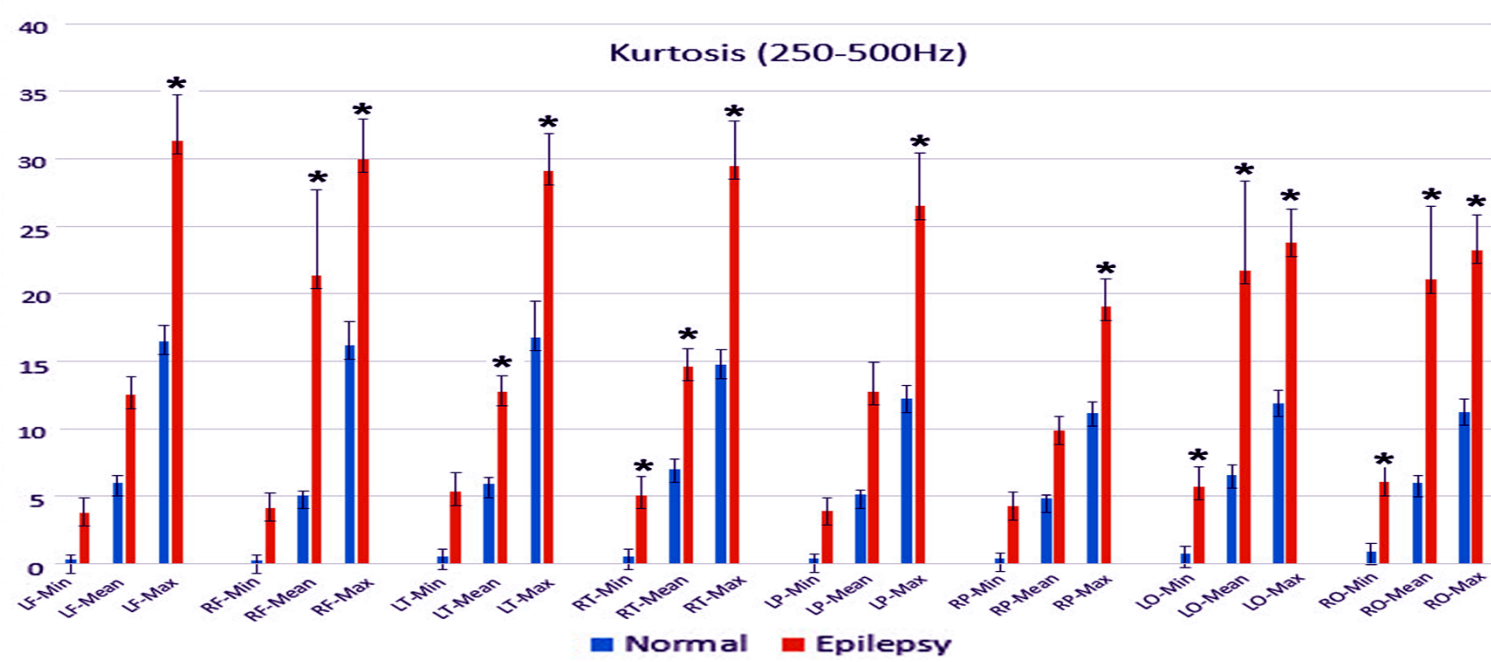


Normal

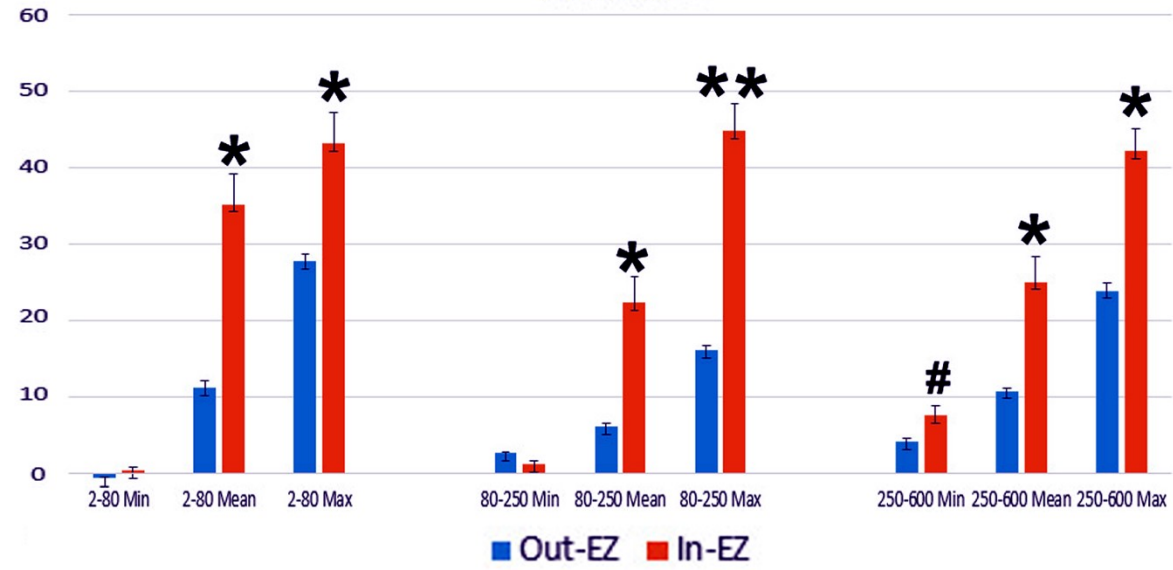




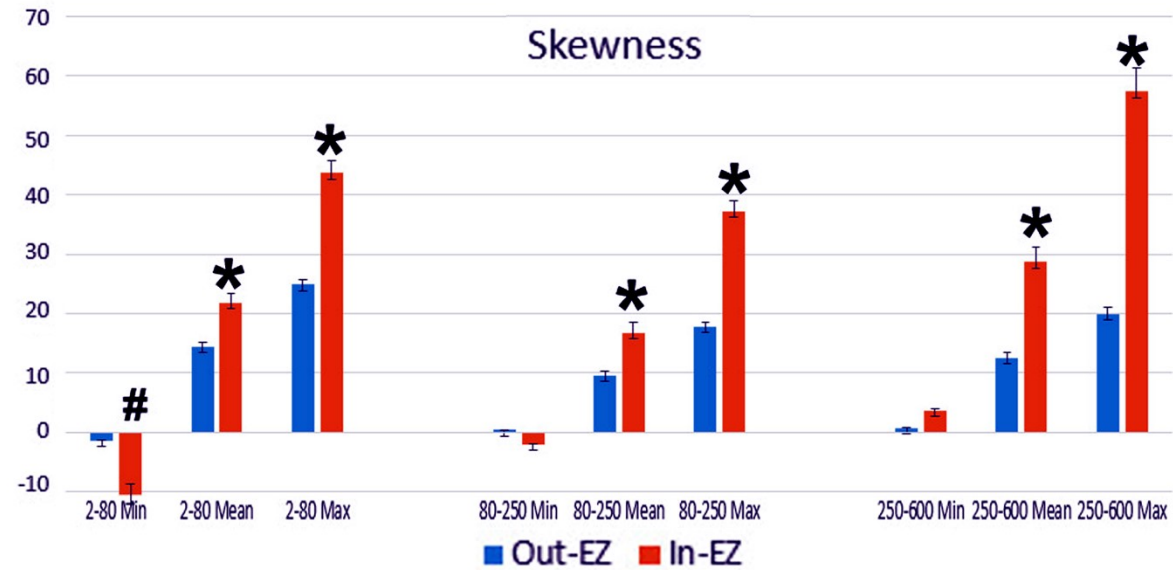


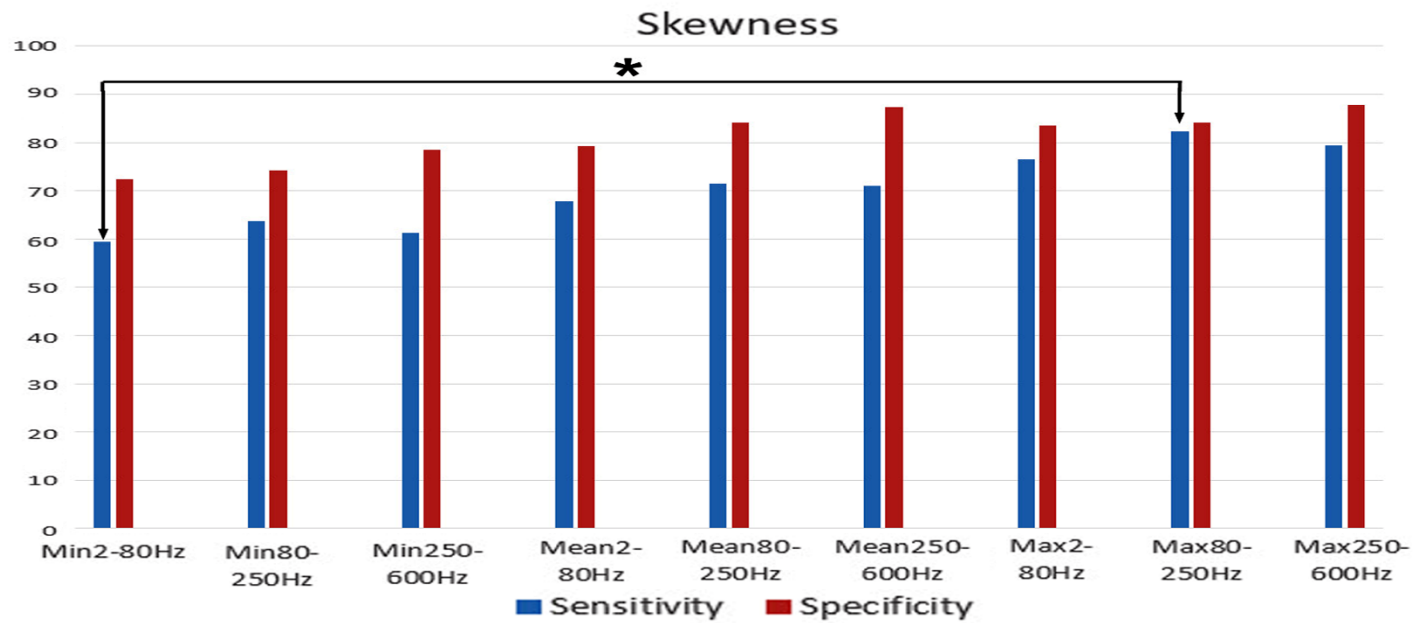
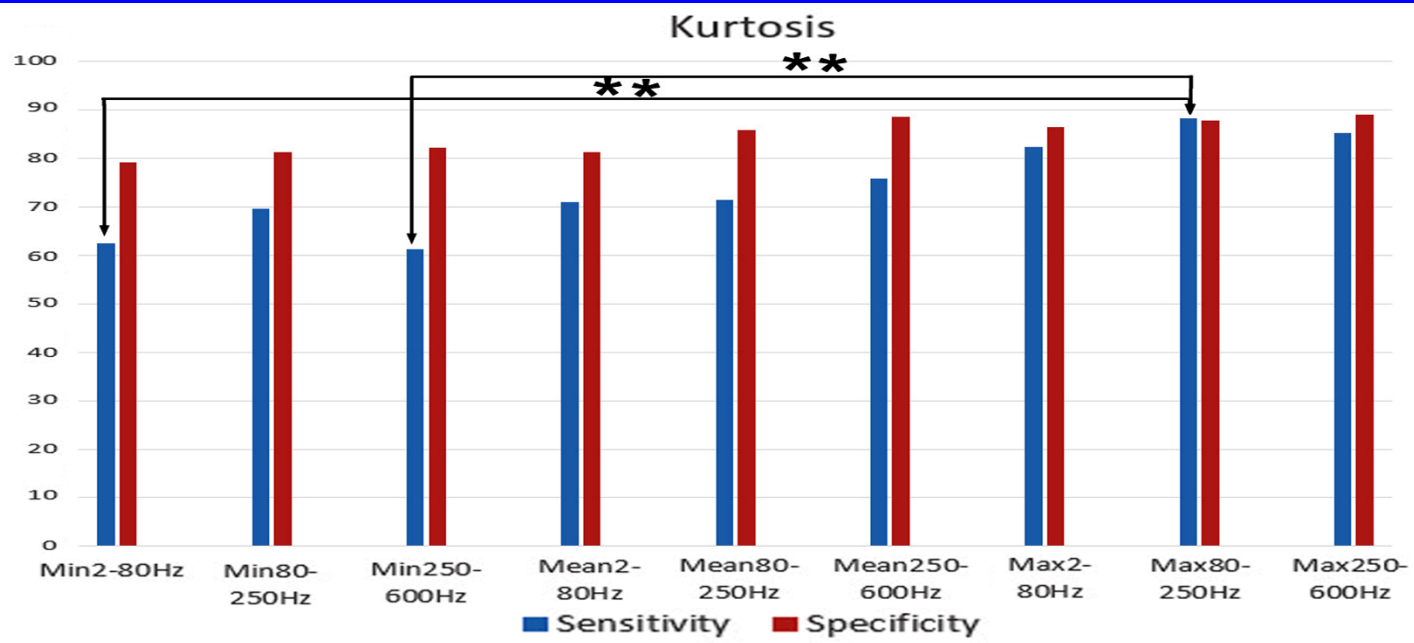


Kurtosis



Skewness

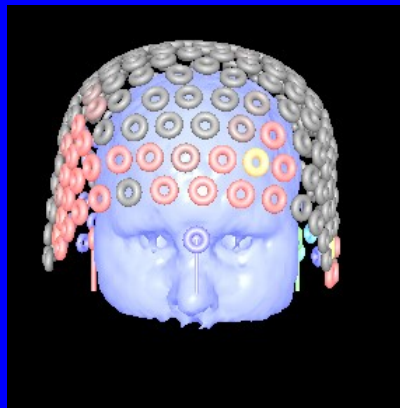
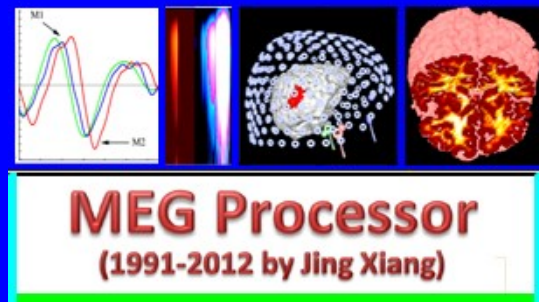




Virtual Sensor Kurtosis and Skewness

- Epilepsy: Altered kurtosis and skewness in VE HFBS.
- Kurtosis of VE signals in 80-250 Hz are the most sensitive
- Kurtosis of VE signals in 250-600 Hz are the most specific
- Propose to use VE HFBS in kurtosis/skewness:
 - ❖ Maximum kurtosis in 80-250 Hz for phase I
 - ❖ Maximum kurtosis in 250-600 Hz for phase II

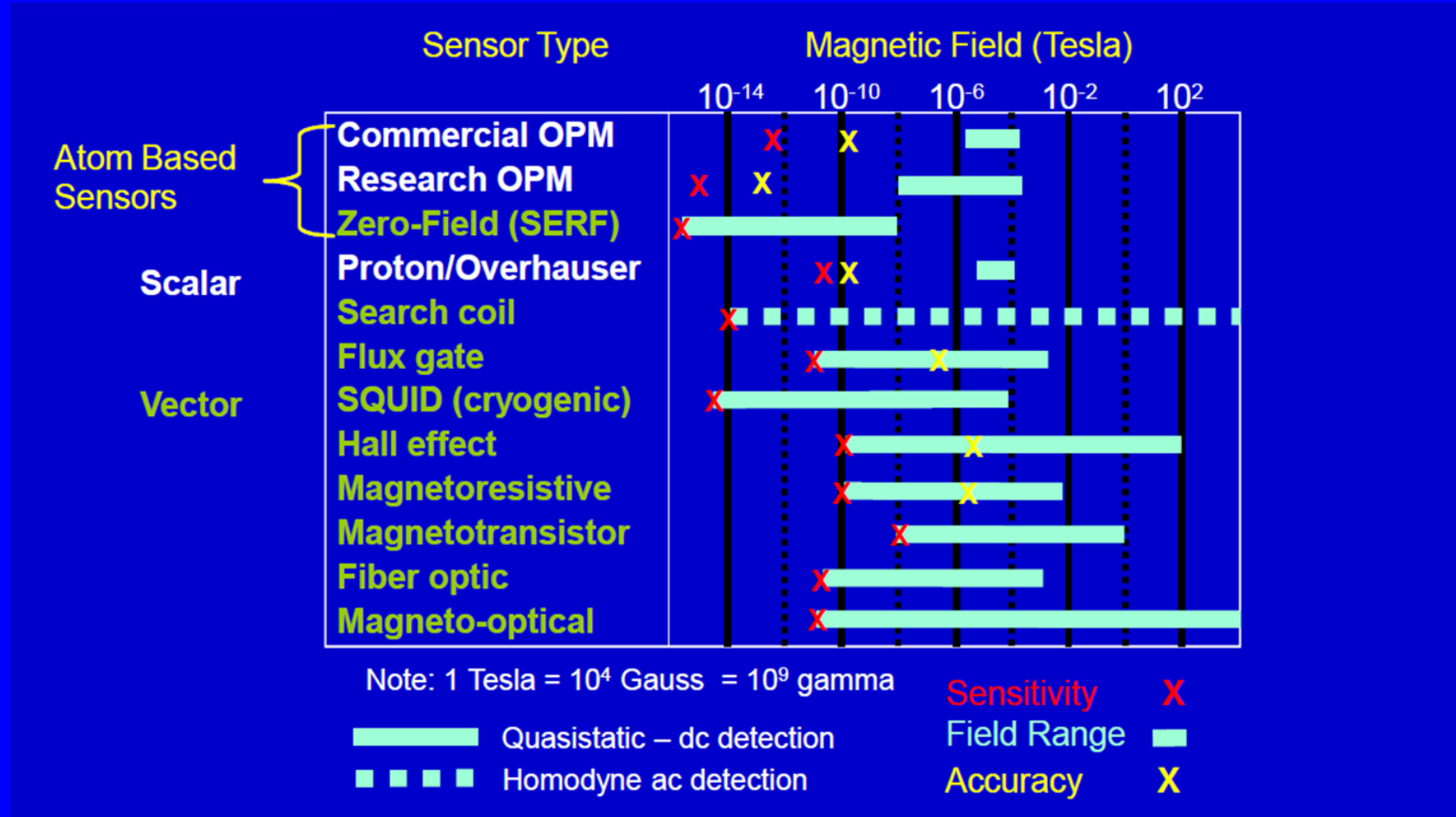
High Sampling Multi-channel MEG/EEG → Big Data



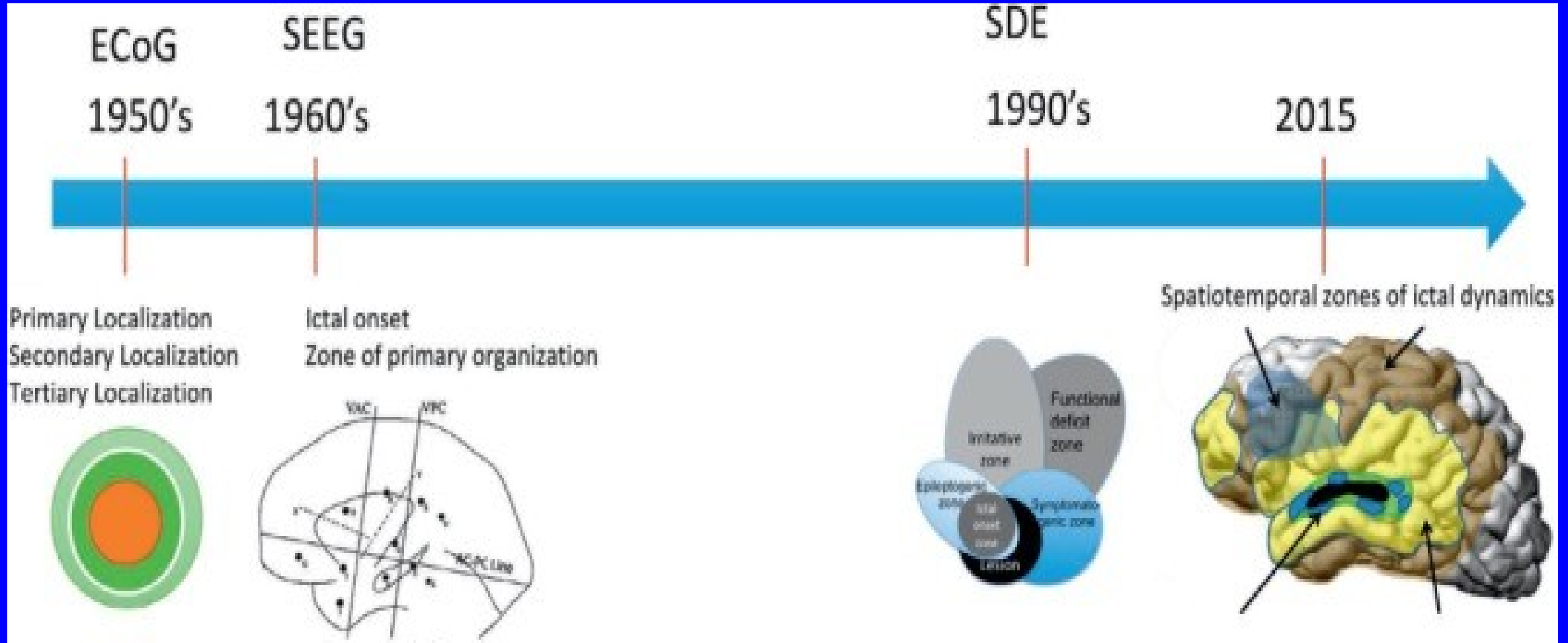
- Big Data
- Cloud

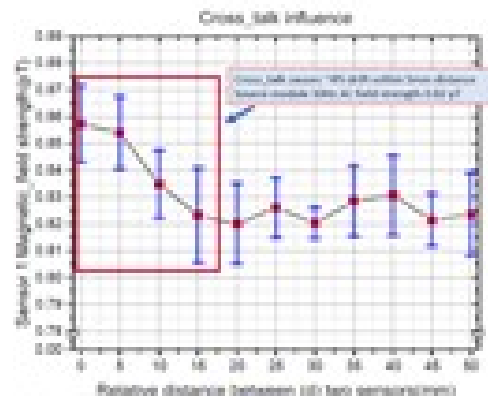
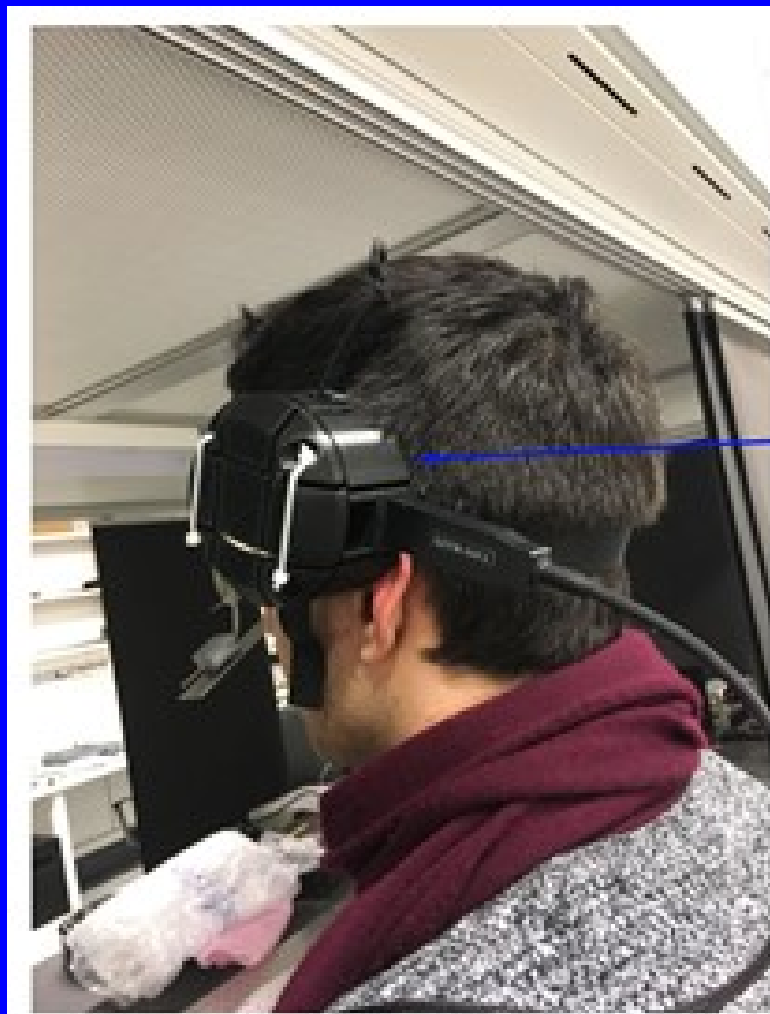
- Multi-channel and high-sampling MEG/EEG → Big Data
- 275 x 12000 → 1 GB/1 Minute → 1 TB/1 Hour

New Next Generation of MEG Sensor

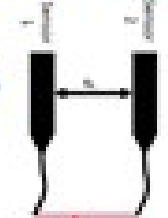


Epilepsy Surgery

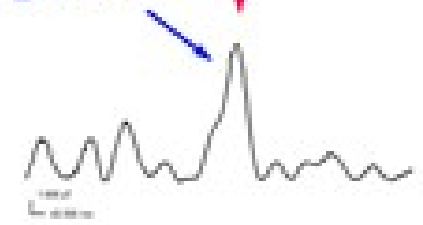




OPM Gradiometer



Spikes



Epileptic vs Physiological HFOs

	Epileptic HFOs	Physiological HFOs	Artificial HFOs*	
Waveforms	Oscillations	>4	any	
	Amplitudes	>1.5 SD of baseline [†]	<1.5 SD of baseline [†]	>10 SD of baseline
	Overlap on spikes	Yes [‡]	No	No
	Ride on slow wave	Yes [‡]	No	No
	Visible in both raw and filtered data	Yes [‡]	Yes	No
Spectrograms	Inter-event interval	>25 ms	> 25 ms	
	Time	irregular burst: 5-30 ms	Rhythmic, ~70 ms	Random/constant
	Frequency	80-250 Hz (ripples); 250-600Hz (fast ripples); 600-2500 Hz (VHFOs)	Elicited: 70-150 Hz Endogenous: 102 Hz	< 100 Hz >2500 Hz 60 Hz or 50 Hz.
	Pattern	Isolate island or horizontal	Connected or vertical	Straight lines
	Power	Very high power > 3 μV	Low-median power ~0.65 μV	Fixed.
Source imaging	Ratio (HFOs/alpha)	>0.38 [‡]	<0.27 [‡]	>4.0 [‡]
	Location	Energy > 95% background Within the brain (cortex, gray matter)	Energy > 85% background Within the brain (cortex, gray matter)	undefined Out of the brain (around neck, eyes)
	Source strength	>3 SD of the global mean	> 1 SD of the global mean	> 10 SD of global mean
	Pattern	Peak with propagated activation	Activation without clear peaks	Typically irregular
Networks	Relation to MRI/CT	Mimic anatomical shape	Mimic anatomical shape	No relation
	Hub Location	Within the brain	Within the brain	Out of the brain
	Hub strength	Increased [‡]	Normal [‡]	No connection
Modulation	Clustering index	Increased [‡]	Normal [‡]	Not available
	Path	Shortened [‡]	Normal [‡]	Not available
	NREM Sleep	Decrease [‡]	No change [‡]	No change
	REM Sleep	No change [‡]	Ripple increase [‡]	No change
	Sleep stage	Large extent (NREM) [‡]	Small extent (REM) [‡]	No change
	Sleep cycle	High rate in first cycle [‡]	Low rate in first cycle [‡]	No change
Clinical correlates	Task induced	No [‡]	Yes [‡]	No
	Sleep time	Decrease with time during NREM	Increase with time during REM	
	High rates in SOZ	Yes [‡]	No [‡]	No relationship
	Increase with Seizure frequency	Yes [‡]	No [‡]	No relationship
	Anti-epileptic drug	Reduce HFOs	No	No relationship
Removal HFO tissues	Good surgical outcomes	No	No relationship	
Hyperventilation	Elicit HFOs (absence epilepsy)	No	No relationship	

SD: standard deviation; SOZ: seizure onset zone; AED: antiepileptic drug
[†]Compared to normative database: ~160 healthy children
[‡]Compared to pediatric epilepsy database: ~ 398 pediatric epilepsy patients
*Artificial HFOs: power-line noise, cardiac signals, muscle activity, eye movement, Gibbs filter artifact

Demo (SEEG/iEEG to MRI/CT)



Demo (3, HFO burst)

The screenshot displays the MEGProcessor software interface. The main window shows a source scan for the current trial, with a table of source locations and their coordinates. The table is as follows:

Name	X	Y	Z
0_E_Vs Tip	3.843047	82.636622	46.000000
1_E_Vs1	-2.000000	84.000000	46.000000
2_E_Vs2	-5.408444	84.795304	46.000000
3_E_Vs3	-8.816888	85.590607	46.000000
4_E_Vs4	-12.225333	86.385911	46.000000
5_E_Vs5	-15.633777	87.181215	46.000000
6_E_Vs6	-19.042221	87.976518	46.000000
7_E_Vs7	-22.450665	88.771822	46.000000
8_E_Vs8	-25.859110	89.567126	46.000000
9_E_Vs9	-29.267554	90.362429	46.000000
10_E_Vs10	-32.675998	91.157733	46.000000
11_E_Vs11	-36.084442	91.953037	46.000000
12_E_Vs12	-39.492886	92.748340	46.000000
13_E_Vs...	-45.335934	94.111718	46.000000

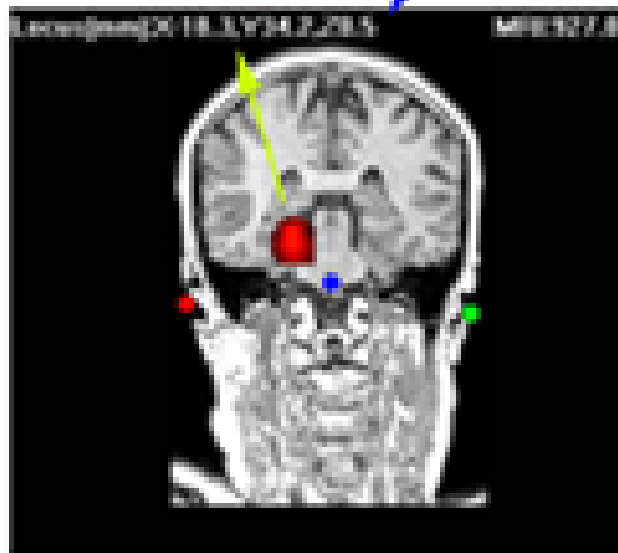
The interface also includes a 'Grid' section with the following settings:

Minimum	Maximum	Step	Grid
-30	30	6	1

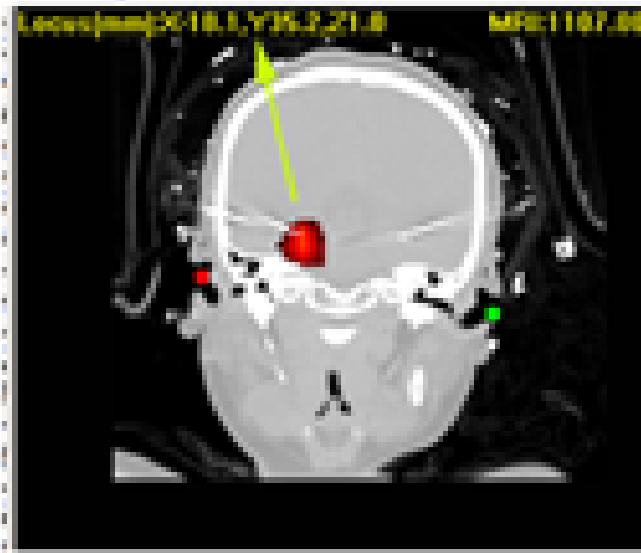
At the bottom, there are source ID labels: MRF0921, MRF0931, and MZF0941, along with their corresponding coordinates.

HFO Source Imaging (Noninvasive vs. Invasive)

Location Measurement



MEG + MRI



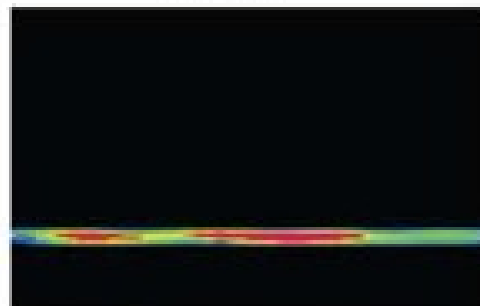
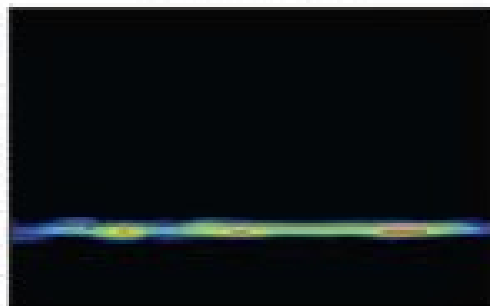
iEEG + CT

0 100

Interictal

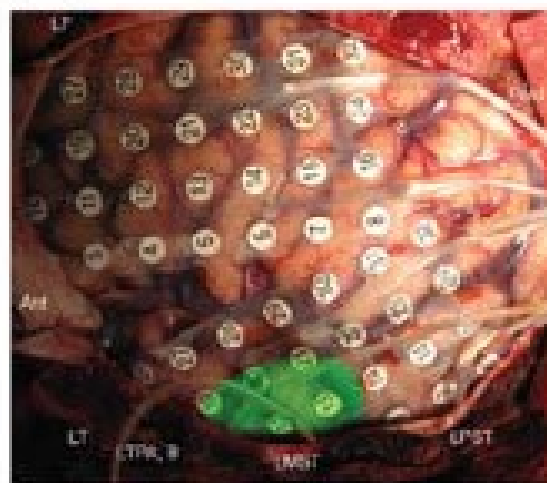
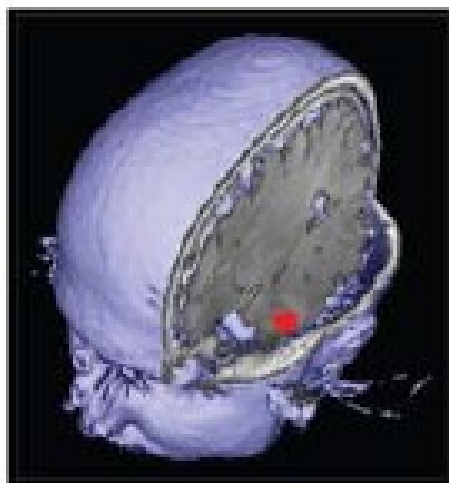
Ictal

1000 Hz



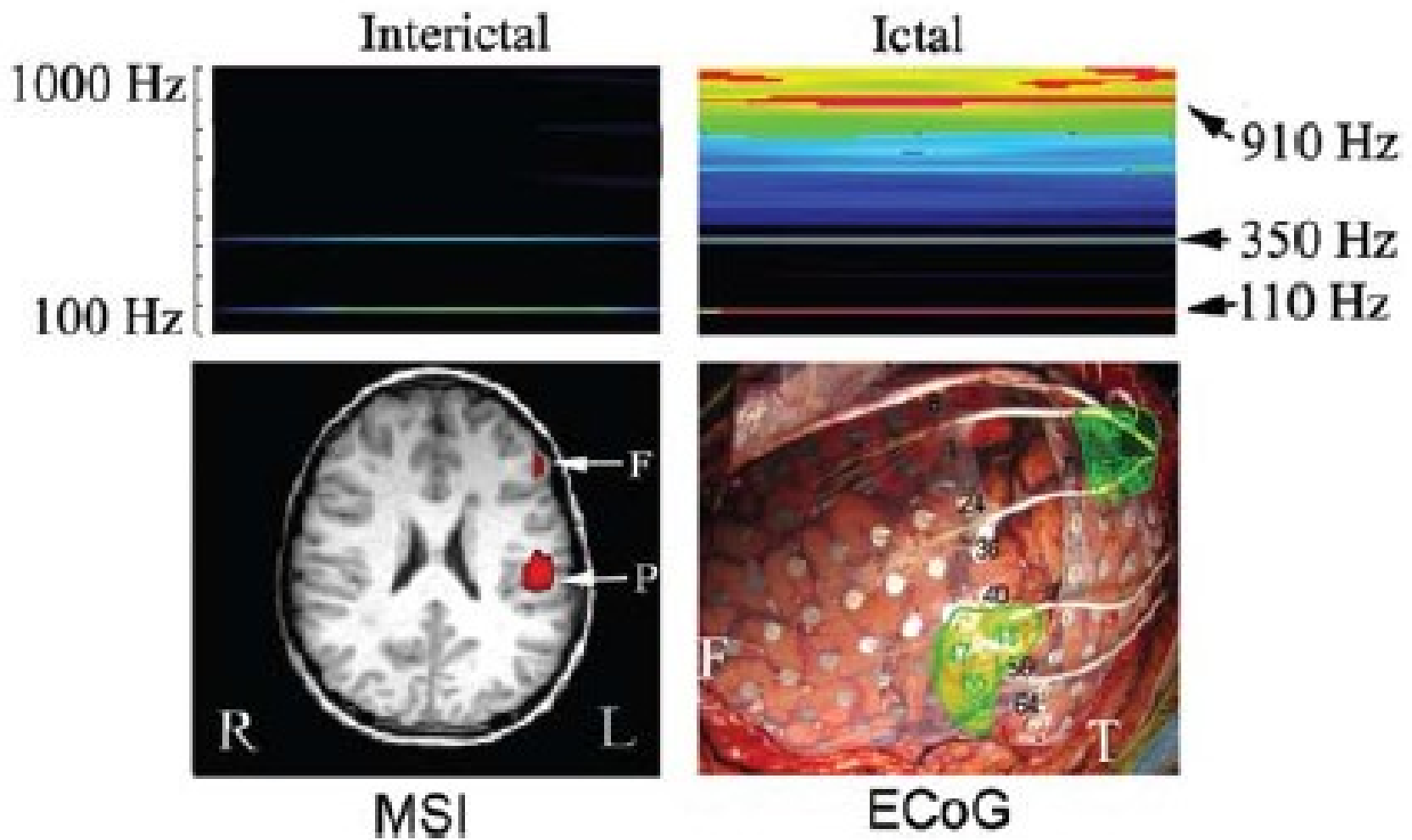
230 Hz

100 Hz

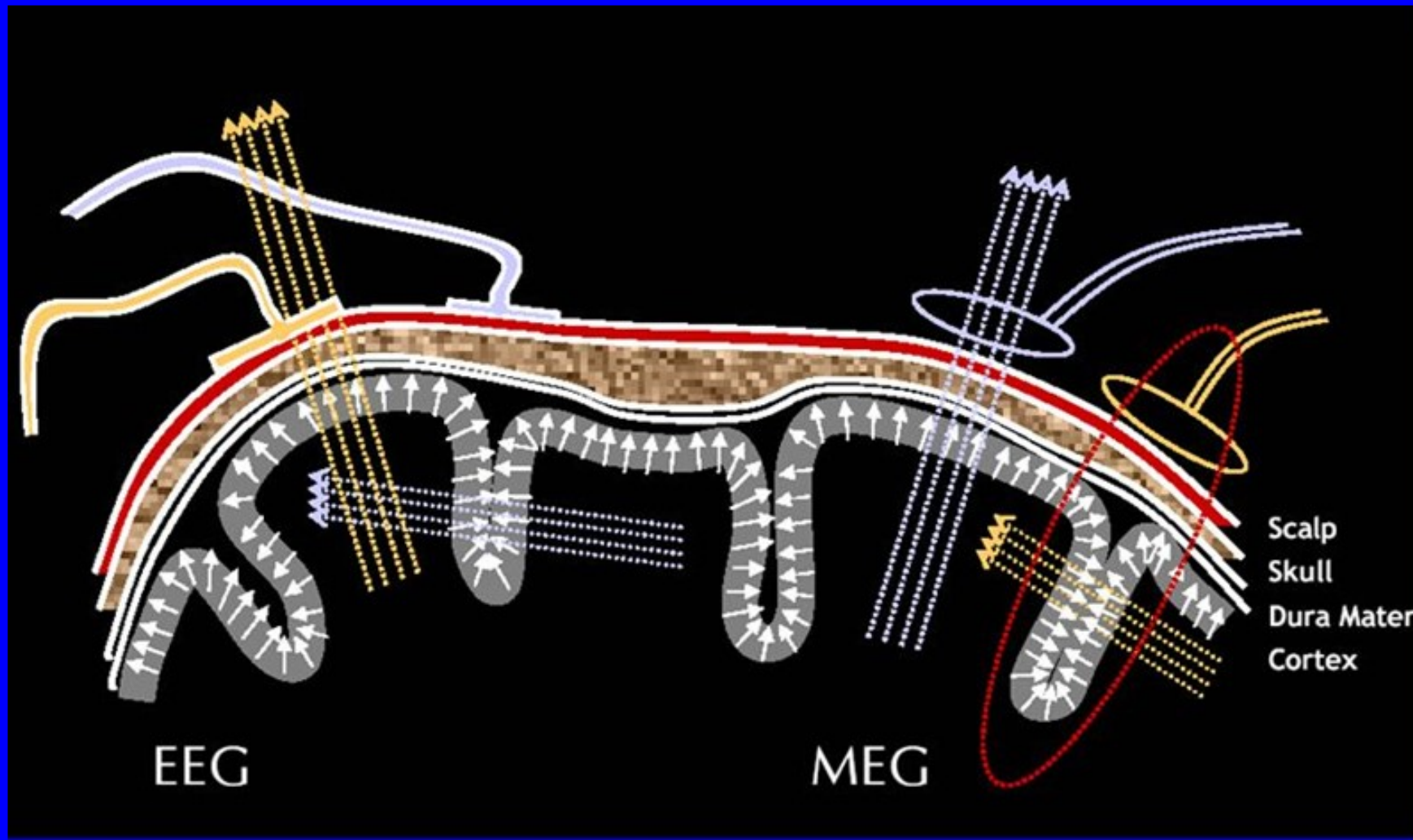


MSI

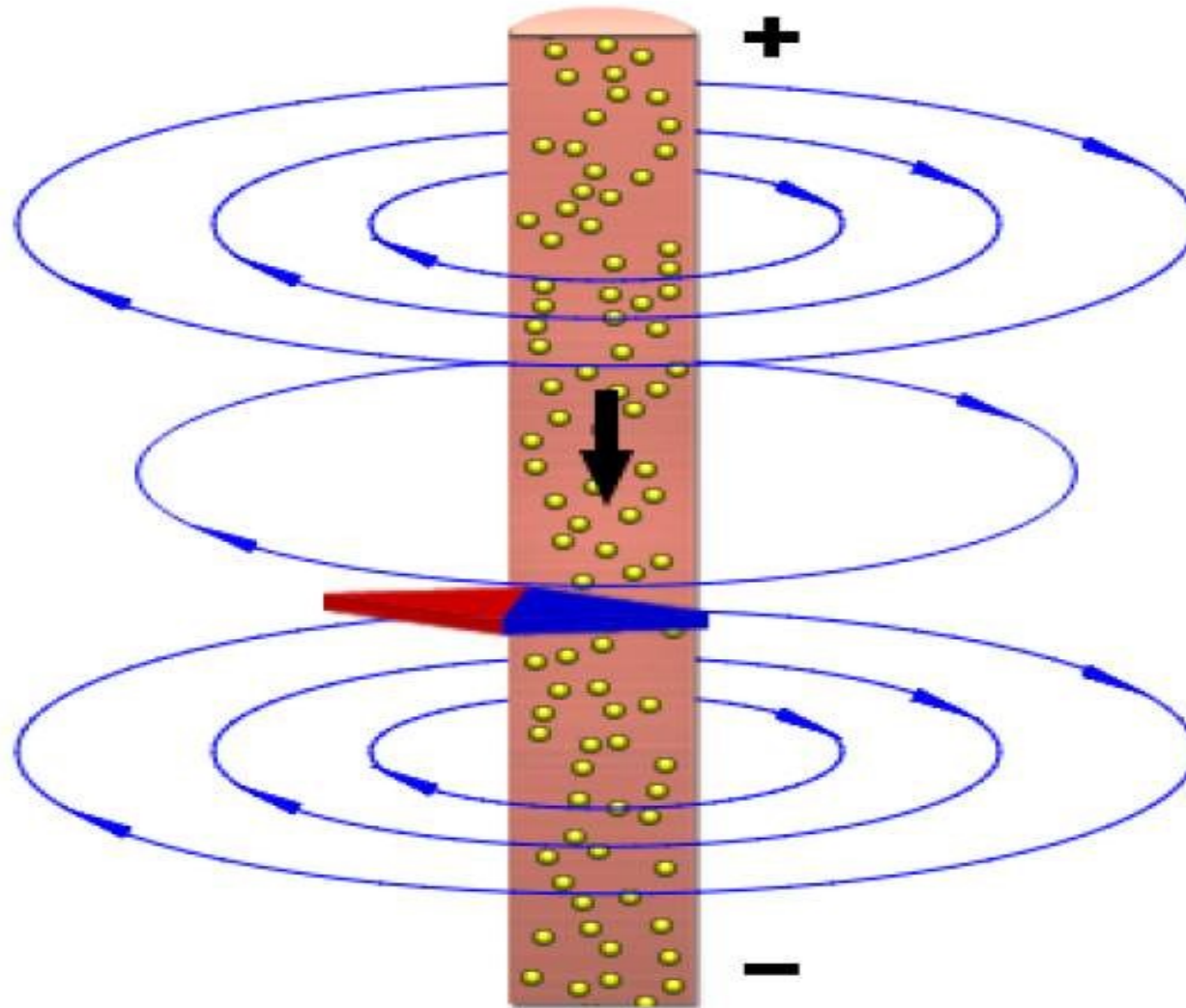
ECoG



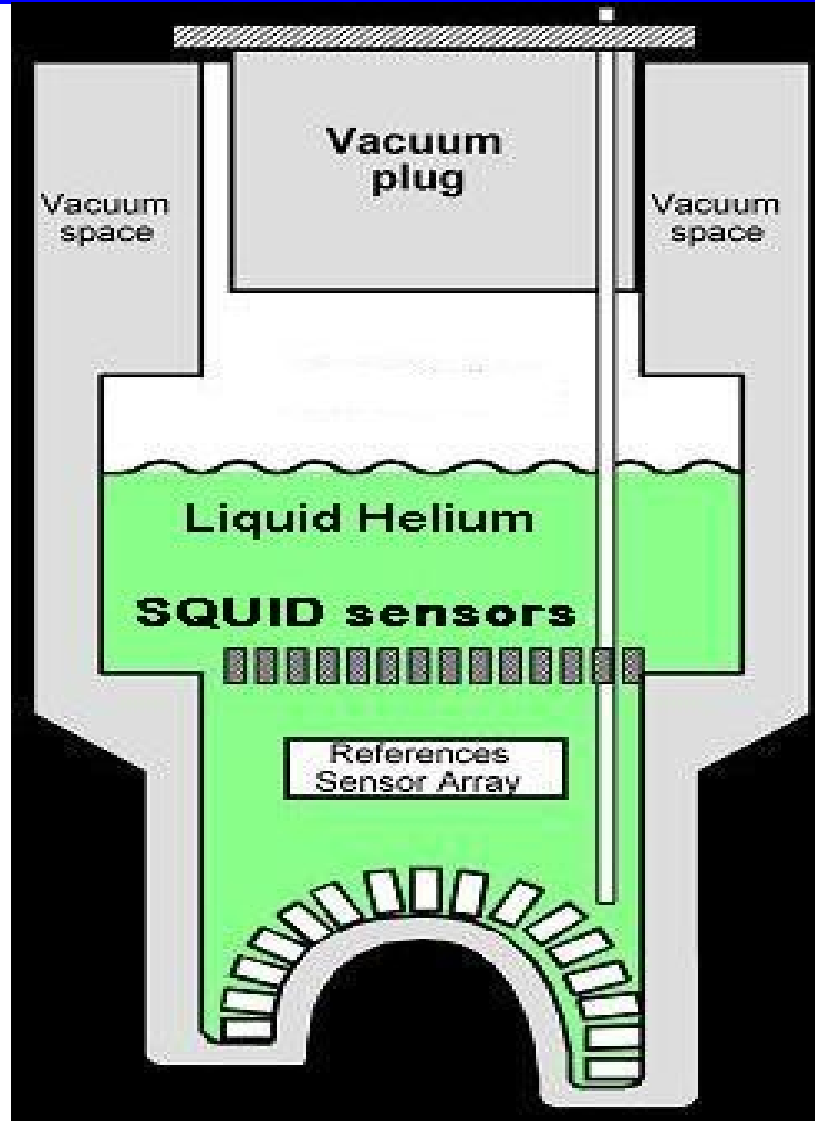
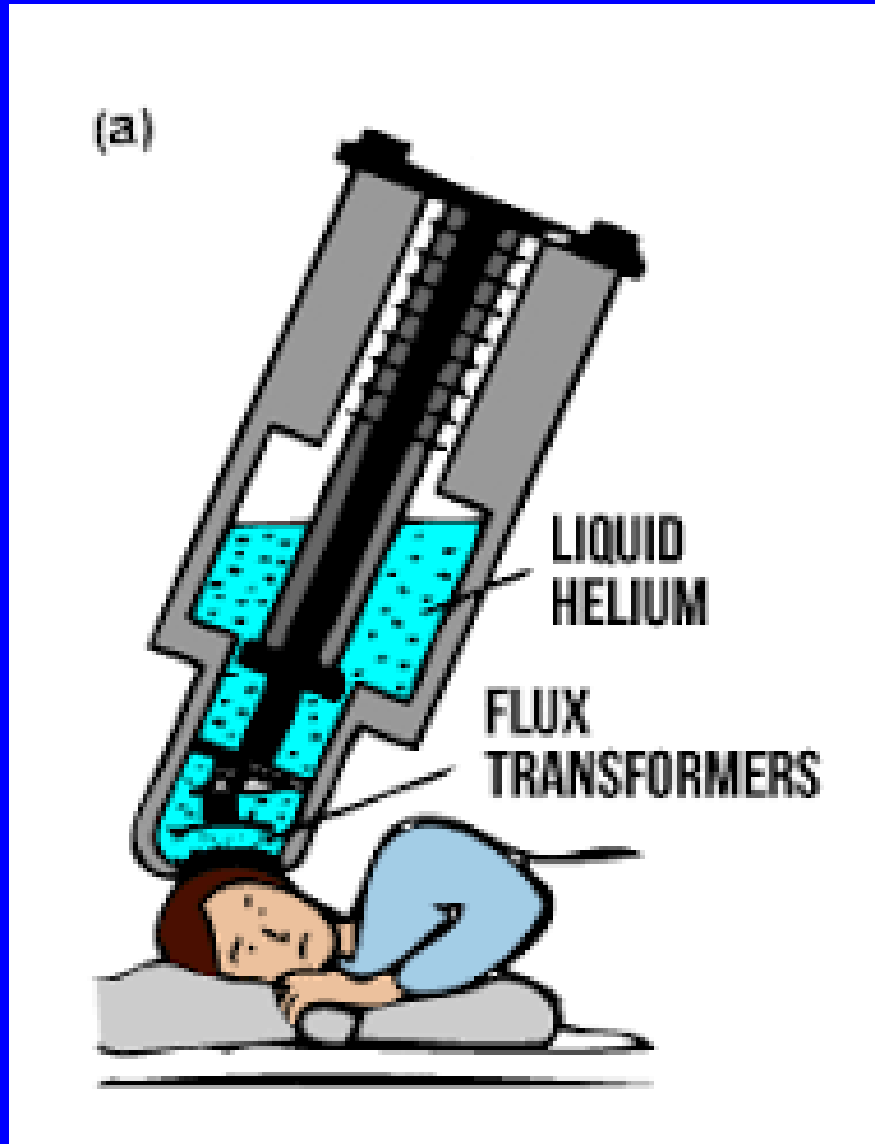
MEG and EEG



Electrical vs. Magnetic Signals



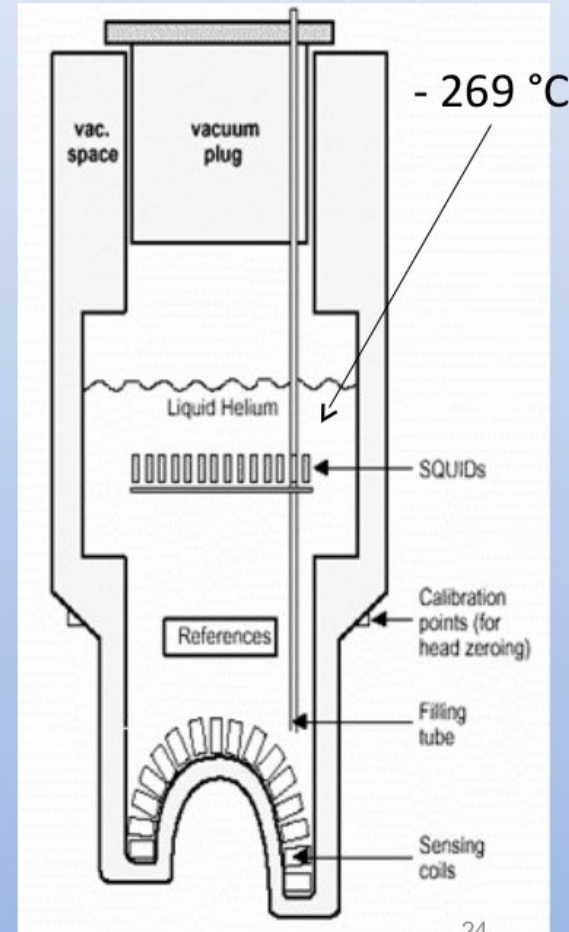
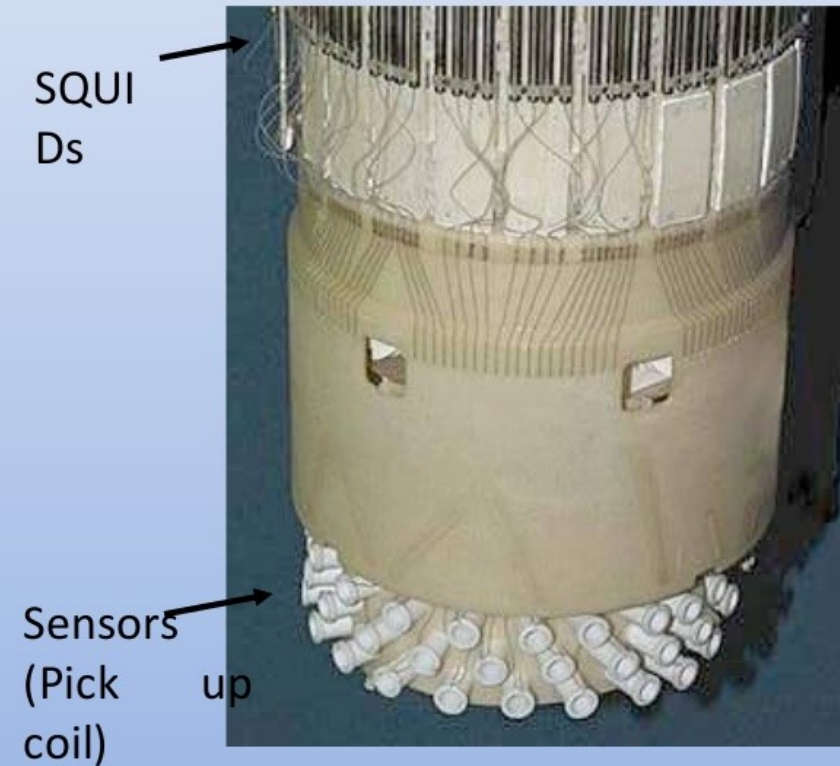
SQUID Based MEG



Superconducting Quantum Interference Device (SQUID)

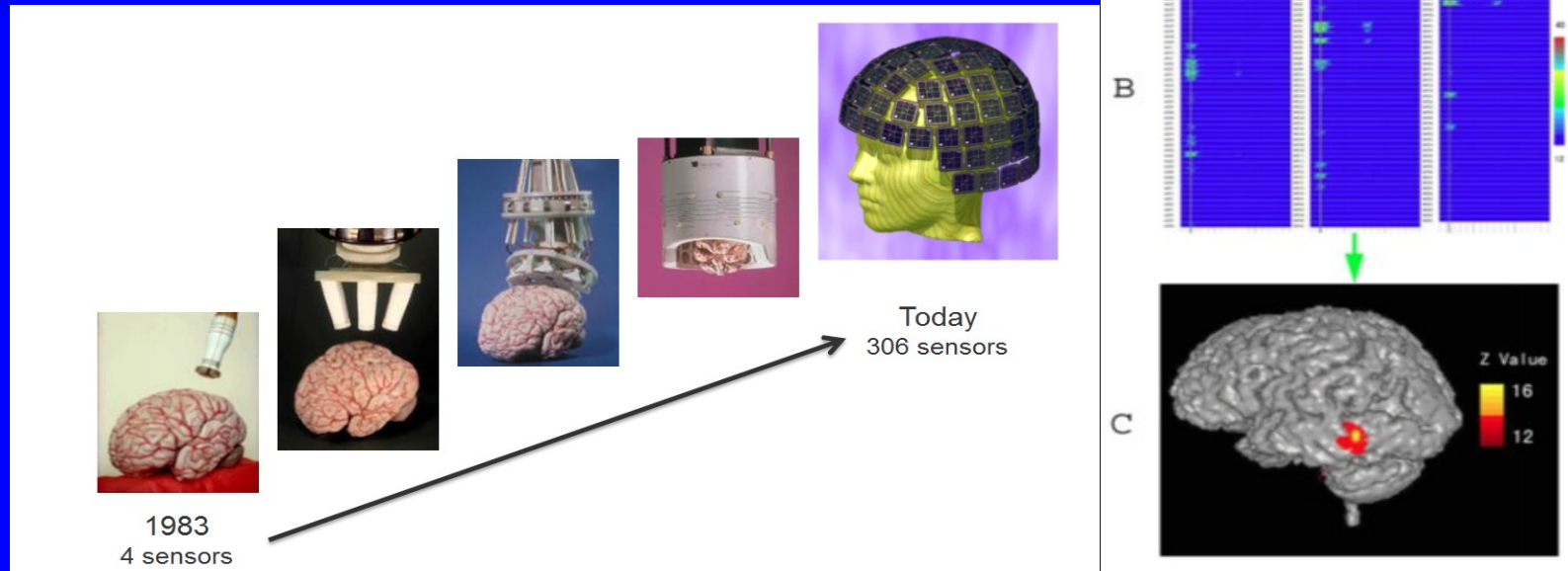
The EEG & MEG instrumentation

MEG

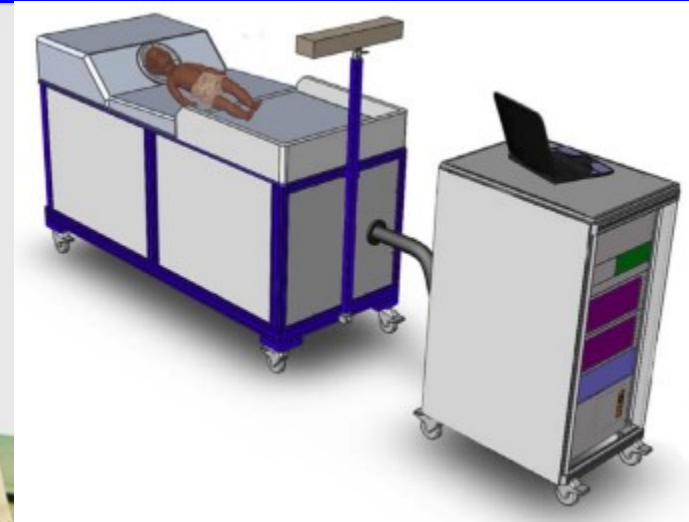
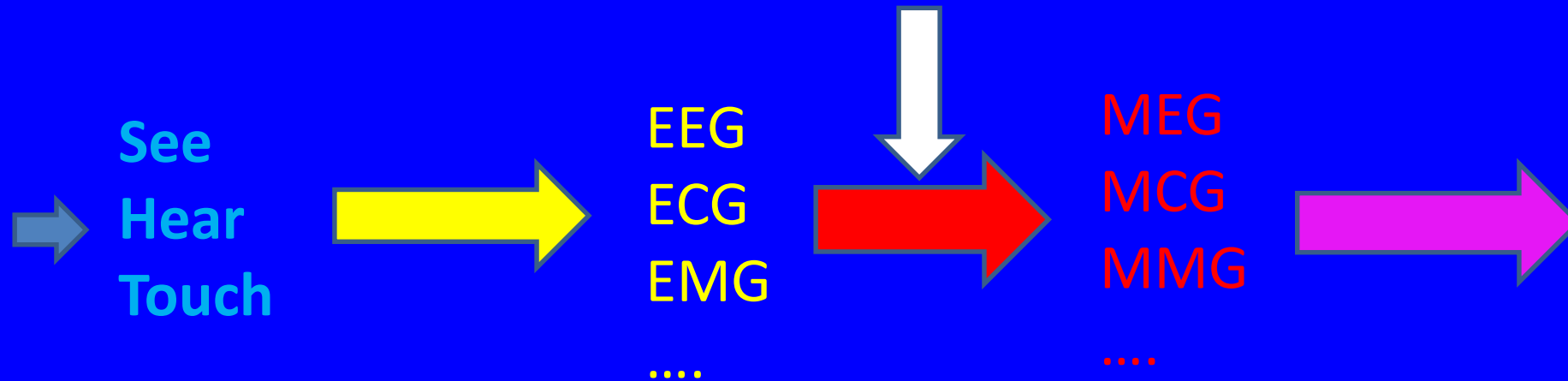


Development of Magnetoencephalography (MEG)

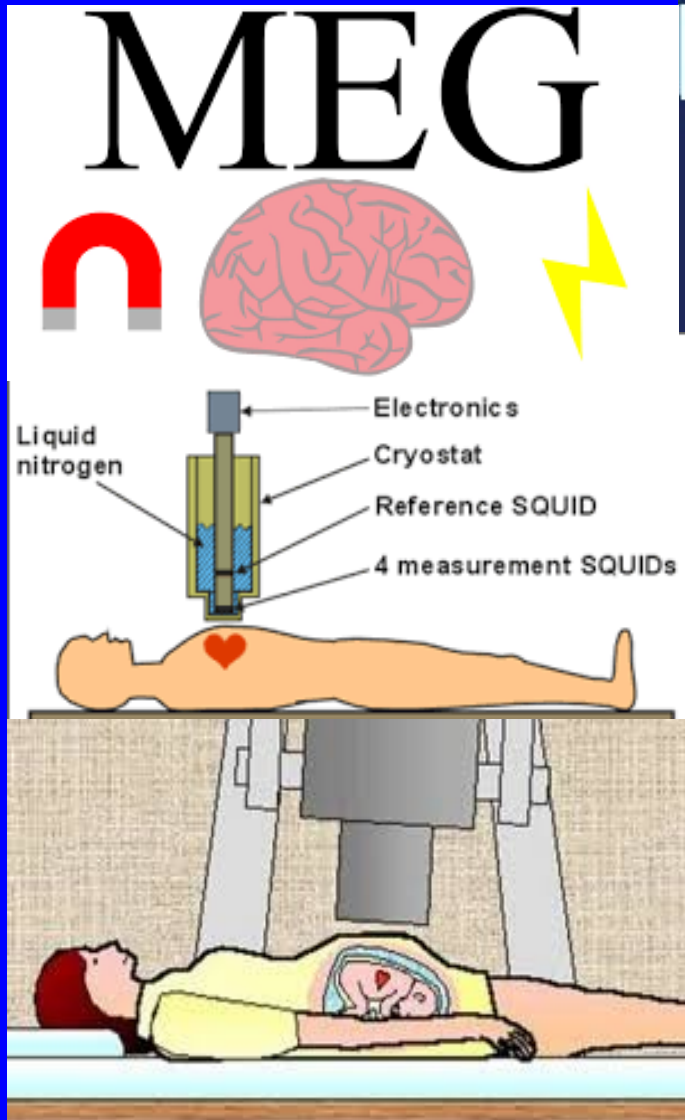
- High sampling rate hardware
- HFOs are highly localized and can be utilized for developing better MEG/EEG source localization methods (e.g. wavelet-based beamformer).



Development of Biomagnetism



Biomagnetic Signals



Focus on MEG

The human heart's magnetic field can be measured several feet away from the body.

Negative emotions can create nervous system chaos, but positive emotions do the opposite.

Positive emotions can increase the brain's ability to make good decisions.

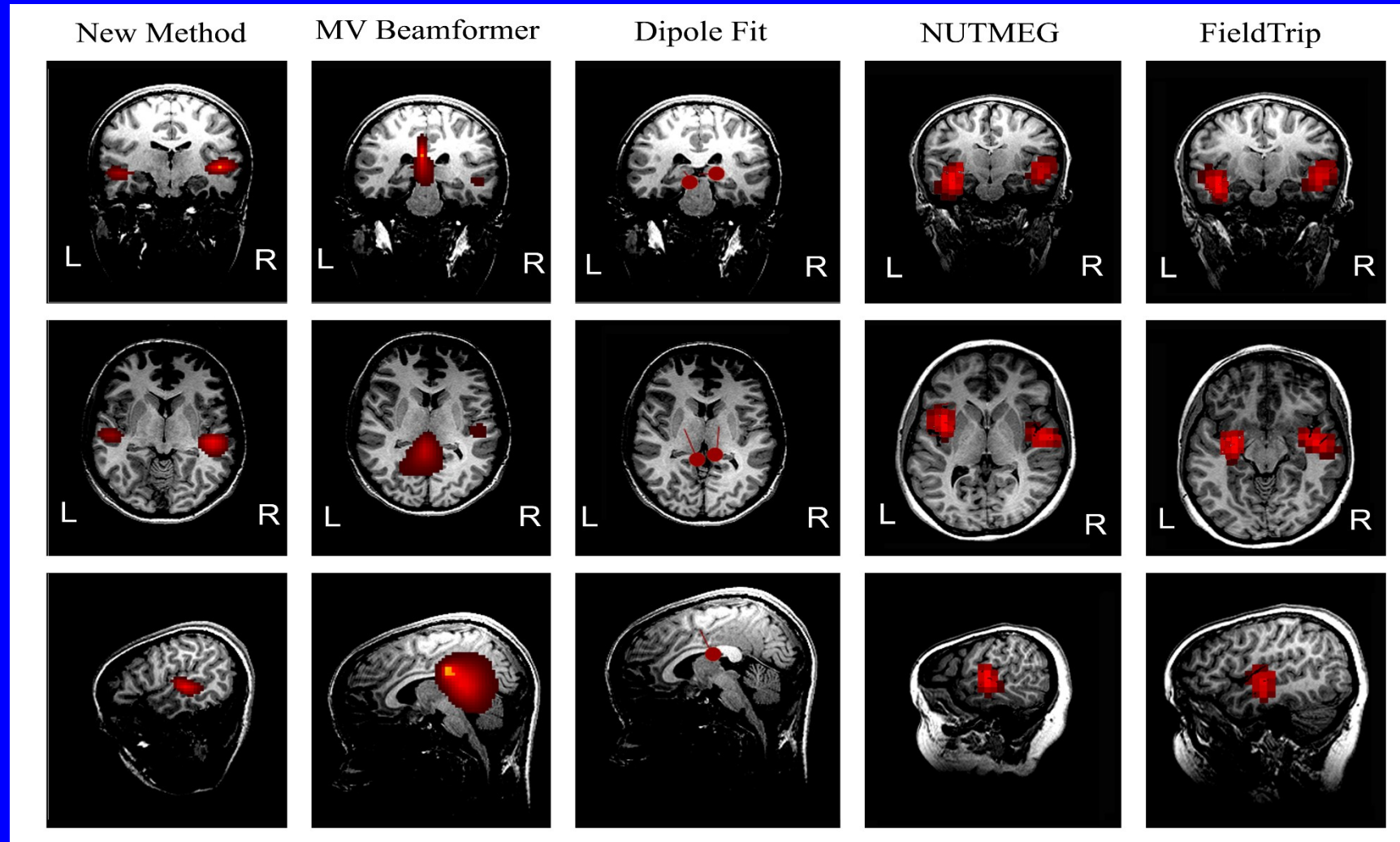
You can boost your immune system by focusing on positive emotions.

Positive emotions create physiological benefits in your body.

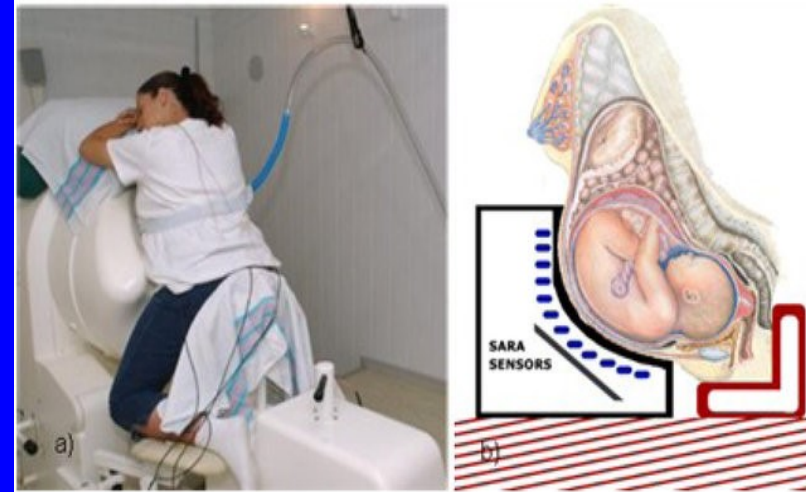
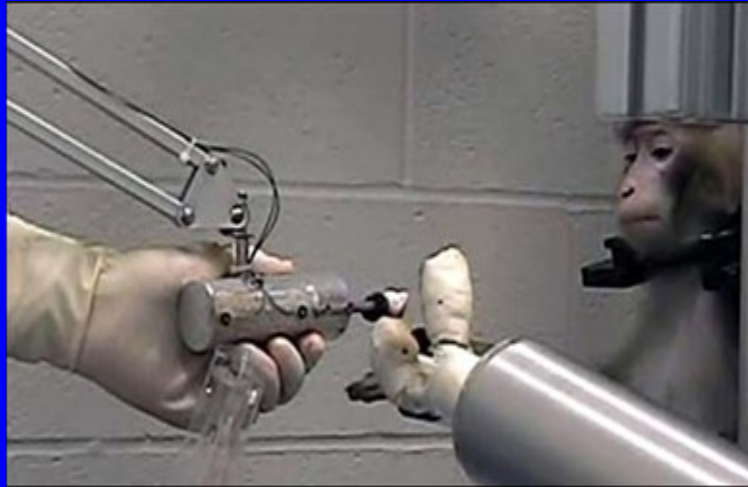
In fetal development, the heart forms and starts beating before the brain begins to develop.

The infographic features a central blue human silhouette with a glowing heart. Surrounding it are various illustrations: a wireframe human, a brain with neural activity, a fetus, and a person with a glowing heart. Text boxes provide information about the heart's magnetic field, the relationship between emotions and the nervous system, and the benefits of positive emotions. A green and purple waveform is shown at the top right.

Source Analysis Methods

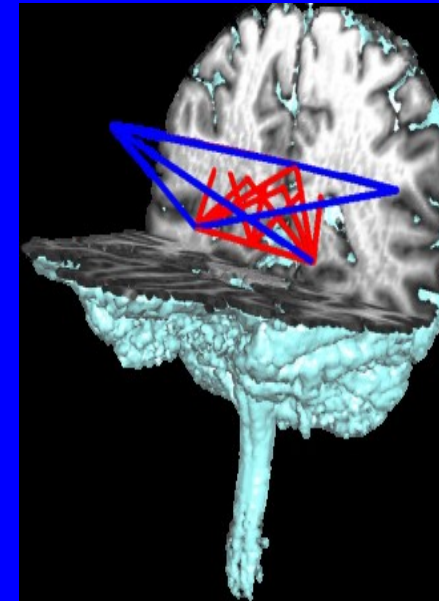
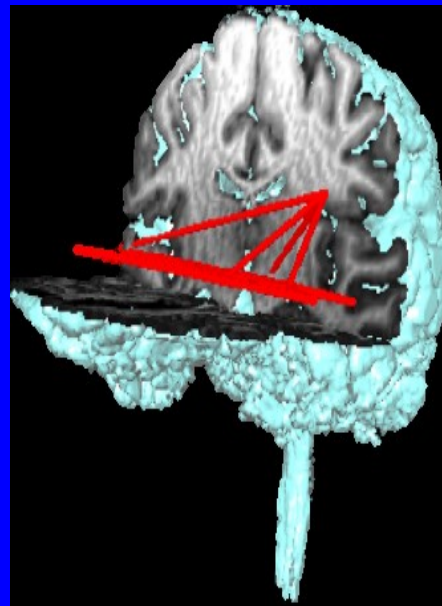
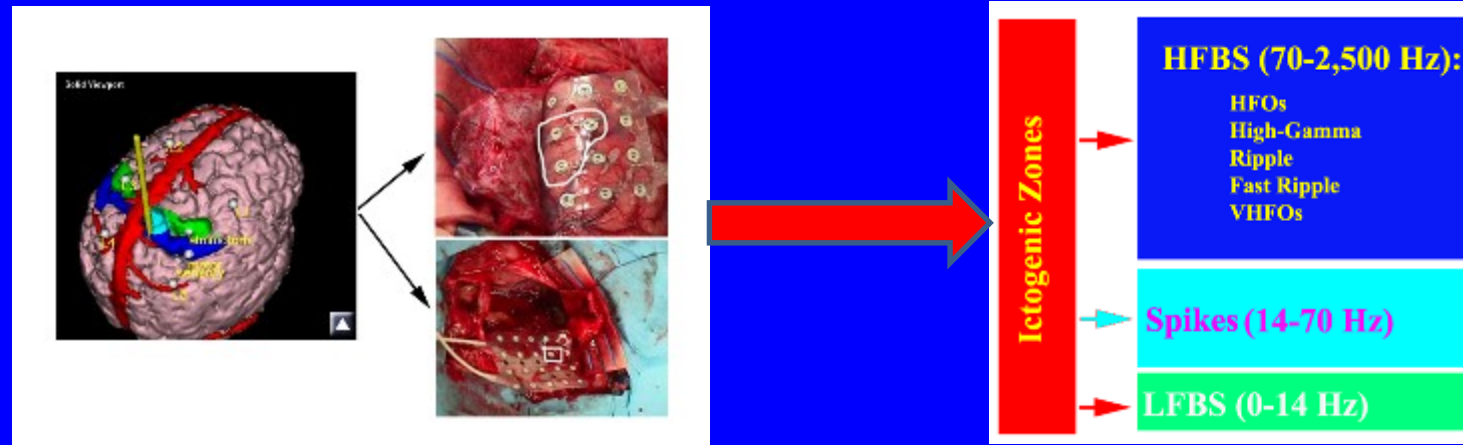


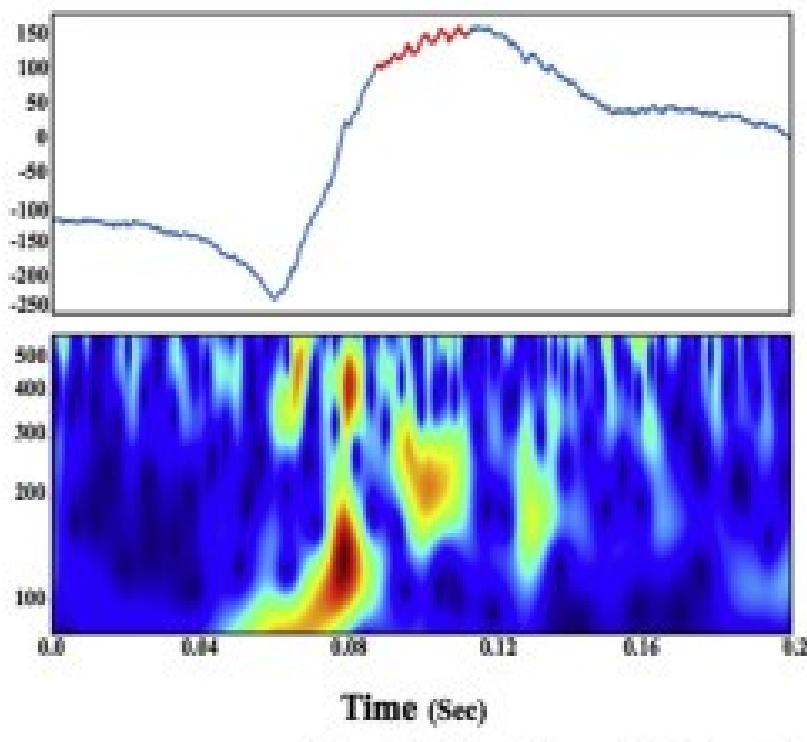
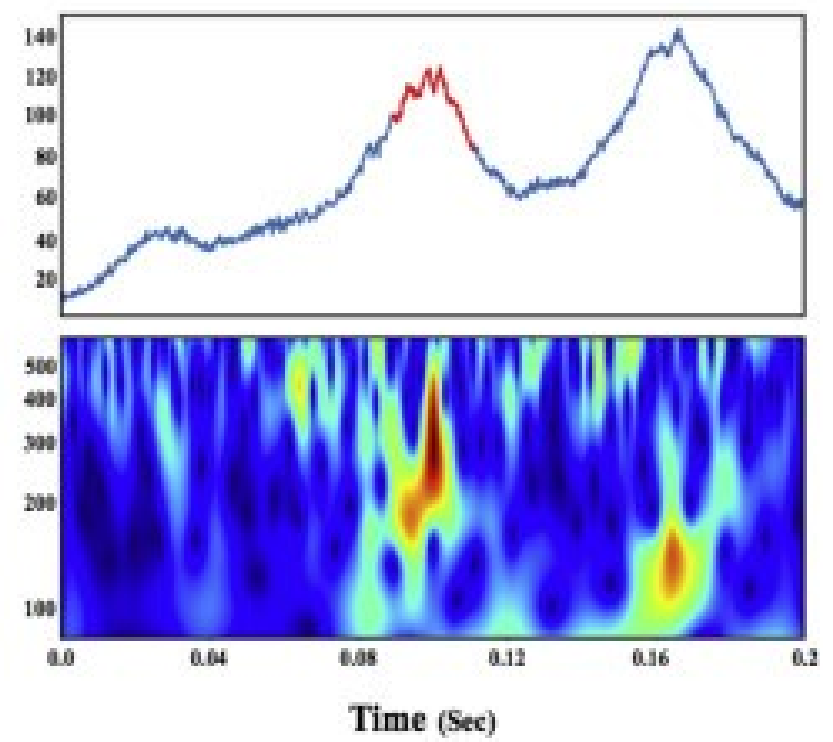
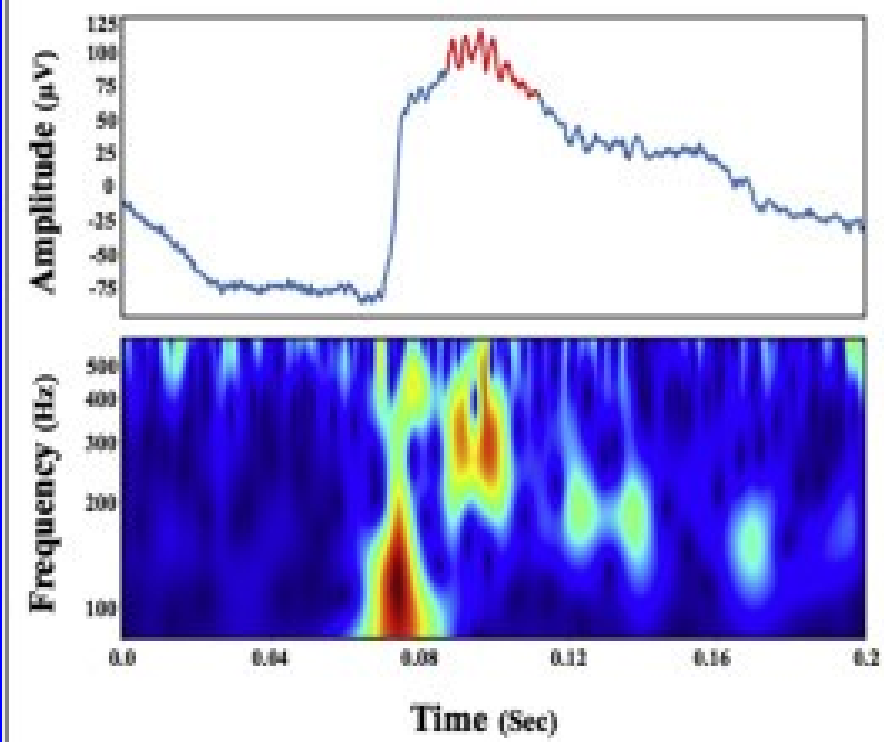
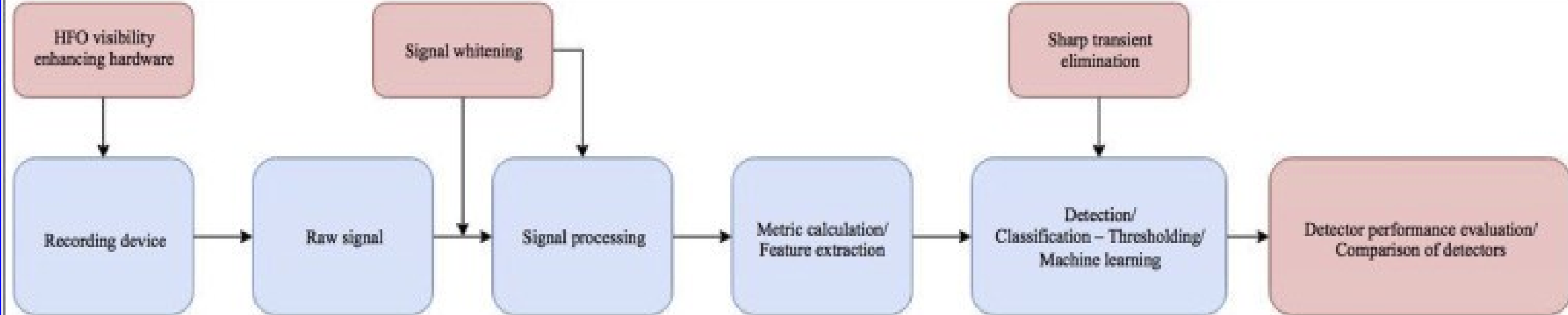
Other Applications of HFBS



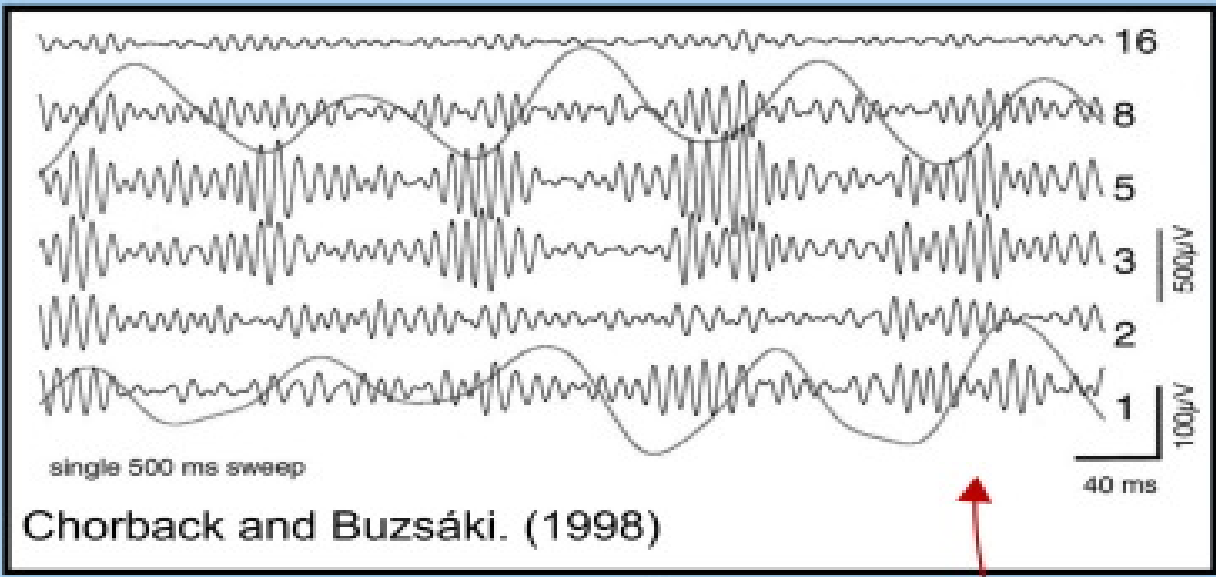
HFOs Are Noninvasively Detectable

(Change outcomes in Epilepsy and Migraine)

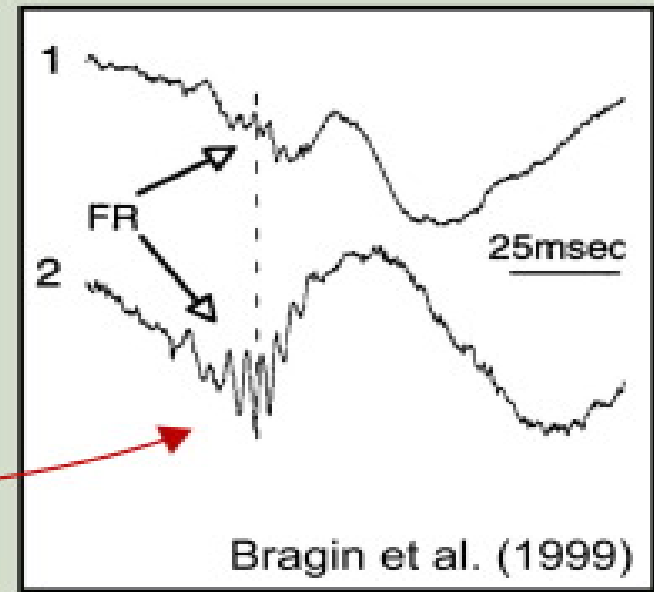
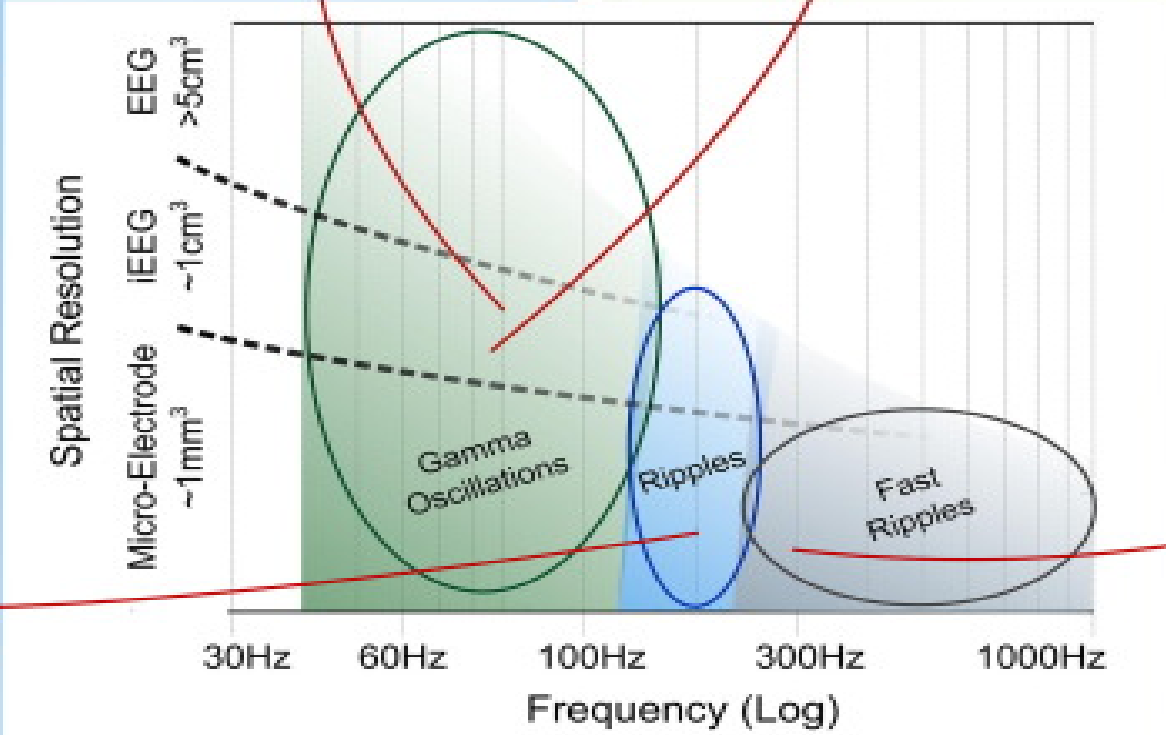
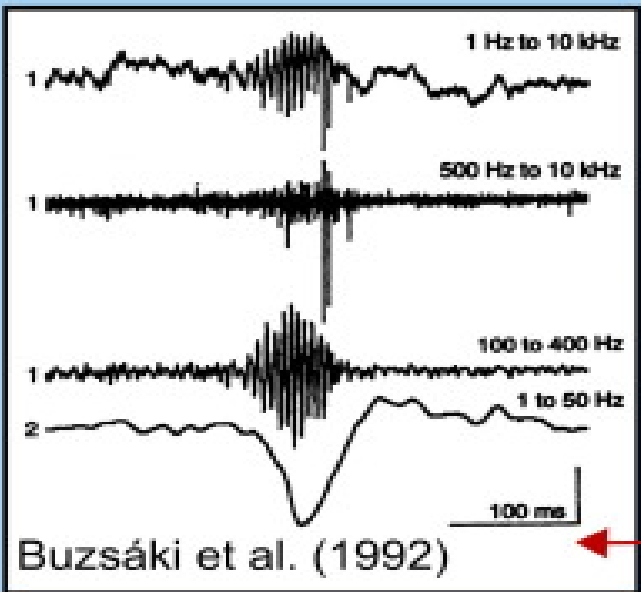
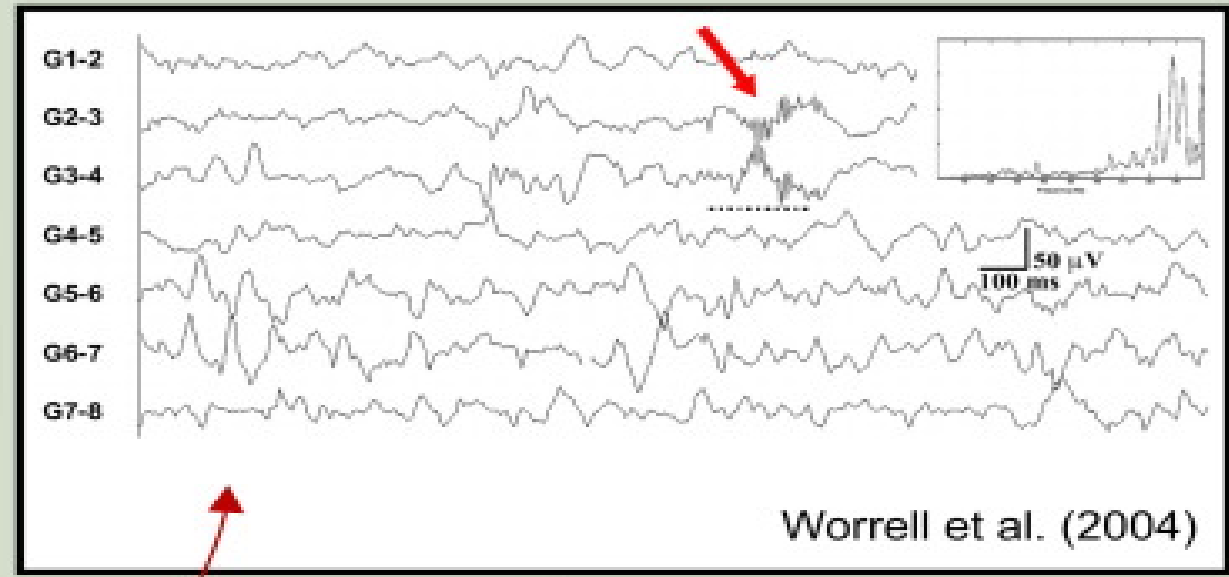




Physiological HFO



Pathological HFO



Brain Oscillations during Mental Preparation and Resting-State Activity

-Right hemisphere
-Left hemisphere
-Both

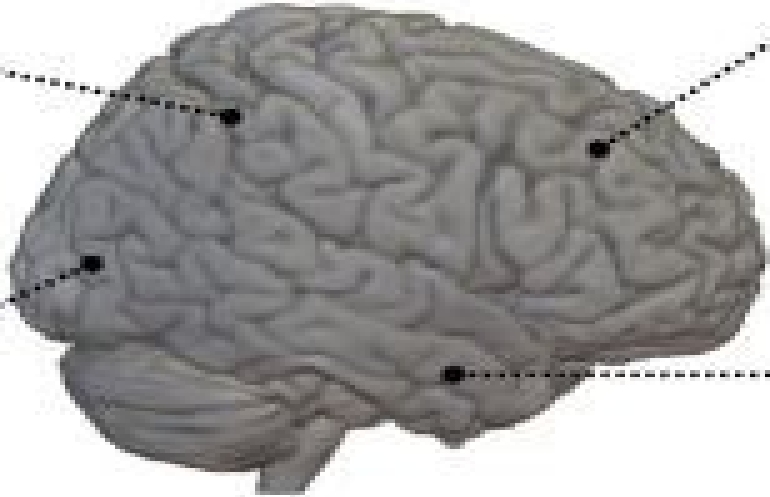
Studies:
(7) Kounios et al. 2006 (mental preparation - CRA)
(8) Kounios et al. 2008 (resting-state - anagrams)

Parietal lobe:

- ↓ α power (7)
- ↓ β_2 power (8)
- ↑ γ power (8, EO)
- ↓ β_3 power (8, EC)
- ↑ β_3 power (8, EO)
- ↓ γ power (8, EC)

Frontal lobe:

- ↓ α power (7)
- ↑ α power (8-9, 75Hz) (8)
- ↓ α power (8-9, 75 Hz) (8)
- ↑ β_2 power (8)
- ↑ β_3 power (8, EC)
- ↑ γ power (8, EC)



Occipital lobe:

- ↓ α (10-12, 75Hz) power (8)
- ↑ α power (7)
- ↓ β_1 power (8)
- ↑ β_3 power (8, EO)
- ↓ β_2 power (8)

Temporal lobe:

- ↓ α power (7)
- ↑ α power (8-9Hz) (8)
- ↑ β_2 power (8)
- ↑ β_3 power (8, EO)
- ↑ γ power (8, EC)
- ↑ β_3 power (8, EC)

High Insight subjects show widespread greater RH activity (11)